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# ABSTRACT

We present a statistical mechanics theory of rubber-like elasticity in swollen and unswollen polymer networks characterized by explicitly non-Gaussian distribution functions (Laplace's, Cauchy's, and continuous Poisson's in the exponential limit). An important outcome is the derivation of new families of statistical and mechanical laws, including a discussion of energy functions of strain invariants, which are reasonably simple for a model comparison with available data on polymer networks. Accordingly, a theoretical–experimental approach based on LF-NMR was devised to identify the most likely end-to-end length distribution in an arbitrary network. When this strategy is applied to agar 1 %, alginate 1 %, and scleroglucan 2 % hydrogels, it turns out that the end-to-end distribution should be never regarded as Gaussian even if, as in agar and scleroglucan systems, the normal statistics is the best among those here regarded. Remarkably, Poisson's distribution is proved instead to be the most realistic for the alginate hydrogel.

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# 1. Introduction

Rubber elasticity theory had probably the most enduring history in all of polymer disciplines, displaying a remarkable size of discrepancies with experimental data which were intensively and contradictorily debated for decades (see e.g. bibliography in Hild (1998)). The agreement one is usually left with is mainly qualitative and the probability distribution function governing the nascent network, whether it is swollen or unswollen, is generally unknown (Huang, Szleifer, & Peppas, 2002). A crucial question, which still remains, is a profound self-consistent description of microscopic chain conformations versus macroscopic network deformations, as the basic properties of deformation processes can only be explained qualitatively by means of topology arguments. Many disputes were on the roles of cross-link junctions, their fluctuations, cooperative movements and constraints they exert on the (first) neighboring chain conformations (Candau, Bastide, & Delsanti, 1982) and any relevant steric interaction, specially entanglements and various types of network defects, like physical and intramolecular crosslinks (Gedde, 1995). Topological constraints are not ascribable to chemical cross-links, they are very heterogeneous, act as interchain effects almost continuously along the chain and

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ultimately interplay with elastic and osmotic forces (Panyukov & Rabin, 1996; Priss, 1981). Entangled points, in particular, are temporary and of short duration (Hild, 1998). Mullins' early hypothesis, to deal with an apparent crosslink number summing chemical junctions and physical entanglements, was afterwards denied (Gedde, 1995).

Over the years polymer scientists complemented and/or corrected the classical theories by more realistic mechanisms (Priss, 1981). Gaussian mean-field assumptions, in fact, are anyway restrictive (e.g. small elongations, networks prepared by coalescing concentrated solutions with compressed or weakly stretched chains, etc.) and, normally, better tolerated in the dry state, which is representative of dense neutral polymer systems where excluded volumes screen out. On the other hand, swollen networks in good solvents are notoriously non-Gaussian, the most effective, yet elegant analysis, being still given by de Gennes' scaling theory. furnishing a universal description in terms of blob correlations (de Gennes, 1979). Between dilute and Gaussian regimes, chain conformations behave as a random walk of blobs with correlation length equal to the average mesh size of semidilute solutions (see e.g. Mezzasalma (2008)). The  $c^*$  theorem, however, only holds in networks with almost regular topology and synthesized at the overlap threshold between dilute and semidilute regimes (Panyukov, 1990), while real swelling phenomena are affected by topological disorder and inhomogeneities (entanglements, dangling ends, closed loops, crosslink reactions), trapped in the preparation process, by heterogeneous fluctuations in the cross-link density, increasing beyond the thermodynamic values, and by geometric effects (Johner, Vilgis, & Joanny; Mezzasalma, 2001; Panyukov, 1989, 1990). Cross-link density seems itself to be an ill-defined variable that, particularly in highly cross-linked states, strongly depends on the adopted model (Valentín, Carretero-González, Mora-Barrantes, Chassé, & Saalwächter, 2008). Even to define a consistent measure for polymer volumes is not an immediate task, as the average network energy seems to scale with anomalous exponents that are incompatible with mean-field approaches (Hadizadeh, Linhananta, & Plotkin, 2011).

Besides statistical mechanics of networks, their topology and continuum mechanics, a second analysis level focuses on chain conformations and chemical structure, like the quite recent inquiries into segmental orders show. In short, vector order parameters, inaccessible to NMR, relates to the residual chain orientation, while tensor parameters from multi-quantum NMR measurements characterize the fluctuation extents in segment orientations. The true network elasticity follows in fact from the actual conformation space made available to chain portions, i.e. from the excursion of individual segment orientations. The narrow dynamic profile that comes from local NMR measurements in elastomers thus suggests that the single chain description relying on a purely affine model should fail (Saalwächter & Sommer, 2007). Alongside Edwards' second-moment tensor parameter, of flexible excluded-volume polymers in a weakly good solvent, displays a inhomogeneous distribution decaying along the chain, with lower segmental orders than in Gaussian statistics (Usatenko & Sommer, 2008). End-linked mono- and bi-modal networks were also studied by means of Monte Carlo bond-fluctuation simulations. The vector order parameter of longer chains was twice as large as in Gaussian systems, the shorter ones displaying a much lower value than expected (Sommer & Saalwächter, 2005). Such discrepancies suggest that interchain effects may influence the bond orientation even in concentrated states, where Gaussian statistics should be expected (de Gennes, 1979).

Motivated by this challenging picture, an alternative view is proposed here to formalize the effect of explicitly non-Gaussian states in the distribution function of polymer networks, and then to devise an NMR-based discrimination criterion. Experimentally, despite the large number of characterization techniques for cross-linked networks (such as inverse gas chromatography, neutron scattering, osmometry, dielectric and mechanical analysis, see e.g. references in (Valentín et al., 2008)), the most exploited remain NMR spectroscopy and equilibrium swelling. Attention will be paid here to hydrogel behaviors, either interesting from the fundamental point of view, where distinct elasticity regimes can occur according to polymer dilution (Gundogan, Okay, & Oppermann, 2004), or for their notable large-strain features (Gong, Katsuyama, Kurokawa, & Osada, 2003; Webber, Creton, Brown, & Gong, 2007). Theoretically, the present work puts forward an intermediate model placing itself between the refinement of affine versus phantom theories and the analysis of Gaussian versus non-Gaussian effects.

It is known in fact that two milestones of polymer elasticity theory, both based on (unentangled) Gaussian statistics in an infinite network with no loose chain ends, are the 'classical' junction affine and phantom models, related respectively to the uppermost and lowermost chain deformation limits. The elastic response of rubber networks and swollen systems is generally believed to be intermediate between such two extremes, with an uncertainty on cross-link densities of  $\approx 40\%$  the phantom-like value (Valentín et al., 2008). In the former, macroscopic and microscopic deformations are assumed to be practically the same, cross-links being fixed in space to positions imposed by the specimen deformation ratio ( $\alpha$ ). Junction points in James and Guth's phantom model are instead unrestricted, only a small fraction of them being anchored to the boundary surface (Burak Erman, 1989) and chains in between being only constrained to the forces they are subjected to (Flory & Erman, 1982). Crosslinks are modeled by holonomic constraints (Eichinger, 2015) to move affinely around the average positions prescribed by the macroscopic deformation (Gedde, 1995) and are roughly confined to the root mean square end-to-end distance of a network strand (Gottlieb, 1982), i.e. much smaller than the contour chain length but large enough to allow an overwhelming majority of possible conformations (Gedde, 1995). Fluctuations in this model are taken to be strain-independent, developing asymmetrically in deformed states and reducing the strain below the value set by the experiment (Mark, 1992). One is therefore left with a chain functionality-dependent (f)non-affine transformation of instantaneous end-to-end distance and of mean gyration radius of elastic chains (Candau et al., 1982). Microscopic deformations, especially in stiff or semiflexible chains, should become non-affine below a certain length scale and/or above a certain deformation degree (Basu et al., 2011; Curro & Mark, 1984).

Despite the affine hypothesis was afterwards discarded for the phantom network, the latter turns out to be still inaccurate (Hild, 1998). Furthermore, as the two theories rely on a number of alike assumptions (e.g. individual chain models with only intramolecular effects and the same network forces (Gedde, 1995), chain vector distribution in undeformed network equal to the single chain's in uncrosslinked bulk Burak Erman (1989)), it is no surprise that both free energy and stress–strain equations are similar, to the point

of concluding that no essential difference between James-Guth's and Flory–Wall's theories would take place (Eichinger, 2015). More rigorous constrained junction theories (Ronchi-Allegra's, Flory–Erman's, Edward's tube, non-affine and slip-link models Ball, Doi, Edwards, and Warner (1981), Erman (2010), Erman and Flory (1982a), Flory and Erman (1982), Mergell and Everaers (2001), Ronca and Allegra (1975), Rubinstein and Panyukov (2002)) describe in detail the dependence of fluctuations on deformations to get the excess free energy in comparison to classical (phantom) theories, where elasticity is only affected by network connectivity, and time averages only transform with the macroscopic deformation. Overall, they were able to explain stress–strain data in intermediate extension ranges (say, up to  $\alpha \approx 2$ ), when fluctuations are far from being suppressed and deformation makes cross-links more mobile (Gedde, 1995). On the contrary, for a network subject to small deformations or high junction interpenetration, crosslinks are strongly hindered, their instantaneous position well approximating the affinity condition to the external strain (Gottlieb, 1982; Neai & Roland, 1994).

As the role of chain vector distributions is exceptionally important here, a number of non-Gaussian network models were proposed to refine the theoretical predictions (see e.g. the overview in (Elfas-Zúñiga, 2006)). The Gaussian distribution only corresponds to the first linear term in the force–extension relation for a single polymer chain (Treloar, 1973), it neither matches (very) short chains nor the limit of high enough elongations (e.g.  $\alpha > 3$  (Gedde, 1995)), when the mechanical response displays marked upturns (Burak Erman, 1989; Elfas-Zúñiga & Beatty, 2002). A problem is it does not fall to zero at the contour length scale (Treloar, 1973), though an explanation in terms of limited extensibility then was discredited. Experimental workers detected modulus upturns in natural rubbers only in networks undergoing strain-induced crystallization at high elongations (Mark, 1992). Another issue is in the monomer number between two cross-links, often  $\leq 10^2$ , chains being not long enough to be regarded in the Gaussian limit (Huang et al., 2002). Polymer scientists were traditionally employing analytical and semi-heuristic models, with expanded or perturbed Gaussian distributions (e.g. Fixman and Alben (1973)), or combining finite chain extensibility with entanglement effects (e.g. tube models Erman (2010)), rotational isomeric state models (Mark & Curro, 1983) and computations of short-chain distributions (Curro & Mark, 1984). Again, it should be remarked that the agreement achieved by numerical simulations of non-Gaussian systems may be only qualitative (Menduina, Freire, Llorente, & Vilgis, 1986).

To the best of the authors' knowledge, this is the first time a non-Gaussian statistics is used *in explicit form* in a rubber-like elasticity theory. In Treloar's words (Treloar, 1975) "Unfortunately the attempt to replace the Gaussian statistical theory by a more exact treatment involves a considerable sacrifice of both simplicity and generality. ... The treatment of this problem in a rigorous manner presents formidable mathematical difficulties." However, the final equations we obtain are quite simple and lend themselves to a prompt check. To do so, a strategy relying on Low-Field NMR is proposed to pseudo-experimentally infer the end-to-end distribution in real hydrogels. In this paper, we applied it to alginate, agar and scleroglucan hydrogels, that is, three examples of amply used materials for biomedical use and drug release (Matricardi, Alhaique, & Coviello, 2016). It is important to remind the non-Gaussian character we refer to is not associated to a polymeric network approaching its extensibility limit (upon swelling), a condition that requires adopting the inverse Langevin's function (or more conveniently some approximation of it, as proposed by Warner (Bird, Armstrong, & Hassager, 1990)) to model the swelling equilibrium (Coviello, Grassi, Rambone, & Alhaique, 2001). Our focus on the contrary is on the possibility that, just after crosslinking as well, the end-to-end chain distribution function does not follow a Gaussian behavior, this being still one of the main limitations of Flory's theory, as it was further emphasized quite recently (Richbourg & Peppas, 2020).

The distributions chosen here as candidates for the network states of interest are Laplace's, Cauchy's and Poisson's. They have the two-fold purpose of formally mimicking the normal law but deviating from it to a quantitative extent that can be regarded not only perturbative (see next Fig. 1). The former, in fact, was formulated by Laplace some years before the 'second law of errors' (i.e. the Gaussian) and takes place in a wealthy of stochastic applications, like modeling sizes of sand particles, diamonds and beans (Kotz, Kozubowski, & Podgorski, 2001). From a technical viewpoint, in a similar way as to Lindeberg & Feller's central limit theorem (Feller, 1991), it is shown that a suitably normalized geometric sum of independent random variables converges in law to Laplace's even though they are not identically distributed (Toda, 2011). Poisson's law represents the asymptotic regime of phenomena like waiting times, extremes, quasi-stationary distributions and rare events (Peköz & Röllin, 2011). Mathematically, this turned out to be the toughest distribution, but here it was also necessary to complete and discuss in more detail the statistical mechanics picture raised by Laplace's law. Getting explicit bounds on the error of the exponential limit may be notably difficult as well (Aldous, 1989). In between, the broad-tailed Cauchy's law (or Cauchy & Lorentz') is part of the extended family of Lévy or stable distributions. It does not possess a generating function, thence is an exception to the wealthy of laws belonging to the attraction domain of the central limit theorem, which only requires the first two moments to be finite. In spite of this anomaly, it keeps a central place in a number of physical and chemical topics, such as Ornstein & Zernike's theory of critical opalescence (Ornstein & Zernike, 1914), the lifetime broadening of spectral lines (Thorne, 1988) and Lorentz' model for the complex electric permittivity (Fox, 2001).

As a short outline, Sections 2–4 of the paper deal with the statistical mechanics derivation of the theory whereas, in the second part, the focus is shifted on a Low-Field NMR-based approach for deriving the realistic end-to-end distribution function in hydrogels. An analysis of the model outputs in light of experimental data is conducted in Section 6. In developing the theory, instead, we will stick to the conceptual route (and notations) devised by Flory in Chapters (X-XI) of his seminal book (Flory, 1953), aiming to a generalization to polymer networks which are not ideal.

# 2. Network entropy function

### 2.1. General formulation and link to mechanics

The analysis hereby presented is in line to the statistical mechanics tradition developed from the beginning until recently, which assumes the work of deformation (i.e. the strain energy density *U* (Dietmar & Thomas, 2011)) to be proportional to the change

of entropy (*S*) on stretching the chains from the undeformed state. For an isotropic and incompressible hyperelastic material, the principal Cauchy stress components ( $\sigma_{\nu}$ ) then stem from *U* as (Beatty, 2003):

$$\sigma_k = \alpha_k \frac{dU}{d\alpha_k} + p_{_H} \qquad \text{(no sum over repeated indices)} \tag{1}$$

 $\alpha_k$  here denoting the principal elongation stretches (often also referred to as  $\lambda_k$ ) and *U* being symmetric functions of  $\alpha_k$ . The hydrostatic pressure term  $(p_H)$  comes from the incompressibility or constant volume condition (i.e. the Jacobian J = 1 in the next Eq. (7)), since it is no longer determined by the strain energy density and needs to be added explicitly as a constraint on *U*. Evidently, any difference between two principal stresses:

$$\sigma_j - \sigma_i = \alpha_j \frac{dU}{d\alpha_j} - \alpha_i \frac{dU}{d\alpha_i}$$
(2)

cancels out the effect of *p*. Eq. (2) then may undergo the fundamental conditions of mechanics, such as Baker–Ericksen inequalities,  $(\alpha_j - \alpha_i)(\sigma_j - \sigma_i) > 0$  ( $j \neq i$ ), postulating the larger principal stress to always establish along the direction of the larger principal stretch (Baker & Ericksen, 1954; Wilber & Criscione, 2005). A fascinating aspect of rubber elasticity is that a complex deformation curve can be rebuilt up by means of a mesoscopic analysis, in which the random arrangement of monomer units (in an elastomer or in a gel) is modeled by a given statistical mechanics approach. The relationship between randomness and mechanical response ultimately form the subject of the present investigation, the entropy function representing the key property that needs to be in focus. When enthalpic terms may be ignored, the statistical thermodynamics function connecting Eq. (1) to the thermally driven state of a random network is Helmholtz free energy F = -TS (T = absolute temperature) per unit referential volume ( $V_0$ ). If entropy refers to a single chain, the number density of crosslinked strands (e.g.  $n^*$ ) can be employed to tackle a polymer network (Arruda & Boyce, 1993; Huang, 2014; Rubinstein & Colby, 2003):

$$U\left(\{\alpha_k\}\right) = \frac{F}{V_0}\left(\{\alpha_k\}\right) = -n^*TS\left(\{\alpha_k\}\right)$$
(3)

Contributions from interchain interactions are basically thermodynamic and not expected to take any role in elastic free energy calculations. Therefore, despite the main emphasis is given here to the elastic part of the entropy function, the reader may remember that any statistical point of view on the network will correspond to a given strain energy density (for a survey of phenomenological constitutive equations in rubber-like materials see e.g. Destrade, Saccomandi, and Sgura (2017), Puglisi and Saccomandi (2016)). Whenever non-negligible heat transfers may develop, F is ceasing however to be fully representative of the network behavior.

With this in mind, our starting point is Flory's entropy decomposition into a configuration and an ideal gas contributions, that is, in Boltzmann's constant unit  $(k_n)$ :

$$\ln \Omega = \ln \Omega_1 + \ln \Omega_2 \tag{4}$$

where  $\Omega$  and  $\Omega_k$  denote the respective partition functions (sums over microstates) with  $S = \ln \Omega$  and  $S_k = \ln \Omega_k$ . What will matter is clearly the entropy change upon deformation, the difference  $\Delta S$  between the initial and final states. In what follows such two terms ( $\Omega_{1,2}$ ) will be given a separate account, making the customary assumption to deal with different overlaps of conformational domains, extensibility, steric and connectivity effects (Hermans, 1962) in terms of three explicitly non-Gaussian statistics. While the Gaussian distribution alone cannot account for conformational differences between unlike types of polymeric chains, it is known that stress–strain behaviors can be affected by the chain structure even in very small deformation limits (Mark & Curro, 1983). Swelling networks then can display large macroscopic deformation with no meaningful change of chain dimensions, this behavior being tough to be translated in the language of classical theories (Candau et al., 1982).

Note again that, as Flory–Rehner's hypothesis assumes the free energy to be additive, Eq. (4) does not include interaction and liquid-like terms, elastic contributions are the only ones depending on deformation (Flory & Rehner, 1943). The independence of spatial configurations of intermolecular interactions was thoroughly tested, especially by neutron scattering experiments in undiluted amorphous polymers and classical rubbers, where steric interactions are short-ranged and force fields are weak (see e.g. (Mark, 1992) and references therein) but was afterwards criticized by a number of authors (Baek & Srinivasa, 2004; Ball & Edwards, 1980; Edwards & Vilgis, 1988; Sommer, Vilgis, & Heinrich, 1994; Vilgis & Wilder, 1998). However, while an inquiry into Flory–Renher's hypothesis falls outside the aim of the present study, classical or perturbed rubber elasticity models still find a wealthy of applications, including the hydrogel systems that will form the subjects of our investigation (Chan & Neufeld, 2009; Koetting, Peters, Steichen, & Peppas, 2015). Also the thorny relation between statistical mechanics and continuum theory (Eichinger, 2015) as well as explicit concentration effects on fluctuations of cross-link points (Candau et al., 1982) will not be accounted here for. Finally, in the spirit of a milestone work on non-Gaussian effects (James & Guth, 1943; Treloar, 1973), the affinity assumption will be retained in the next elaboration of extension-force relationships (James & Guth, 1943; Treloar, 1973). The perfect gas entropy term in Eq. (4) will then be generalized in compliance with the conformational statistics, yielding a hybrid model that is able to retrieve the phantom limit behavior by means of local or microscopic elasticity constraints.

In conclusion to this section, to further clarify our central aim, this work stems from a doubt that may have often been quelled over the years. Is it permissible that, for some micro- or meso-structural reasons, presumably related to physical chemistry or topology of monomer strands, the architecture of a polymeric network may be (explicitly) non-Gaussian also in undeformed conditions ? Theoretical approaches generally involving the inverse Langevin function (e.g. eight-chain and full network models) have already been known for decades to catch the stress–strain curve at large deformations due to the finite extensibility of polymer chains (Arruda & Boyce, 1993; Bechir, Chevalier, & Idjeri, 2010; Wu & van der Giessen, 1992). Our point of view here is rather

different. What would happen to the mechanical response once the Gaussian hypothesis were somehow relaxed, or even dropped, near enough the low stretch regime ? The present exploratory inquiry tries to open up a debate on this quest, nonetheless taking care to provide an adequate theoretical background and a thorough experimental verification to the ideas hereby presented.

## 2.2. Configuration term

The first entropic term quantifies the statistical mechanics effects of the distribution function for the end-to-end chain displacement in the deformed state,  $W = W(\mathbf{r})$ :

$$\frac{1}{v}\ln\Omega_1 = \ln \mathbf{J} + \int_{\Re^3} W(\mathbf{R})\ln\frac{W(\mathbf{r})}{W(\mathbf{R})} d\mathbf{R}$$
(5)

where v is the number of crosslinked strands, taken to be homogeneously distributed in the sample (Beatty, 2003). By this density of probability, the local chain strain at the mesoscopic level is transferred to the macroscopic scale of the contiguous particle-system (i.e. the continuum) hosting the process. For an undeformed system, undergoing a material point transformation in the stretched state,  $\mathbf{R} \rightarrow \mathbf{r}$ , the scalar quantity:

$$\mathbf{J} = \left\| \frac{\partial \mathbf{r}}{\partial \mathbf{R}} \right\| \tag{6}$$

is the Jacobian determinant of the deformation gradient  $\mathbf{F} = (\partial \mathbf{r}/\partial \mathbf{R})$  (or, simply, the gradient of  $\mathbf{r}$ ). This mapping is generally assumed to be a one-to-one and smooth function (for a rigorous introduction to these concepts, see e.g. Beatty (1987)). The image ( $d\mathbf{r}$ ) of a tangent element to an undeformed material line ( $d\mathbf{R}$ ), pointing out the separation vector between two materials points in the reference state, then is set univocally by  $d\mathbf{r} = \mathbf{F}d\mathbf{R}$ , irrespective of the deformation gradient decomposition into pure stretch and rotation tensors. The square of the local change in separation distances stems from the related right and left Cauchy–Green's deformation tensors, e.g.  $d\mathbf{r}^2 = d\mathbf{R} \cdot \mathbf{C} \cdot d\mathbf{R}$  with  $\mathbf{C} = \mathbf{F}^T \mathbf{F}$  (right tensor). We will not enter details of deformation tensors in the following as, to our purposes, it will suffice to represent undeformed and stretched configurations in Cartesian coordinates (Flory, 1953) with respect to an orthonormal basis { $\mathbf{e}_k$ }, and set  $X_i = x_i/\alpha_i$ , i.e.:

$$\mathbf{J} = \prod_{i} \alpha_{i} \quad , \tag{7}$$

 $x_i = \mathbf{e}_i \cdot \mathbf{r}$  being the transformed coordinates of  $X_i = \mathbf{e}_i \cdot \mathbf{R}$ , while  $\alpha_i \equiv \alpha_x, \alpha_y, \alpha_z$  are the positive elongation coefficients or extension ratios, characterizing a pure homogeneous deformation gradient.

The term  $\Omega_1$  is only affected by the statistics of polymer molecules forming the elastic medium. In order to detect some meaningful variation from classical results, the conditions of the central limit theorem should be somehow violated. It is well known, in fact, that the Gaussian distribution,  $W_n(\mathbf{r}) = (\beta/\sqrt{\pi})^3 \exp(-\beta^2 \mathbf{r}^2)$ , leads to:

$$\frac{1}{v}\ln\Omega_{1n} = -\frac{1}{2}\sum_{i}\alpha_{i}^{2} + \frac{3}{2} + \ln \mathbf{J}$$
(8)

in which the constant  $\beta^2 = 3/(2Nl^2)$  is only influenced by intrinsic polymer properties such as Kuhn's segment length *l* and monomer unit number *N* (i.e. the chain displacement length). The above quadratic expression in  $\alpha_i$  may be deemed as the signature of the ideal behavior. Clearly, if the probability density is no longer Gaussian,  $\ln \Omega_i / v$  could sensibly deviate from Eq. (8). This is shown in Appendix A–Appendix B, reporting the calculations for three even and continuous distribution functions that monotonically decrease in  $|x_i| \in [0, \infty)$ . To this aim, we factorize *W* with respect to each coordinate:

$$W(\mathbf{r}) = \prod W_i(x_i) \tag{9}$$

and make use of the following property:

$$\int_{\Re^3} W(\mathbf{R}) \ln \frac{W(\mathbf{r})}{W(\mathbf{R})} \, d\mathbf{R} = \mathbf{J}^{-1} \sum_{i \neq r \neq s} \alpha_r \alpha_s \bar{\mathbf{I}}_i \tag{10}$$

with:

$$\bar{\mathbf{I}}_{i} = \int_{-\infty}^{\infty} W_{i}(X_{i}) \ln \frac{W_{i}(x_{i})}{W_{i}(X_{i})} dx_{i}$$
(11)

being a reduced configuration integral. Therefore, as:

$$\int_{\Re^3} W(\mathbf{R}) \ln \frac{W(\mathbf{r})}{W(\mathbf{R})} \, d\mathbf{R} = \sum_i \frac{\bar{\mathbf{l}}_i}{\alpha_i} \quad , \tag{12}$$

one can redefine:

$$\bar{\mathbf{I}}_{i}(\alpha_{i};W_{i}) \equiv \int_{-\infty}^{\infty} W_{i}(X_{i}) \ln W_{i}(x_{i}) \, dx_{i} + \mathbf{c}_{i} \alpha_{i}$$
(13)

$$c_i \equiv -\int_{-\infty}^{\infty} W_i(s) \ln W_i(s) \, ds \quad , \tag{14}$$

and observe the most important (elastic) contribution to  $S_1 = \ln \Omega_1$ , the one genuinely linked to the deformation, arises from the first term on the right side of:

$$\int_{\Re^3} W(\mathbf{R}) \ln \frac{W(\mathbf{r})}{W(\mathbf{R})} d\mathbf{R} = \sum_i \mathbf{I}_i + \mathbf{c}_i$$
(15)

i.e. from the sum of reduced integrals like:

$$I_i(\alpha_i; W_i) = \int_{-\infty}^{\infty} W_i(t) \ln W_i(\alpha_i t) dt \quad ,$$
(16)

whereby:

$$\mathbf{I}_i(1; \mathbf{W}_i) = -\mathbf{c}_i \tag{17}$$

stands for an entropic constant, representative of the undeformed state. As the mechanical response that will be inquired in an isothermal system stems from entropy variations, whenever the configuration integral is too complicated or does not admit an explicit solution, one may start directly from the derivatives  $\partial I_i / \partial \alpha_i$ . Obviously, the values for a Gaussian network:

$$I_{in} + c_{in} = -\frac{1}{2} \left( \alpha_i^2 - 1 \right)$$
(18)

are recovered by setting  $W_{in} \equiv W_n(x_i)$  in Eq. (15). In the other cases, the first configuration integrals, recalculated in Appendix A-Appendix B for three meaningful statistics (Laplace', Cauchy', Poisson's), give us:

$$\frac{1}{\nu} \ln \Omega_{11} = -(\alpha_x + \alpha_y + \alpha_z) + \ln(\alpha_x \alpha_y \alpha_z) + 3 \quad \text{(Laplace)}$$
<sup>(19)</sup>

$$\frac{1}{\nu} \ln \Omega_{1C} = -\ln(1+\alpha_x)^2 - \ln(1+\alpha_y)^2 - \ln(1+\alpha_z)^2 + \ln(\alpha_x \alpha_y \alpha_z) + 6\ln 2 \quad \text{(Cauchy)}$$
(20)

$$\frac{1}{\nu} \ln \Omega_{1P} \approx \frac{1}{\nu} \sum_{i} \ln \Omega_{i,1P} \quad \text{(Poisson)}$$
(21)

where, in the last equation, the sum:

$$\frac{1}{\nu}\ln\Omega_{i,1P} = -(\ln\lambda_i)^2\alpha_i \ \Xi_{\lambda_i}[1] + (\ln\alpha_i)(\ln\lambda_i) \ \Xi_{\lambda_i}\left[t^{-1}\right] + (\ln\lambda_i) \ \Xi_{\lambda_i}\left[t^{-1}\ln\Gamma(\alpha_i t)\right] + \text{const.}$$
(22)

applies to a continuous Poisson's density (Ilienko, 2013) with parameters approaching the exponential regime ( $\lambda_i \ll 1$ ), and:

$$\Xi_{\lambda}\left[g\right] \equiv \int_{0}^{\infty} g(t) \,\frac{\lambda^{t}}{\Gamma(t)} \,dt \tag{23}$$

is a functional based on the gamma function ( $\Gamma$ ). A comparison among Eq. (19), Eq. (20) and (21), which quantify the configuration entropy function per polymer strand  $S_{1}/v$ , is reported in the section on results and discussion.

### 2.3. Perfect gas term

We recast here the combinatorial procedure leading to (the controversial) Flory's logarithmic contribution to the total entropy function. Despite James and Guth criticized it harshly, the theoretical view they put forward as an alternative would be devoid of a realistic unstressed state whether a log-term were neglected or absent (Eichinger, 2015; Hild, 1998). Ronca and Allegra made the point it should appear instead in the free energy every time macroscopic deformation and junction fluctuations couple to a non-negligible extent (Ronca & Allegra, 1975).

Second Flory's contribution stems from the likelihood of finding all crosslinked units coupled throughout a network with volume  $V_0$  that deforms to  $V = JV_0$ . We may begin from regarding the probability to find any of the (adjacent) v units in an elementary (small) volume  $\delta v$ , regarded to be intrinsically constant. Adopting the framework of Bernoulli's trials, at a given step *m*, such a probability can be written as:

$$P_{\nu m} = \begin{pmatrix} \varphi_{\nu m} \\ 1 \end{pmatrix} p \ q^{\varphi_{\nu m} - 1}$$
(24)

with  $\varphi_{vm} = v - 2 m + 1$  and  $p = 1 - q = \frac{\delta v}{V}$ . As  $p \ll 1$ , then:

$$P_{\nu m} \approx \varphi_{\nu m} \frac{\delta \upsilon}{JV_0}$$
(25)

and the number of states associated with this process in an ideal network is:

$$\Omega_{2n} = \prod_{m=1}^{\frac{\nu}{2}} P_{\nu m} \approx \left(\frac{\nu}{2}\right)! \left(\frac{2\delta \nu}{JV_0}\right)^{\frac{\nu}{2}}$$
(26)

in which  $\left(\frac{v}{2}\right)! \equiv (v-1)(v-3) \dots 1$ . The final calculation follows from application of Stirling's formula under  $v \gg 1$ :

$$\frac{1}{2}\ln\Omega_{\rm p} \approx -\frac{1}{2}\ln J + \text{const.}$$
(27)

We note that  $\delta v$  is an indivisible, 'pointwise' volume, totally unaffected by chain configurations near interlinking sites. So long as the experiment is isochoric, Eq. (27) has no effect. However, based on our strategy to effectively compare different statistics, a generalization of the perfect gas term is necessary to account for the involved probability density at the junction scale, allowing crosslink points to fluctuate accordingly. In the discrete process  $\Omega_2$ , the functional form  $W = W(\mathbf{r})$  thus will be regarded by means of a new perturbation term. Precisely, we reformulate  $\delta v/V$  as the likelihood that two network points belong for simplicity to a rectangular neighborhood with volume  $\delta V = \prod_i \delta x_i$  (i = x, y, z):

$$p = \prod_{i} \int_{-\frac{\delta x_{i}}{2}}^{\frac{\delta x_{i}}{2}} W_{i}(u) \, du \tag{28}$$

and factorize it so to separate the contribution connected to  $\delta V$ , which now identifies the new probability to work with  $(p \rightarrow P)$ , from its coordinate-dependent part. Calculus of probability may be framed still in the context of Bernoulli's trials, but this time with *P* in place of *p*, and with:

$$\Pi_{\nu m} = \begin{pmatrix} \varphi_{\nu m} \\ 1 \end{pmatrix} P \left(1 - P\right)^{\varphi_{\nu m} - 1} \approx \varphi_{\nu m} P \tag{29}$$

in place of  $P_{vm}$ . Mathematically speaking, the equation  $p(P) = \delta v/V$  now requires to be inverted, with *P* denoting a generalization of *p* in terms of  $\delta x_i$  (> 0). These calculations are carried out in Appendix C, where Flory's result turns out to be perturbed as follows (d = L, C, P):

$$\ln \Omega_{\gamma_d} \approx \ln \Omega_{\gamma_d} + \ln \omega_{\gamma_d} \tag{30}$$

where  $S_{2d} = \ln \Omega_{2d}$  is the recalculated perfect gas entropy function,  $S_{2n} = \ln \Omega_{2n}$  is Flory's result and the second sum over states on the right is a perturbation of statistical nature. One therefore obtains, minus some additive constant:

$$\frac{1}{\nu} \ln \omega_{2L} = \xi_L \sum_i \alpha_i^{-1} \quad \text{(Laplace)}$$
(31)

$$\frac{1}{v} \ln \omega_{2C} = \xi_C \sum \alpha_i^{-2} \quad \text{(Cauchy)}$$
(32)

$$\frac{1}{v}\ln\omega_{2P} = \xi_P \sum_{i}^{i} \alpha_i^{-1} \quad \text{(Poisson)}$$
(33)

The coefficients  $\xi_d \ge 0$  couple the elementary volume scale, characteristic of crosslink fluctuations, to the background elastic medium. A behavior of Cauchy's type is found as well for the Gaussian distribution,  $\omega_{2n} \approx \omega_{2c}$ , while Laplace's and Poisson's coupling terms turn out to coincide in the exponential limit and generally fulfill  $\xi_i \le \xi_p$  (Appendix C).

### 3. Notes on strain energy and invariants

In Section 2.1 it was shortly recalled that the Helmholtz free energy is the key concept to relate strain energy to the entropy function. A question thus arises of which formal representations may be induced in all generality by the statistical mechanics pictures in the former paragraphs. As a detailed analysis of constitutive laws in invariant tensor form would take us too far from the central aims of this study, we will limit ourselves to discussing the strain energy density for the present cases  $(U_j; j = n, L, C, P)$ . We therefore suppose to deal with hyperelastic (or Green elastic) elastomers, and there exists a function  $U = U(\{\alpha_k\})$  so that the stress power per unit referential volume descends from its material derivative. For simplicity, and uniformity with the previous analysis, the Cartesian notation k = x, y, z is retained in what follows, though it could promptly be extended to any system of principal axes, say  $k \rightarrow k' = 1, 2, 3$ . Then we know that for an isotropic sample,  $U = U(\mathbf{F}) \equiv U[I_i(\mathbf{C}), I_{iii}(\mathbf{C})]$ , where:

$$I_i(\mathbf{C}) = \operatorname{Tr}(\mathbf{C}) = \alpha_x^2 + \alpha_y^2 + \alpha_z^2 \tag{34}$$

$$I_{ii}(\mathbf{C}) = \frac{1}{2} \left[ \text{Tr}^2(\mathbf{C}) - \text{Tr}(\mathbf{C}^2) \right] = \alpha_x^2 \alpha_y^2 + \alpha_y^2 \alpha_z^2 + \alpha_z^2 \alpha_x^2$$
(35)

$$I_{iii}(\mathbf{C}) = \text{Det}(\mathbf{C}) \equiv \mathbf{J}^2 = \alpha_x^2 \alpha_y^2 \alpha_z^2$$
(36)

are the linear, quadratic and cubic principal invariants of the Cauchy–Green right tensor (Spencer, 1971), expressed on the right in terms of principal stretches. The incompressibility constraint reduces the strain energy dependence to  $U = U[I_i(\mathbf{C}), I_{ii}(\mathbf{C})]$ , for the Cauchy stress tensor reads:

$$\mathbf{T} = -p_{H}\mathbf{I} + 2\left(\frac{\partial U}{\partial I_{i}} + I_{i}\frac{\partial U}{\partial I_{ii}}\right)\mathbf{B} - 2\frac{\partial U}{\partial I_{ii}}\mathbf{B}^{2}$$
(37)

where **I** and **B** = **FF**<sup>*T*</sup> are respectively the identity and Cauchy–Green left (or Finger's) tensors, the latter owing the same eigenvalues and principal invariants of **C** (Amabili, 2018). Eq. (37) stems from the three-fold dependence of *U* upon J = Det(**F**) = 1 and  $-2J(\partial U/\partial I_{iii}) = p_{H}$ . Once the energy is explicited in terms of  $\alpha_k$ , it clearly identifies a symmetric function of principal stretches, moreover, the principal Cauchy stress components get back to Eq. (1).

In summary, mechanical models are in a way complementary to mesoscopic approaches. To capture the stress–stretch relation in homogeneous and isotropic (dry or swollen) elastomers, a free energy law can be set as a function of strain tensor invariants, and a number of advanced models with highly complicated energy behaviors were put forward with a number of phenomenological coefficients making up for the knowledge at the molecular level (Hossain & Steinmann, 2013; Mihai & Goriely, 2017). However, no one could ever rule out that different energy functions, provided with the same parameters, may predict the mechanical response equally well (Okumura, Kondo, & Ohno, 2016).

With this in mind, let us consider which strain energy forms turn out to be suggested by the found entropy functions. To this end, it suffices referring to the configurational Eqs. (18)–(22) complemented by the perfect gas Eqs. (30)–(33), which bring to Eqs. (52)–(55) of the next Section 4.1. Fundamental aspects of constitutive theories, mostly mathematical in nature (e.g. when quadratic form energies are positive definite in linear elasticity theory, or polyconvexity constraints apply in nonlinear regimes) will not be dealt with hereinafter, although they are reported to be often bypassed by the same scientists working in the field (Puglisi & Saccomandi, 2016). Our Gaussian response, modified by the small scale perturbation, points out the following dependence on the strain invariants:

$$\frac{1}{\nu}\ln\Omega_{n} = -\frac{1}{2}I_{i} + \frac{1}{2}\ln\sqrt{I_{iii}} + \xi_{n}\frac{I_{ii}}{I_{iii}}$$
(38)

thence, the strain energy form induced by an isochoric process is generally of the Mooney & Rivlin type (Mooney, 1940):

$$U_{n}(I_{i}, I_{ii}) = C_{1}\left(I_{i} - I_{i}^{*}\right) + C_{2}\left(I_{ii} - I_{ii}^{*}\right)$$
(39)

the asterisk denoting the values taken in the undeformed state,  $I_i^* = I_{ii}^* = 3$ , the phenomenological constants  $C_1$  and  $C_2$  being two material coefficients whose mechanical meaning is to be adjusted afterwards the best fit to experimental data (Puglisi & Saccomandi, 2016), with  $C_2$  taking potentially negative values as well (Mihai, Woolley, & Goriely, 2019). When  $\xi_n = 0$ , the constitutive law becomes neo-Hookean ( $C_2 = 0$ ) and  $2C_1$  identifies the classical shear modulus (Amabili, 2018). It is interesting to note that, in the compressible case ( $I_{iii} \neq 1$ ), the ratio  $I_{ii}/I_{iii}$  appears in Blatz & Ko model, proposed for a class of (isotropic) foam rubber materials (Blatz & Ko, 1962).

The other statistical mechanics views are somewhat more complicated, but may be expressed in terms of  $I_V = \sum_i \alpha_i$  and  $I_{VV} = \sum_i 1/\alpha_i$ , functions of principal stretches characterizing Varga's model (Hill & Arrigo, 1995; Varga, 1966):

$$U_{V}(I_{i}, I_{iii}, I_{iii}) = C_{1}(I_{V} - I_{V}^{*}) + C_{2}\sqrt{I_{iii}} (I_{1/V} - I_{1/V}^{*})$$
(40)

with reference values  $I_V^* = I_{1/V}^* = 3$  and, generally:

$$I_{iii}I_{1/V}^2 = I_{ii} + 2\sqrt{I_{iii}}I_V = \frac{1}{2}(I_V^2 - I_i)^2$$
(41)

Accordingly, in an isochoric transformation, the strain energy density in Laplace's statistics is of Varga's type:

$$U_{L}(I_{i}, I_{ii}) = U_{V}(I_{V}, I_{1/V})$$
(42)

A square root dependence on the quadratic invariant,  $I_{1/V} = (I_{ii} + 2I_V)^{\frac{1}{2}}$ , takes place in Carroll's model for vulcanized rubbers (Carroll, 2011). Strain functions  $I_V$ ,  $I_{1/V}$  are also met in Cauchy's and Poisson's statistics. The implicit relation to be regarded in the former is:

$$\prod_{i} (1 + \alpha_{i}) = \sqrt{I_{iii}} (I_{1/V} + 1) + I_{V} + 1$$
(43)

so that:

$$U_{C}(I_{i}, I_{ii}) = C_{1} \ln(I_{V} + I_{1/V} - I_{C}^{*}) + C_{2}(I_{ii} - I_{ii}^{*})$$
(44)

with  $I_c^* = 6$ . A logarithmic behavior is classically found in Gent models for limited chain extensibility (Gent, 1996). Poisson's statistics display instead a constitutive law like:

$$U_{p}(I_{i}, I_{ii}) = U_{i}(I_{v}, I_{1/v}) + u_{p}$$
(45)

where  $u_p$  is highly nonlinear, as it depends on the Gamma function, and is hardly expressible in terms of strain invariants straight away. For the moment, a most convenient way to focus on this behavior is to frame it between former Laplace's and a general Ogden model (see e.g. Ogden and Hill (1972)), being:

$$u_{p}(I_{i}, I_{ii}, I_{iii}) = \sum_{kqh} O_{kqh}(I_{i} - I_{i}^{*})^{k}(I_{ii} - I_{ii}^{*})^{q}(I_{iii} - I_{iii}^{*})^{h}$$
(46)

for some tensor **O** of materials coefficients, and upon the isochoric constraint  $I_{iii} = I_{iii}^* = 1$ . Concluding this section, we may remark that all such constitutive relations point towards a necessary dependence on the second strain invariant  $I_{ii}$ , as it was also emphasized

by other authors (Anssari-Benam, Bucchi, & Saccomandi, 2021). The perturbation to the perfect gas term, likely the most affected by network details at the junction scale (i.e. chemical functionality, topology, etc.), breaks the neo-Hookean symmetry even in the (modified) Gaussian-like statistics. Except for this case, however, strain energy laws in the other incompressible rubber-like models are not separable functions of  $I_i$  and  $I_{ii}$ , and seem to display a more complex behavior. Their analysis may thereby represent an interesting issue left for future work. The matching between phenomenological coefficients and polymeric parameters will be addressed through the experimental and numerical analysis of paragraphs 5 and 6. First we need to evaluate, in the next section, the actual mechanical response in some cases of fundamental interest.

#### 4. Mechanical properties of unswollen and swollen networks

The expressions for  $\ln \Omega$  can be used to obtain the mechanical features (uniaxial and shear stresses,  $\sigma$  and  $\tau$ ; elastic and shear moduli, *E* and *G*) in uniaxial tensile deformation ( $D_{U}$ ) and pure shear deformation ( $D_{S}$ ) experiments. In a swelling phenomenon, the material is characterized by an initial ( $\phi_0$ , before swelling) and a final ( $\phi$ , before deformation) value of polymer volume fraction, the quantity  $Q = \phi_0/\phi$  generalizing the former Jacobian condition, i.e.  $J^2 = \text{Det } \mathbf{C} = (\text{Det } \mathbf{F})^2 = 1$  to:

$$\prod_{i} \alpha_{i} = Q \tag{47}$$

If the initial network is in dry state ( $\phi_0 = 1$ ), the former equation identifies the (equilibrium) swelling ratio in a fully swollen permanent network (Q > 1), where mechanical modulus and osmotic (or mixing) pressure balance each other without disrupting the essential skeletal structure (Flory & Rehner, 1943). Otherwise, provided the polymer chains are not too stiff, nothing forbids to work as well in the shrinking or collapse domain (Q < 1). In either case, we will consider the following deformation geometries, representative of uniaxial (tensile) deformation (D<sub>µ</sub>) and pure shear (D<sub>p</sub>) (Arruda & Boyce, 1993; Flory, 1953):

$$D_{i_{1}}(\alpha_{i}, Q) = \{\alpha_{i} \mid \alpha_{x} \equiv Q^{\frac{1}{3}}\alpha, \ \alpha_{y} = \alpha_{z} = Q^{\frac{1}{3}}\alpha^{-\frac{1}{2}}\}$$
(48)

$$D_{S}(\alpha_{i}, Q) = \{\alpha_{i} \mid Q^{-\frac{1}{3}}\alpha_{x} = Q^{\frac{1}{3}}\alpha_{y}^{-1} \equiv \alpha, \ \alpha_{z} = Q^{\frac{1}{3}}\}$$
(49)

both held at fixed temperature (T) and volume. Stretch components in the previous two definitions define the deformation gradient **F**. We provide now with a separate account of such two mechanical frameworks, grouping the relevant calculations in Appendix D. It should be reminded that, although swelling can induce cavity formations inside spherical elastic matrices (Pence & Tsai, 2006), this possibility is disregarded here as we assume that (uniform) swelling establishes without application of a load. It will be supposed, in other words, that swelling precedes the occurrence of deformation implied by the external load.

#### 4.1. Uniaxial deformation

Consider a state of uniaxial stress (here, in the  $\alpha_x$  direction) and the related homogeneous deformation. The stress component  $\sigma \equiv \sigma_x$  produced by the elastic retraction force stems from differentiating the Helmholtz free energy, and reads (Flory, 1953):

$$\sigma = -\frac{k_B T}{V_0 Q} \left(\frac{\partial \ln \Omega}{\partial \alpha}\right)_{T,V}$$
(50)

where the so-called engineering strain is related to the  $\alpha$  value as  $\epsilon = \alpha - 1$ , and equilibrium Young's modulus in the limit of small deformations is ( $\alpha \approx 1$ ):

$$E \approx \sigma/\epsilon$$
 (51)

In Eq. (50),  $k_B$  is still Boltzmann's constant, *T* the absolute temperature and  $V_0$  the reference volume in which the crosslinking phenomenon occurred. We resume again the complete expressions of the configuration integral deduced in each case, i.e. (minus some additive entropy constant):

$$\frac{1}{\nu} \ln \Omega_L = -(\alpha_x + \alpha_y + \alpha_z) + \frac{1}{2} \ln(\alpha_x \alpha_y \alpha_z) + \xi_L \left( \alpha_x^{-1} + \alpha_y^{-1} + \alpha_z^{-1} \right) \quad \text{(Laplace)}$$
(52)

$$\frac{1}{\nu}\ln\Omega_{c} = -2\ln\left[(1+\alpha_{x})(1+\alpha_{y})(1+\alpha_{z})\right] + \frac{1}{2}\ln(\alpha_{x}\alpha_{y}\alpha_{z}) + \xi_{c}\left(\alpha_{x}^{-2} + \alpha_{y}^{-2} + \alpha_{z}^{-2}\right) \quad \text{(Cauchy)}$$
(53)

$$\frac{1}{\nu}\ln\Omega_{p} \approx -l_{p}\left[\alpha_{x} + \alpha_{y} + \alpha_{z} + \frac{1}{2}\ln(\alpha_{x}\alpha_{y}\alpha_{z})\right] + \sum_{i}\Xi_{\lambda}\left[\frac{\ln\lambda}{t}\ln\Gamma(\alpha_{i}t)\right] + \xi_{p}\left(\alpha_{x}^{-1} + \alpha_{y}^{-1} + \alpha_{z}^{-1}\right)$$
(Poisson) (54)

where, in the last,  $l_p = 1 - \frac{2\ell}{\ln \lambda}$  ( $\ell = 0.577$  is Euler's constant), the sum refers to an isotropic system (see Eq. (22)–(23), Eqs. (B.18)–(B.19)) and its contributions to the mechanical response are worked out in Appendix D. In this framework, ideal polymer networks would obey:

$$\frac{1}{\nu}\ln\Omega_n \approx -\frac{1}{2}\left(\alpha_x^2 + \alpha_y^2 + \alpha_z^2\right) + \frac{1}{2}\ln(\alpha_x\alpha_y\alpha_z) + \xi_n\left(\alpha_x^{-2} + \alpha_y^{-2} + \alpha_z^{-2}\right) \quad \text{(Gauss)}$$
(55)

which gets back to Flory's expression upon  $P \to p(\omega_{2n} \to 1)$  e.g. when the coupling extent 'shrinks' from an interlinking volume to a network point ( $\xi_n \to 0$ ). It is known in fact that mechanical features get normally reduced by larger fluctuations (i.e. with increasing  $\xi_d$ ). Substituting Eqs. (52)–(55) into Eq. (50) yields, upon Eq. (48):

I. Laplace :

$$\sigma_{L} = \frac{1}{3} E_{F} Q^{-\frac{2}{3}} (1 - \alpha^{-\frac{3}{2}}) (1 - \xi_{L} Q^{-\frac{2}{3}} \alpha^{-\frac{1}{2}})$$
(56)

$$E_{L} \approx \frac{1}{3}E_{F}Q^{-\frac{2}{3}}\frac{1-\alpha^{-\frac{3}{2}}}{\alpha-1}(1-\xi_{L}Q^{-\frac{2}{3}}\alpha^{-\frac{1}{2}}) = E_{F}Q^{-\frac{2}{3}}\left[\frac{1}{2}(1-\xi_{L}Q^{-\frac{2}{3}}) + -\frac{5}{8}(1-\frac{7}{5}\xi_{L}Q^{-\frac{2}{3}})(\alpha-1) + \frac{35}{48}(1-\frac{59}{35}\xi_{L}Q^{-\frac{2}{3}})(\alpha-1)^{2} - \dots\right]$$
(57)

II. Cauchy :

$$\sigma_{c} = \frac{2}{3} E_{F} Q^{-\frac{2}{3}} \left[ \frac{1}{1 + Q^{\frac{1}{3}} \alpha} - \frac{1}{\alpha(\sqrt{\alpha} + Q^{\frac{1}{3}})} - \xi_{c} Q^{-1}(1 - \alpha^{-3}) \right]$$
(58)

$$E_{c} \approx \frac{2}{3}E_{F}\left[\frac{Q^{-\frac{2}{3}}}{\alpha-1}\left(\frac{1}{1+Q^{\frac{1}{3}}\alpha}-\frac{1}{\alpha(\sqrt{\alpha}+Q^{\frac{1}{3}})}\right)-\xi_{c}Q^{-\frac{5}{3}}\alpha^{-3}(1+\alpha+\alpha^{2})\right] = E_{F}Q^{-\frac{2}{3}}\left\{\frac{1}{(1+Q^{\frac{1}{3}})^{2}}-2\xi_{c}Q^{-1}-\frac{1}{4}\left[\frac{5+7Q^{\frac{2}{3}}}{(1+Q^{\frac{1}{3}})^{3}}-16\xi_{c}Q^{-1}\right](\alpha-1)+\frac{1}{24}\left[\frac{35+76Q^{\frac{1}{3}}+59Q^{\frac{2}{3}}}{(1+Q^{\frac{1}{3}})^{4}}-160\xi_{c}Q^{-1}\right](\alpha-1)^{2}-\ldots\right\}$$
(59)

III. Poisson :

$$\sigma_{p} \approx \frac{1}{3} E_{F} Q^{-\frac{2}{3}} (1 - \alpha^{-\frac{3}{2}}) (l_{p} - \xi_{p} Q^{-\frac{2}{3}} \alpha^{-\frac{1}{2}})$$
(60)

$$E_{p} \approx \frac{1}{3}E_{F}Q^{-\frac{2}{3}}\frac{1-\alpha^{-\frac{3}{2}}}{\alpha-1}(l_{p}-\xi_{p}Q^{-\frac{2}{3}}\alpha^{-\frac{1}{2}}) = E_{F}Q^{-\frac{2}{3}}[\frac{1}{2}(l_{p}-\xi_{p}Q^{-\frac{2}{3}}) + \frac{5}{8}(l_{p}-\frac{7}{5}\xi_{p}Q^{-\frac{2}{3}})(\alpha-1) + \frac{35}{48}(l_{p}-\frac{59}{35}\xi_{p}Q^{-\frac{2}{3}})(\alpha-1)^{2} - \dots]$$
(61)

the Gaussian results becoming:

$$\alpha \frac{\Delta \sigma_{FQ}}{\sigma_F} = \frac{\Delta E_{FQ}}{E_F} = -2\xi_n Q^{-\frac{4}{3}}$$
(62)

with  $\Delta \sigma_{FQ} = \sigma_{nQ} - \sigma_{FQ}$  and  $\Delta E_{FQ} = E_{nQ} - E_{FQ}$  now denoting the variations between modified and pure Gaussian values. Note that Flory's relations are promptly recovered, i.e.:

$$\frac{\sigma_{FQ}}{\sigma_F} = \frac{E_{FQ}}{E_F} = Q^{-\frac{1}{3}}$$
(63)

where, as usual:

$$\sigma_F = \frac{1}{3} \varepsilon E_F (1 + \alpha^{-1} + \alpha^{-2}) , \qquad (64)$$

and:

$$E_{F} = 3\rho k_{B}T$$
(65)

is Flory's elastic modulus for an unswollen network as a function of the number density of polymer strands,  $\rho = v/V_0$ . As expected, the original expressions for a Gaussian system are regained upon  $\xi_n \to 0$  in Eq. (62).

### 4.2. Pure shear

Analogously to the former subsection, Helmholtz free energy (per unit volume) allows to connect the configuration integral to the shearing stress as well (Flory, 1953):

$$\tau = -\frac{k_B T}{V_0 Q} \left(\frac{\partial \ln \Omega}{\partial \gamma}\right)_{T,V}$$
(66)

and hence to the equilibrium shear modulus in infinitesimal deformations, still related to the slope of stress–strain curve near the zero-strain point ( $\alpha \approx 1$ ):

$$G \approx \tau / \gamma$$
 (67)

As the shear strain can be taken on to be  $\gamma = \alpha - 1/\alpha$  (Flory, 1953), the expressions generated by Eqs. (52)–(54) under Eq. (49) now are:

I. Laplace :

$$\tau_L = G_F Q^{-\frac{2}{3}} \frac{\alpha^2 - 1}{\alpha^2 + 1} (1 - \xi_L Q^{-\frac{2}{3}})$$
(68)

$$G_{L} \approx G_{F} Q^{-\frac{2}{3}} \frac{\alpha}{\alpha^{2} + 1} (1 - \xi_{L} Q^{-\frac{2}{3}}) = G_{F} Q^{-\frac{2}{3}} (1 - \xi_{L} Q^{-\frac{2}{3}}) \left[ \frac{1}{2} - \frac{1}{4} (\alpha - 1)^{2} + \dots \right]$$
(69)

II. Cauchy:

$$\tau_{c} = 2G_{F}Q^{-\frac{2}{3}} \left[ \frac{\alpha^{2}}{1+\alpha^{2}} \left( \frac{1}{Q^{\frac{1}{3}}\alpha+1} - \frac{1}{\alpha(Q^{\frac{1}{3}}+\alpha)} \right) - \xi_{c}Q^{-1}\gamma(\alpha) \right]$$
(70)

$$G_{C} \approx 2G_{F}Q^{-\frac{2}{3}} \left[ \frac{\alpha^{2}}{(\alpha^{2}+1)(Q^{\frac{1}{3}}+\alpha)(Q^{\frac{1}{3}}\alpha+1)} - \xi_{C}Q^{-1} \right] = G_{F}Q^{-\frac{2}{3}} \left[ \frac{1}{(1+Q^{\frac{1}{3}})^{2}} - 2\xi_{C}Q^{-1} - \frac{1}{2} \frac{1+4Q^{\frac{1}{3}}+Q^{\frac{2}{3}}}{(1+Q^{\frac{1}{3}})^{4}} (\alpha-1)^{2} + \dots \right]$$
(71)

III. Poisson :

$$\tau_{p} = G_{F} Q^{-\frac{2}{3}} \frac{\alpha^{2} - 1}{\alpha^{2} + 1} (l_{p} - \xi_{p} Q^{-\frac{2}{3}})$$
(72)

$$G_{p} \approx G_{F} Q^{-\frac{2}{3}} \frac{\alpha}{\alpha^{2} + 1} (l_{p} - \xi_{p} Q^{-\frac{2}{3}}) = G_{F} Q^{-\frac{2}{3}} (l_{p} - \xi_{p} Q^{-\frac{2}{3}}) \left[ \frac{1}{2} - \frac{1}{4} (\alpha - 1)^{2} + \dots \right]$$
(73)

where, with similar notations to Eq. (62), the relationships:

$$\frac{\Delta \tau_F}{\tau_{FO}} = \frac{\Delta G_F}{G_{FO}} = -2\xi_n Q^{-\frac{4}{3}}$$
(74)

$$\frac{\tau_{FQ}}{\tau_{F}} = \frac{G_{FQ}}{G_{F}} = Q^{-\frac{1}{3}}$$
(75)

still represent modified Flory's predictions for a swollen Gaussian network, with:

$$\tau_F = G_F \gamma \tag{76}$$

$$G_F = \frac{1}{3}E_F = \rho k_B T \tag{77}$$

Again, unperturbed results can be retrieved upon  $\xi_n \to 0$  in Eqs. (74).

## 4.3. Theoretical remarks

Fig. 1 reports a sketchy relationship among Gaussian, Cauchy's and exponential-like distributions in one dimension, the last category including Laplace's and Poisson's. Three main regions for the polymer end-to-end distance can be crudely identified, delimited for simplicity by the probability axis and two vertical dashed lines. In comparison with the Gaussian, polymer ends in Cauchy's and exponential chains tend to be more spaced out both at small and intermediate length scales. At small scales, exponential distributions stand for the most repulsive of the three classes, Cauchy's taking their place in the halfway region. Quite the contrary, the likelihood to find two Gaussian ends at larger distances is the least, whereas Cauchy's chains display the largest attraction. The specific way by which such mutual statistical weights (or chain interactions) may emerge falls outside the aim of this study. What matters here is to point out that, whenever the polymer network could be driven outside the Gaussian state, it would still be possible to resort to a consistent and fairly applicable framework. Different mechanical responses than Flory's then can be sensed and analyzed at the experimental level.

Accordingly, expressing the previous results in units of  $\sigma_F$  or  $E_F$  quantifies at once the discrepancies one would get from adopting the other statistics in place of the Gaussian's. Laplace's and Poisson's predictions differ as expected by the coefficient  $l_p = 1 - 2\ell/\ln \lambda > 1$ , determined in isotropic materials ( $\lambda_i \equiv \lambda$ ) at second order in the exponential regime (see Appendices B and

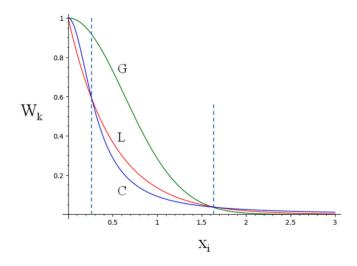


Fig. 1. Gaussian (G, green), Cauchy's (C, blue), Laplace's (L, red) end-to-end distribution functions with zero average and normalized in one dimension to  $W_k(x_k = 0) = 1$ . As being a statistics of exponential type, Poisson's should be regarded in this scheme as to fall into the L category.

D). Since  $\lambda \approx (1.25 \cdot 10^{-1} \div 5) \cdot 10^{-2}$  implies  $l_p \approx (1.15 \div 1.4)$ , Poisson-like moduli would be approximately  $\approx (20 \div 40)$  % larger than the corresponding exponential values.

The terms  $\xi_d$  are proportional to a mean coupling parameter of order *h*, defined in Appendix C as  $\xi_h \approx \frac{1}{3} \sum_i (\delta x_i/x_0)^h$  (h = 2 for Gauss's and Cauchy's statistics, h = 1 for Laplace's and Poisson's). An evaluation of it may be given through relative fluctuation weights (or volume fractions),  $\xi_h \approx (\delta V/V_0)^{h/3}$ , i.e. the portion of space swept out on the average by crosslinked units owing to energy sources and constraints. Scattering experiments showed that cross-links undergo simultaneous translational and orientational diffusion, not dissimilar in magnitude from the chain gyration radius, and connecting its ends on the ns time scale (D. Stein, A. Hoffman, Frank, & D. Fayer, 1992). By neglecting elastic constraints produced by network connections, the variance of junction fluctuations can be derived from the stiffness tensor (Erman & Flory, 1982a). However, Eq. (74) may be used to prompt a relationship with the cycle rank in the phantom model (Rubinstein & Colby, 2003),  $G/G_F = 1-2/f$ , adopted in the following as to set a Gaussian reference state to which normalizing any other phenomenological coefficient. In a perfect network, with f/2 strands per crosslink, it evaluates the difference between the numbers of elastically effective strands and crosslinks, and is believed to be suitable especially for diluted systems (e.g. gels). In our case, confronting Eq. (74) with it identifies:

$$\xi_n = \frac{Q_n^2}{f} \tag{78}$$

and, correspondingly:

$$\xi_{L} = \sqrt{3/(2\pi f)} Q^{\frac{2}{3}}$$
(Laplace) (79)  
$$\xi_{C} = \xi_{n}$$
(Cauchy) (80)  
$$\xi_{P} = I_{P}\xi_{L}$$
(Poisson) (81)

In imperfect networks, cycle rank should take the influence of dangling chains and loops into account. Network defects, however, are not going to be examined here, nor chain dimension ratios or front factors. Conceptually, they do not lead to significant changes of classical theories (e.g., Flory's (Eichinger, 2015)) and would not alter the conclusions we will come to later.

### 5. Materials and methods

The three hydrogels studied, based on alginate, agar and scleroglucan, find a wide spreading in biomedical field for their peculiar properties such as biocompatibility and giving rise to strong and weak hydrogels in mild conditions (Matricardi et al., 2016). Alginate is a collective term to describe a family of polysaccharides isolated from brown seaweeds and bacteria (Donati & Paoletti, 2009). Chemically, alginates are linear copolymers of  $1 \rightarrow 4$  linked  $\beta$ -d-mannuronic acid (MM) and its C–5 epimer,  $\alpha$ -l-guluronic acid (GG), arranged in a blockwise pattern, with homopolymeric regions of MM- and GG residues, indicated as MM-blocks and GG-blocks, respectively, and interspersed with regions of alternating structure (MG blocks). The ability to form stable physical hydrogels upon treatment with divalent ions, such as calcium's (Draget, Smidsrød, & Skjåk-Bræk, 2005), have resulted in alginates being widely used in industrial and biomedical applications. For example, they have been used for encapsulation of insulin-producing Langerhans islets for treatment of type I diabetes (de Vos et al., 2009) and as drug delivery systems (Matricardi, Meo, Coviello, Hennink, & Alhaique, 2013). The higher the GG content, the stiffer and more fragile is the gel they form in water in presence of divalent cations. Alginate

used in this paper (molecular weight  $\approx 10^6$  Da), a kind gift from FMC Biopolymer Ltd, UK, was characterized by a high GG content ( $\approx 70\%$  GG and 30% MM). In order to prepare the hydrogel, a proper amount of alginate powder was slowly added to stirred distilled water contained in a beaker at room temperature up to forming a homogeneous solution (alginate mass fraction 0.02; % mass fraction = 2%). A proper amount of alginate solution then was poured into a bottom flat beaker to get a film of thickness  $\approx 1$  mm. Subsequently, a CaCl<sub>2</sub> water solution (Ca<sup>2+</sup> concentration = 5 g/l) was rapidly sprayed on the gel surface to promote alginate crosslinking (volume of sprayed crosslinking solution was approximately equal to the gel volume). After 5 min of contact, the solution was removed and the crosslinked film was immediately and gently cleaned by laboratory paper. Upon formation, the gel was cut into 35 mm diameter disks (thickness  $\approx 1$  mm) by means of a stainless-steel punch with the same diameter of the rheometer sensor. In case of LF-NMR tests, the gel was cut into  $\approx 8$  mm diameter disks ( $\approx 1$  mm thick) and put inside the LF-NMR glass tube.

Agar is a gel forming polysaccharide with a main chain consisting of alternating 1.3-linked  $\beta$ -D-galactopyranose and 1.4linked 3.6 anhydro- $\alpha$ -L-galactopyranose units (Arnott et al., 1974). It is composed by agarose and agaropectin (Labropoulos, Niesz, Danforth, & Kevrekidis, 2002). Agarose is a neutral polysaccharide and represents the fraction with gelling capacity while agaropectin contains the charged polysaccharide components. Agarose and agaropectin contents depend on the seaweed source which agar is extracted from and affects physicochemical, mechanical and rheological properties of the gels (Labropoulos et al., 2002). It has been suggested that the agarose network arises from double helix formation and subsequent aggregation into bundles. called suprahelices (Djabourov, Clark, Rowlands, & Ross-Murphy, 1989; Labropoulos et al., 2002). However, according to molecular modeling studies (Kouwijzer & Pérez, 1998), agarose appears to be capable of creating both single- and double-helical structures, which are left-handed and antiparallel-packed. As expected for a gel-forming polysaccharide, all of the proposed crystal structures show enough available space (30–45%) for water molecules. The agar considered in this paper (molecular weight  $\approx 1.2 \cdot 10^5$  Da). supplied by Biokar (Diagnostics, France), was of alimentary grade, i.e. essentially composed by agarose. Agar gel was realized by dissolving 1 g of polymer into 99 g of distilled water at 90° C, so that the polymer mass fraction in final gels was 0.01 (% mass fraction = 1%). The solution was homogenized and poured into proper vessels to allow gelation due to cooling at room temperature. For rheological characterization, the vessel used was a cylinder  $\approx 2$  mm thick with a diameter of  $\approx 50$  mm. Again, the formed gel was cut into 35 mm diameter disks by means of a stainless-steel punch with the same diameter of the rheometer sensor. About NMR tests, the solution was poured directly inside the LF-NMR glass tube.

Scleroglucan is a nonionic polysaccharide secreted exocellularly by fungi of genus Sclerotium. Its primary structure consists of a linear backbone of (1,3)- $\beta$ -linked d-glucopyranosyl residues bearing a single (1,6)- $\beta$ -linked d-glucopyranosyl unit every three sugar residues of the main chain (Rinaudo & Vincendon, 1982). Both in aqueous solution and the solid state, scleroglucan adopts a highly ordered, rigid, triple helical tertiary structure (triplex), which consists of three individual strands composed by six residues in the backbone per turn. The three triplex strands are held together by inter-strand H-bonds at the center of the triplex. The  $(1 \rightarrow 6)$ -linked  $\beta$ -d-glucopyranosyl side groups protrude from outside the triplex, preventing intermolecular aggregation and polymer precipitation (Bluhm, Deslandes, Marchessault, Pérez, & Rinaudo, 1982; Fariña, Sineriz, Molina, & Perotti, 2001; Palleschi, Bocchinfuso, Coviello, & Alhaique, 2005). Triplex conformation is destabilized only in dimethyl sulfoxide or strong alkaline conditions, and characterized by a high rigidity, responsible for the peculiar properties exhibited by aqueous scleroglucan solutions in a wide pH range and even at relatively high temperatures. As triplex clustering increases, the formation of three-dimensional hydrogel networks takes place (this happens, typically, for a polymer mass fraction (Grassi, Lapasin, & Pricl, 1996)  $\geq 0.0025$ ). Owing to its rheological properties, scleroglucan is used as thickener and suspending agent in several industrial sectors (Lapasin & Pricl, 1995). In addition, as it is biocompatible, biodegradable and bio-adhesive, it is widely used in cosmetics and pharmaceutics fields, its main application being the release of bioactive molecules (Coviello, Grassi, Lapasin, Marino, & Alhaique, 2003; Grassi et al., 2009; Matricardi, Onorati, Coviello, & Alhaique, 2006; Viñarta, François, Daraio, Figueroa, & Fariña, 2007). Scleroglucan used in this study (Actigum CS11) was provided by Cargill (Minneapolis, MN, USA) and characterized by an average molecular weight of  $1.2 \cdot 10^6$  Da. The hydrogel (polymer mass fraction 0.02; 2%) was prepared by gradually adding the polymer powder to distilled water under mechanical stirring at room temperature. Just after preparation, the system was kept in fridge at temperature of 8 °C for 24 h in order to promote the gel formation. The weak gel nature allowed to easily put it in the rheometer sensor and LF-NMR glass tube by the aid of a spatula.

## 5.1. Low-field NMR

The end-to-end distribution, of the polymeric network pervading the studied hydrogels, was determined by means of Low-Field NMR, looking at the magnetic relaxation of hydrogen units of water molecules trapped in the network. Information on the network architecture (mesh size distribution) thus was gained indirectly by recording the effect of polymeric chains (the solid hydrogel component) on magnetically relaxing water hydrogens. Because of the very fast process, magnetic relaxation of hydrogen units of polymer chains did not affect our measurements.

Water protons relaxation time  $T_2$  was measured by means of a Bruker Minispec mq20 (0.47 T, 20 MHz, Germany) at 25 °C resorting to the CPMG (Carr–Purcell–Meiboom–Gill) (Meiboom & Gill, 1958) sequence  $\{90^\circ[-\tau-180^\circ - \tau(echo)]_n-T_R\}$  with a 8.36 µs wide 90° pulse,  $\tau = 250$  µs,  $T_R = 10$  s (sequence repetition rate), *n* being the number of detected experimental intensities. The criterion to deem the relaxation process over and choose the value of *n* was to wait for the FID (Free Induction Decay) intensity reaching about 2% of its initial value. Each relaxation experiment, composed by *n* points, was repeated 36 times (four scans each of 9 repetitions performed). The continuous  $T_2$  distribution was determined by fitting the experimental FID ( $I_s(t)$ ) by the following equation (Whittall & MacKay, 1989):

$$I(t) = \int_{T_{2\min}}^{T_{2\max}} a(T_2) \exp\left(-\frac{t}{T_2}\right) dT_2$$
(82)

where  $T_{2max}$  and  $T_{2min}$  indicate, respectively, the smallest and largest values of the continuous  $T_2$  distribution,  $a(T_2)$  is the unknown amplitude of the spectral component at relaxation time  $T_2$ , while  $\exp(-t/T_2)$  represents the decay term. In order to fit Eq. (82) to the experimental FID ( $I_s(t)$ ) and get the continuous  $T_2$  distribution ( $A_i$  vs  $T_{2i}$ ), the following discretization scheme was adopted (Whittall & MacKay, 1989):

$$I(t) \approx \sum_{i=1}^{N} a_i \exp\left(-t/T_2^i\right) \left(T_2^{i+1} - T_2^i\right) = \sum_{i=1}^{N} A_i \exp\left(-t/T_2^i\right)$$
(83)

where the range of the  $T_2$  distribution ( $T_{2min} - T_{2max}$ ) was logarithmically subdivided into N = 200 parts (larger N values were proven to be unnecessary).

Because of some noise disturbing the measure of  $I_s$ , the fitting procedure must not minimize the  $\chi^2$  statistics, but a smoothed definition (Whittall & MacKay, 1989) of it ( $\chi_s^2$ ):

$$\chi_{s}^{2} = \sum_{i=1}^{N} \left( \frac{I_{s}(t_{i}) - I(t_{i})}{s_{i}} \right)^{2} + \mu \sum_{i=1}^{N-2} |A_{i+2} - 2A_{i+1} + A_{i}|^{2}$$
(84)

where  $\sigma_i$  is the i<sup>th</sup> datum standard deviation, and  $\mu$  is weighting the smoothing term as proposed by Provencher (Provencher, 1982). Although different criteria can be followed for determining  $\mu$ , we adopted the strategy proposed by Wang (Wang & Ni, 2003), according to which the correct value is pointed out just below the heel (slope variation) of the plot  $\ln \chi_s$  vs  $\ln \mu$ .

The continuous  $T_2$  profile can be transformed into hydrogel mesh size distribution by resorting to the Fiber-Cell (Chui, Phillips, & McCarthy, 1995) and Scherer theories (Scherer, 1994). To this purpose, it was recently demonstrated that, for a hydrogel polymer volume fraction  $\phi < 0.61$ , the average mesh size  $\zeta$  deriving from the Scherer theory can be properly approximated by (Abrami et al., 2018):

$$\zeta = R_f \sqrt{\frac{C_1}{C_0} \left(\frac{1 - 0.58\phi}{\phi}\right)}$$
(85)

where  $R_f$  is the radius of the polymeric chain (imagined to be a long cylinder), while  $C_1$  and  $C_0$  are two constants depending on the mesh architecture which for a cubic mesh are equal, respectively, to 1 and  $3\pi$ . In light of Eq. (85), the Fiber-Cell theory (Chui et al., 1995) leads to the following relation between  $\zeta$  and the average value of the reciprocal of relaxation time  $(1/T_2)_m$ :

$$\left(\frac{1}{T_2}\right)_{\rm m} = \frac{1}{T_{2\rm H2O}} + \frac{2\mathcal{M}}{\zeta\sqrt{\frac{C_0}{C_1}\left(\frac{1-0.58\phi}{\phi}\right)}}$$

$$\left(\frac{1}{T_2}\right)_{\rm m} = \sum_{i=1}^{\rm N} \frac{A_i}{T_{2i}}$$
(86)
(87)

in which  $T_{2H2O}$  is the bulk proton relaxation time (i.e. the water proton relaxation time in the absence of polymer, the so-called free water relaxation time  $\approx$  3000 ms at 25 °C and 0.47 T) (Coviello et al., 2013) and  $\mathcal{M}$  (length/time) is the 'relaxivity', a parameter accounting for the surface effect of polymer chains on water proton relaxation. In fact,  $\mathcal{M}$  is the ratio between thickness and relaxation time of the bound water layer adhering to the solid surface (Chui et al., 1995). While Eq. (86) holds, on average, for all the polymeric network meshes, similar expressions can be written for meshes of different dimensions ( $\zeta_i$ ) by assuming  $\mathcal{M}$  to be independent of the mesh size (Chui et al., 1995):

$$\frac{1}{T_{2i}} = \frac{1}{T_{2H2O}} + \frac{2\mathcal{M}}{\zeta_i \sqrt{\frac{C_0}{C_1} \left(\frac{1-0.58\phi}{\phi}\right)}}$$
(88)

 $T_{2i}$  being the relaxation time of water protons trapped in polymer meshes of size  $\zeta_i$ . The bi-univocal correspondence between  $T_{2i}$  and  $\zeta_i$  only holds in the fast-diffusion regime, i.e when mobility of water molecules, expressed by their self-diffusion coefficient (Holz, Heil, & Sacco, 2000) D (2.09  $\cdot$  10<sup>-9</sup> m<sup>2</sup>/s at 25 °C), is large as compared to the rate of magnetization loss, identifiable with  $R_c \mathcal{M}$  (i.e.  $R_c \mathcal{M}/D \ll 1$ ). In fact in the slow diffusion regime, relaxation of all water protons contained in the volume of a mesh of size  $\zeta_i$  is not described by only one  $T_{2i}$  but a multiplicity of  $T_{2i}$ .  $R_c$ , indicating the radial distance from polymer chain axis at which the effect of polymeric chains on water proton relaxation gets negligible, can be expressed by (Chui et al., 1995):

$$R_{c} = \frac{R_{f}}{\sqrt{\phi}}$$
(89)

The combination of Eqs. (86) and (88) allows to conclude that the ratio between  $\zeta_i$  and its maximum value,  $\zeta_{max}$ , is influenced exclusively by the relaxation times  $T_{2i}$  and  $T_{2max}$  (apart from the free water relaxation time  $T_{2H2O}$ ):

$$\zeta_{i}^{+} = \frac{\zeta_{i}}{\zeta_{max}} = \frac{\left(\frac{1}{T_{2max}} - \frac{1}{T_{2H2O}}\right)}{\left(\frac{1}{T_{2i}} - \frac{1}{T_{2H2O}}\right)}$$
(90)

Thus, as Eq. (90) yields a way to convert relaxation times into mesh size, it does not require the knowledge of the two parameters  $R_f$  and  $\phi$ , whose determination is not always straightforward. Accordingly, the probability  $P_i(\zeta_i^+)$  of finding a mesh of size  $\zeta_i^+$  inside

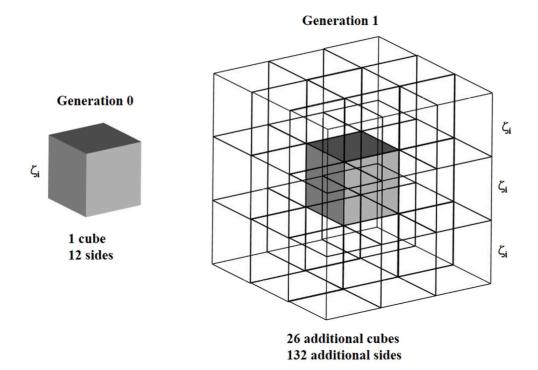


Fig. 2. The polymeric network is generated by covering the 'seed cube' (generation 0, size  $\zeta_i$ ) by other identical cubes (generation 1). This covering process, repeated up to generation  $n_i$ , gives rise to a polymeric network with cubic mesh size  $\zeta_i$ .

<b>Table 1</b> Geometric characteristics of a network after $n_i$ generations.					
Generation	Additional cubes	Additional sides			
0	1	12			
1	26	132			
2	$26 \cdot 3^3$	132 .3			
3	$26.3^{6}$	$132 \cdot 3^2$			
n.	$26 \cdot 3^{3(n_i-1)}$	$132 \cdot 3^{(n_i-1)}$			

the polymer network writes:

$$A_{i}(\zeta_{i}^{+}) = A_{i}(T_{2i}), \quad P_{i}(\zeta_{i}^{+}) = \frac{A_{i}(\zeta_{i}^{+})}{\sum_{i=1}^{N} A_{i}(\zeta_{i}^{+})}$$
(91)

where coefficients  $A_i(T_{2i})$  are known from Eq. (83) fitting the experimental relaxation data.

## 5.2. End-to-end size distribution

Starting from the distribution of cubic meshes in Eqs. (90)–(91), it is possible determining the end-to-end size distribution, i.e. the distribution of vectors moduli representing the length (end-to-end distance) of polymer segments extending from a fixed crosslink to the next one along a given primary polymer molecule. To this aim, though other structures may be certainly regarded, let us assume in accord with Eq. (85) that polymer meshes are cubical and the entire network can be generated equivalently by "covering" the "seed cubic mesh" of size  $\zeta_i$  (generation 0; see Fig. 2) by other cubic meshes of size  $\zeta_i$  (generation 1). Whilst generation 1 requires considering further 26 cubes (3<sup>3</sup> cubes minus the seed cube), the number of new cube sides are not 26 · 12, as further cubes share several sides, and it is easy to verify the additional sides are only 132. In order to further expand the network, we can repeat such an operation by covering the cubic structure of size  $\zeta_i$  by other 26 cubes of size  $\zeta_i$  (generation 2) and so on, up to generation  $n_i$ . Accordingly, the number of additional cubes and sides at generation 2, 3, ...  $n_i$  are those indicated in Table 1.

Considering that a real network is not composed by meshes of identical size  $\zeta_i$  but, more realistically, it comprises different meshes with sizes spanning from  $\zeta_1$  to  $\zeta_N$  ( $\zeta_1 < \zeta_2 < ... < \zeta_N$ ), we assume it to come from summing the meshes of all dimensions. On the basis of the discussion reported in Appendix E, it can be demonstrated that the fraction of meshes ( $F_{Mi}$ ) and sides ( $F_{Si}$ ) of

size  $\zeta_i$  are related to the probability  $P_i(\zeta_i^+)$  (Eq. (91)) of finding a mesh of size  $\zeta_i^+$  in the polymeric network by:

$$F_{Mi}\% = \frac{P_i}{\sum_{i=1}^{N} P_i}$$

$$F_{Si} = \frac{\sqrt[3]{P_i}}{\sum_{i=1}^{N} \sqrt[3]{P_i}}$$
(92)
(93)

In conclusion, Eq. (93) allows to convert the mesh size distribution, as determined by LF-NMR characterization in Eq. (90), into the end-to-end size distribution, as required by the rubber elasticity theory.

## 5.3. Rheology

Rheological measurements were performed at 25 °C by a stress controlled rotational rheometer (Haake Mars Rheometer, 379-0200 Thermo Electron GmbH, Karlsruhe, Germany) equipped with parallel plate geometry (PP35, diameter = 35 mm, with serrated surfaces to avoid slippage at the wall) and a gap of  $\approx (1 \div 2)$  mm. The measuring device was kept inside a glass bell at saturated humidity conditions to avoid evaporation effects. In order to assess the shear modulus (*G*) dependence on shearing deformation ( $\gamma$ ), stress sweep tests, led at 1 Hz, were performed on each hydrogel. This dependence is given by Eq. (67), where both shear deformation and stress ( $\tau$ ) were experimentally determined.

#### 6. Results and discussion

#### 6.1. Small deformations

It seems reasonable starting the theoretical comparison among the original Flory theory and the results derived in this paper by focusing the three end-to-end distance distributions (i.e. Poisson, Laplace, Cauchy) in the limit of small shear deformations. Fig. 3 shows the trend of the ratio between the new shear moduli (*G*, from Poisson's, Laplace's, Cauchy's statistics) and Flory's (*G<sub>F</sub>*, Eq. (77)) versus the swelling (Q > 1) or shrinking (Q < 1) ratio. This comparison was performed by assuming vanishing shear deformations, a high functionality value (f = 45) and the same crosslink density in crosslinking conditions (Q = 1; reference state). It can be seen that the ratio *G*/*G<sub>F</sub>* (see Eq. (69), (71), (73)) decreases with increasing Q whatever the considered distribution is. Moreover, with Laplace's and Cauchy's statistics, one always has *G*/*G<sub>F</sub>* < 1.

On the contrary, when  $Q \le 0.2$ , Poisson's distribution yields a ratio > 1. It is important to underline that a similar behavior is found for smaller *f*, even though the Cauchy distribution provides with physically consistent results in the whole Q domain when crosslink fluctuations are rather small (large *f* values). In addition, owing to the small deformation hypotheses (E = 3G, see also Eq. (77)), all the above considerations hold with uniaxial deformations as well. Finally, it is interesting recalling that the results shown in Fig. 3 can be seen from a different viewpoint that is closer to the polymeric network architecture. In light of the equivalent network theory (Schurz, 1991), it is possible indeed transforming the results in Fig. 3 in terms of the average network mesh size:

$$\zeta = \sqrt[3]{\frac{6}{\pi N_{\rm A} \rho_{\rm x}}} \tag{94}$$

 $N_A$  being Avogadro's number and  $\rho_x$  being the molar crosslink density (crosslink moles per unit volume). Eq. (94) implies:

$$\frac{\zeta_{\rm k}}{\zeta_{\rm F}} = \sqrt[3]{\frac{\rho_{xF}}{\rho_{\rm xk}}} \tag{95}$$

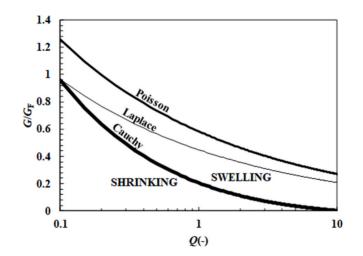
where  $\rho_{xF}$  and  $\rho_{xk}$  indicate, respectively, the crosslink density in original Flory's work and those in Laplace's, Cauchy's and Poisson's distributions, while  $\zeta_F$  and  $\zeta_k$  similarly denote the average mesh size descending from Flory's and the new statistical distributions. As the ratio  $\rho_{xF}/\rho_{xk}$  does not depend on Q,  $\zeta_k/\zeta_F$  is always equal to 0.765, 0.590 and 0.835, respectively (taking on  $l_p = 1.3$ , see Theoretical Remarks). Adopting non-Gaussian statistics therefore reduces the average value of mesh size, at least in the cases hereby regarded.

#### 6.2. Large deformations

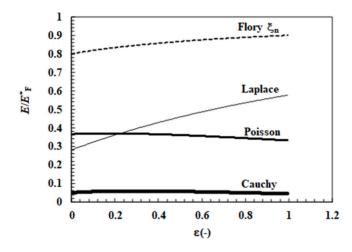
With large deformations, one of the most interesting aspects is the dependencies of Young's and shear moduli on uniaxial ( $\varepsilon$ ) and pure shear ( $\gamma$ ) deformations, respectively. To this purpose, it is worth remembering that in the original Flory theory  $G_F$  does not depend on  $\gamma$  while the elastic modulus decreases with  $\varepsilon$ . Combining Eqs. (64) and (65) and remembering that  $\rho_x = \rho/N_A$ , one explicitly has:

$$E_{\rm F}^* = RT \rho_{\rm xF} Q^{-\frac{1}{3}} \left[ 1 + \frac{1}{\varepsilon + 1} + \frac{1}{(\varepsilon + 1)^2} \right]$$
(96)

It is interesting to study the trend of  $E/E_F^*$  and  $G/G_F$  versus deformation for the three distributions here considered plus the one coming from the modified Flory theory, implemented by the factor  $\zeta_n$  (see Eq. (55)) upon Q = 1 and f = 10. Fig. 4 makes clear



**Fig. 3.** Theoretical comparison amongst the shear modulus descending from the Gaussian theory ( $G_F$ ) and those (*G*) in Eq. (69) (Laplace), Eq. (71) (Cauchy), Eq. (73) (Poisson) in the limit  $\gamma \rightarrow 0$  ( $\alpha \rightarrow 1$ ). It is performed in both shrinking/swelling domains (Q = 1 stands for the crosslink density in the reference state) with a large functionality value (f = 45).



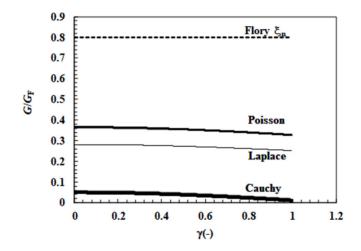
**Fig. 4.** Dependence on the uniaxial deformation ( $\varepsilon$ ) of the ratio  $E/E_F^*$ , between the Young modulus (*E*) implied by the three distributions (Laplace, Eq. (57); Cauchy, Eq. (59); Poisson, Eq. (61)) plus the ones from Flory's theory implemented by the  $\xi_n$  factor (Eq. (55)) and Flory's  $E_F^*$ . Simulations were performed with swelling ratio Q = 1 and network connectivity f = 10.

that whatever  $\varepsilon$ , Young's modulus in Flory's theory is always larger than any other (including the modified Flory's) and the ratio  $E/E_F^*$  does not sensibly depend on  $\varepsilon$  for all distributions except from Laplace's, as it increases with increasing  $\varepsilon$ . For pure shear deformations (Fig. 5), the shear modulus from Flory's theory is always larger than in other distributions, the ratio  $G/G_F$  being almost constant.

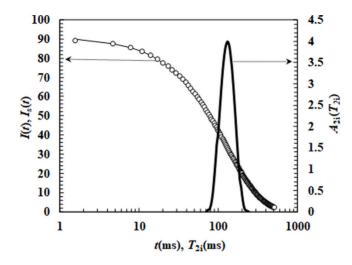
A most important aspect suggested by these non-Gaussian distributions is that shear modulus is affected by  $\gamma$ . This points out a clear generalization of Flory's theory, setting  $E_F^*$  to depend on  $\epsilon$  and  $G_F$  to be  $\gamma$ -independent. Also in these simulations, large junction fluctuations (f < 10) lead Cauchy's distribution to return unrealistic results.

### 6.3. Determination of end-to-end distributions

To derive the end-to-end distribution requires Eq. (83) to be applied to experimental relaxation data ( $I_s(t)$ ), here of agar, alginate and scleroglucan hydrogels as depicted, respectively, in Figs. 6, 7 and 8. This fitting reveals the relaxation time distribution ( $A_{2i}$ ,  $T_{2i}$ ) is characterized by only one peak in agar (Fig. 6) and scleroglucan (Fig. 8) hydrogels, while two main peaks are visible for alginate (Fig. 6). This is simply due to the fact that, after crosslinking, the alginate gel tends to contract by expelling water (syneresis) that accumulates among the hydrogel disks filling the LF-NMR glass tube. The position of the second peak shown in Fig. 7 is very close in fact to the free water relaxation time at 25 °C (3000 ms, 0.47 T) (Coviello et al., 2013). Only the first peak is indicative of water molecules trapped inside the polymer network, this being the reason why the second one will no longer be considered. On the



**Fig. 5.** Dependence on the shearing deformation ( $\gamma$ ) of the ratio  $G/G_F$ , between the shear modulus (*G*) in Eq. (69) (Laplace), Eq. (71) (Cauchy), Eq. (73) (Poisson) and Flory's Eq. (77) ( $G_F$ ). Simulations were performed with a swelling ratio O = 1 and network functionality f = 10.



**Fig. 6.** Best fitting Eq. (83) (I(t), thin solid line: left vertical axis) to experimental relaxation data ( $I_s(t)$ , open circles) of agar hydrogel (smoothing factor  $\mu = 150$ ). Best fit is represented by  $A_i$  vs  $T_{2i}$  relaxation time distribution (thick solid line; right vertical axis).

contrary, the single peak characterizing agar (Fig. 6) and scleroglucan (Fig. 8) time distributions are representative of trapped water molecules, as they are very far from the free water relaxation time. Eqs. (90)–(91) allow us to convert the relaxation time profile ( $A_{2i}$ ,  $T_{2i}$ ) into the mesh size ( $F_{Mi}$ , Eq. (92)) and the end-to-end ( $F_{Si}$ , Eq. (93)) distributions for the agar, alginate and scleroglucan hydrogels (depicted respectively in Figs. 9, 10, 11).  $F_{Mi}$  % and  $F_{Si}$  % represent the percentage probability of finding a mesh or an end-to-end length in the network that equals  $\zeta_i$ , according to Eqs. (92) and (93).

The direct correspondence between relaxation time  $T_{2i}$  and mesh size  $\zeta_i$  is guaranteed by the fast diffusion conditions occurring in our hydrogels. In fact, as the water self-diffusion coefficient at 25 °C is (Holz et al., 2000)  $2.09 \cdot 10^{-9}$  m<sup>2</sup>/s,  $R_f$  typically spans from (Amsden, 1998; Palleschi et al., 2005) 0.5 to 2.2 nm and  $\phi$  is equal to  $6.6 \cdot 10^{-3}$ ,  $5.7 \cdot 10^{-3}$  and  $12.6 \cdot 10^{-3}$  respectively in agar 1% (density = 1520 kg/m<sup>3</sup>) (De'Nobili, Rojas, Abrami, Lapasin, & Grassi, 2015), alginate 1% (density = 1770 kg/m<sup>3</sup>) (Pasut et al., 2008) and scleroglucan 2% (density = 1600 kg/m<sup>3</sup>) (Coviello et al., 2013) hydrogels, then the dimensionless number  $R_c \mathcal{M}/D$ is always  $\ll 1$  ( $\sim 10^{-5} \cdot 10^{-6}$ ). Interestingly, from the Kolmogorov–Smirnov test (Kolmogorov, 1933; Smirnov, 1948) and whatever the gel regarded,  $F_{Si}$ % turns out not to be normally distributed, thus the study of other statistical distributions would be anyway in order. We thus fitted the Gauss, Laplace, Poisson and Cauchy laws with the pseudo-experimental  $F_{Si}$ % profiles for the three systems, as Figs. 12, 13 and 14 show:

$$F_{\rm F}\% = 100 \left(\frac{\beta}{\sqrt{\pi}}\right)^3 e^{-\beta^2 \left(\zeta_{\rm i}^+ - \mu_{\rm a}\right)^2} \Delta \zeta_{\rm i}^+$$

$$F_{\rm I}\% = 50L \ e^{-L|\zeta_{\rm i}^+ - \mu_{\rm a}|} \Delta \zeta^+$$
(97)
(97)
(97)

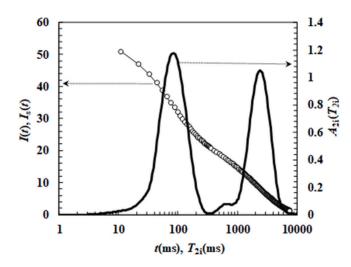


Fig. 7. Best fitting Eq. (83) (I(t)) to experimental relaxation data  $(I_{\mu}(t))$  for alginate hydrogel ( $\mu = 160$ ). Symbols and notations as in Fig. 6.

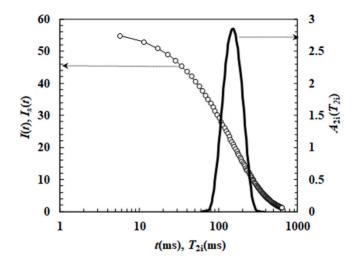


Fig. 8. Best fitting Eq. (83) (I(t)) to experimental relaxation data ( $I_s(t)$ ) for scleroglucan hydrogel ( $\mu = 150$ ). Symbols and notations as in Fig. 6.

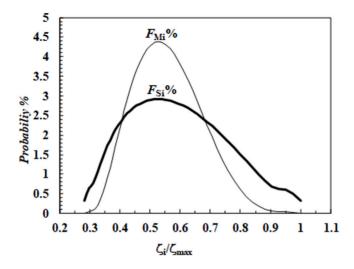


Fig. 9. % mesh size  $(F_{Mi}\%)$  and end-to-end  $(F_{Si\%})$  distributions for agar hydrogel.  $\zeta_i$  and  $\zeta_{max}$  are, respectively, the *i*th mesh size and the maximum mesh size values.

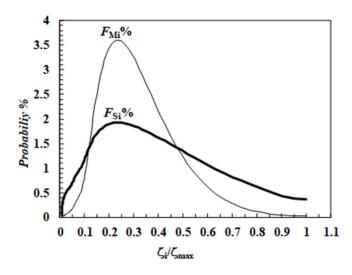


Fig. 10. % mesh size ( $F_{Mi}$ %) and end-to-end ( $F_{Si\%}$ ) distributions for alginate hydrogel. Symbols and notations as in Fig. 9.

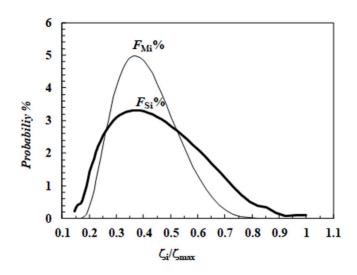


Fig. 11. % mesh size ( $F_{Mi}$ %) and end-to-end ( $F_{Si\%}$ ) distributions for scleroglucan hydrogel. Symbols and notations as in Fig. 9.

$$F_{\rm P}\% = 100 \frac{\lambda^{\zeta_i^+} \ln\left(\frac{1}{\lambda}\right) e^{0.577\zeta_i^+}}{\prod_{k=1}^{\infty} e^{\zeta_i^+/k} / (1+\zeta_i^+/k)} \Delta\zeta_i^+ \qquad 0 < \lambda \ll 1$$
(99)

$$F_{\rm C}\% = 100 \ \frac{C/\pi}{\left(\zeta_{\rm i}^+ - \mu_{\rm a}\right)^2 + {\rm C}^2} \Delta\zeta_{\rm i}^+ \tag{100}$$

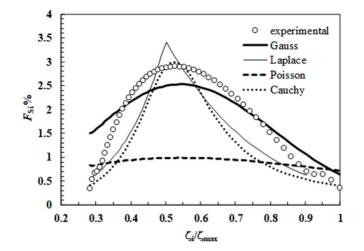
where  $\zeta_i^+ = \zeta_i/\zeta_{max}$  is a dimensionless end-to-end length,  $F_F\%$ ,  $F_L\%$ ,  $F_P\%$ ,  $F_C\%$  are the % probability of finding in the network an end-to-end distance within  $\zeta_i^+$  and  $\zeta_i^+ + \Delta \zeta_i^+$ , according to the Gauss (F), Laplace (L), Poisson (P) and Cauchy (C) statistics,  $\mu_a$  denotes the average value while, as in our former notations,  $\beta$ , *L*,  $\lambda$  and *C* are parameters which stem from adopting Gauss, Laplace, Poisson and Cauchy laws. Fig. 12 and Table 2 immediately reveal that, while Poisson's distribution cannot statistically fit  $F_{Si}\%$  data (*F* test failed), every other was able to (*F* test was positive).

In order to statistically point out the best model, Akaike's criterion (Burnham & Anderson, 2004) was adopted, i.e. the model to be preferred will be characterized by the smallest Akaike number (*AIC*):

$$AIC = N \ln\left(\frac{\chi^2}{N}\right) + 2\frac{\left(N_F + 1\right)\left(N - N_F\right)}{N - N_F - 2}$$
(101)

& Alderson, 2004).						
Agar 1% hydrogel (Fig. 12)						
GAUSS	$\beta = 2.34 \pm 0.03$	$\mu_a = 0.37 \pm 0.01$	F(1,51,0.95) < 181	AIC = -86		
LAPLACE	$L = 5.80 \pm 0.31$	$\mu_a = 0.50 \pm 0.01$	F(1,51,0.95) < 113	AIC = -72		
POISSON	-		-	-		
CAUCHY	$C = 0.13 \pm 0.01$	$\mu_a = 0.51 \pm 0.01$	F(1,51,0.95) < 53	AIC = -48		
Alginate 1% hydrogel (Fig. 13)						
GAUSS	$\beta = 2.50 \pm 0.02$	$\mu_a = -0.037 \pm 0.006$	F(1,104,0.95) < 933	AIC = -341		
LAPLACE	$L = 5.15 \pm 0.17$	$\mu_a = 0.154 \pm 0.005$	F(1,104,0.95) < 433	AIC = -270		
POISSON	$\lambda = 0.015 \pm 0.001$		F(1,105,0.95) < 2881	AIC = -526		
CAUCHY	$C = 0.143 \pm 0.007$	$\mu_a  =  0.167  \pm  0.007$	F(1,104,0.95) < 268	AIC = -233		
Scleroglucan 2% hydrogel (Fig. 14)						
GAUSS	$\beta = 2.45 \pm 0.03$	$\mu_a = 0.20 \pm 0.01$	F(1,51,0.95) < 260	AIC = -70		
LAPLACE	$L = 6.36 \pm 0.33$	$\mu_a = 0.34 \pm 0.01$	F(1,51,0.95) < 1995	AIC = -62		
POISSON	-		-	-		
CAUCHY	$C  =  0.118  \pm  0.009$	$\mu_a = 0.35 \pm 0.01$	F(1,51, 0.95) < 107	AIC = -38		

**Table 2** Parameters for all distributions fitting the  $F_{Sl}$ % data shown in Figs. 12, 13 and 14. *AIC* is Akaike's number (Burnham & Anderson 2004)



**Fig. 12.** Best fitting the Gauss, Laplace, Poisson and Cauchy distributions (continuous, dashed and dotted lines) to the pseudo-experimental  $F_{Si}$ % profile (open circles) for the agar hydrogel ( $\zeta_i$  and  $\zeta_{max}$  are, respectively, the *i*th mesh size and maximum mesh size values).

where *N* and  $N_F$  are respectively the numbers of experimental data and fitting parameters,  $\chi^2$  being the sum of squared differences between experimental data and best fit. This criterion would suggest the Gaussian's as the best distribution among those adopted (Table 2).

For the alginate hydrogel (Fig. 13), all of the adopted distributions can better fit the  $F_{Si}$ % data but, on the basis of Akaike's criterion, the best model turns out to be Poissonian. This may also be expected from a visual inspection of Fig. 13 (dashed line). Finally, from Fig. 14 and Table 2, Poisson's statistics turns out to be unsuitable for scleroglucan data (*F*-test failed), whereas amongst the others Akaike's test would select the Gaussian law. However, as for the agar gel, none of the above distributions may be regarded as fully satisfactory (see Fig. 14).

#### 6.4. Determination of the average mesh size

Once the best end-to end distribution is identified for each hydrogel, we can proceed with the analysis of their rheological behaviors via a proper expression for  $G = G(\gamma)$ . In particular, for agar and scleroglucan hydrogels, we have found that the best distribution among those here regarded is Gaussian while, for the alginate, is Poissonian. In the first two cases, however, the Gaussian statistics is not very accurate and in fact *G* does not behave as a constant in an ample  $\gamma$  domain but starts to non-linearly decrease (Fig. 15) at rather low deformation values (scleroglucan 2%,  $\alpha_c \approx 1.03$ ; agar 1%,  $\alpha_c \approx 1.001$ ), where network damaging is unlikely (here v = constant). A lower crosslink density relates in turn with an increase of the average mesh size, as dictated by Eqs. (77) and (94) (Q = 1):

$$\zeta = \sqrt[3]{\frac{6RT}{\pi N_{\rm A}G}}$$
(102)

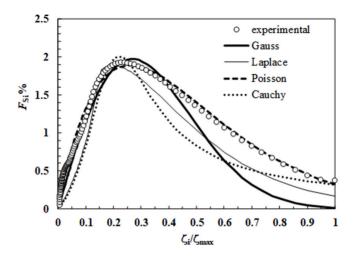


Fig. 13. Best fitting the Gauss, Laplace, Poisson and Cauchy distributions to the pseudo-experimental  $F_{Si}$ % profile for the alginate hydrogel. Symbols and notations as in Fig. 12.

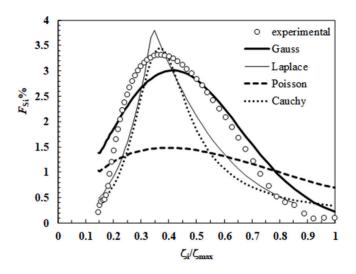


Fig. 14. Best fitting the Gauss, Laplace, Poisson and Cauchy distributions to the pseudo-experimental  $F_{Si}$ % profile for the scleroglucan hydrogel. Symbols and notations as in Fig. 12.

where *R* is the universal gas constant and *T* (= 298.15 K) is absolute temperature. Assuming for *G* in the last equation the average value of the linear part of  $G = G(\gamma)$ , as shown by Fig. 15, ( $\gamma_{max} = 4.1 \cdot 10^{-3}$  for agar,  $\gamma_{max} = 6.2 \cdot 10^{-2}$  for scleroglucan), we get:

$$\rho_{s}^{qgar} = 1.16 \text{ mol/m}^3, \quad \zeta_{agar} = 14 \text{ nm}$$
 (103)

$$\rho_{scl.}^{scl.} = 6 \cdot 10^{-2} \text{ mol/m}^3, \quad \zeta_{scl.} = 38 \text{ nm}$$
 (104)

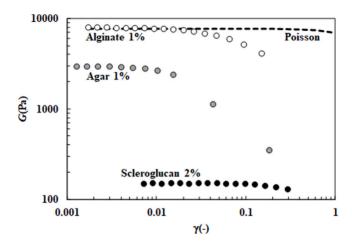
In the alginate case, the  $G(\gamma)$  expression that descends from Poisson's statistics (Eq. (73)) reads:

$$G = RT\rho_x(l_p - \xi_P)\frac{\alpha}{1 + \alpha^2} , \quad \alpha = \frac{1}{2}(\gamma + \sqrt{\gamma^2 + 4})$$
(105)

with  $\xi_{p}$  still given by Eq. (81), and:

$$l_p = 1 - 2\frac{0.577}{\ln\lambda} \tag{106}$$

By setting  $\lambda = 0.015$  (see Table 2) and a wide range of network functionalities, f = (4 - 1000), Eq. (105) was used to fit the dataset in Fig. 15 and deduce the fitting parameter  $\rho_x$ . Eq. (105) works out well for  $\alpha \le \alpha_c$  ( $\approx 1.01$ ; alginate 1%), likely ascribing the recorded non-linearity of  $G = G(\gamma)$  to Poisson's law corrections at larger deformations. This can be proved by limiting Eq. (105) to best fit the linear part of the experimental trend of *G* (dashed line in Fig. 15). The onset of nonlinear behavior foreseen by Eq. (105) occurs



**Fig. 15.** Dependence of shear modulus *G* on shearing deformation  $\gamma$  for the three hydrogels here considered (symbols). Dashed line denotes the *G* = *G* ( $\gamma$ ) trend produced by the Poisson distribution.

in fact at larger deformations,  $\alpha \ge \alpha_c$ . For *f* still varying in the same interval,  $\rho_x$  ranges between 15.8 and 5.1 mol/m<sup>3</sup> and the average mesh size ( $\zeta_{algin}$ ) between 5.8 and 8.5 nm, i.e. a quite moderate effect.

## 7. Conclusions

We studied the influence of explicitly non-Gaussian statistics on elastic properties (Young and shear moduli) of hydrogels, accounting as well for the influence of possible swelling/shrinking processes after crosslinking. An account of such effects in both swollen and unswollen states required a reformulation of the statistical mechanics problem of rubber elasticity, either discussing the configuration integral or the so-called perfect gas term in formally different statistical contexts from the Gaussian's (Laplace', Poisson's, Cauchy's). In the end, the inferred new families of statistical and mechanical laws are reasonably simple for a model comparison, with strain energy densities of Mooney & Rivlin (modified Gaussian statistics) Varga (Laplace's) and Varga & Ogden (Poisson's) types. Cauchy's statistics, on the contrary, seems to put forward a new constitutive law.

Quite predictably, in all the non-Gaussian statistics here adopted, not only Young's but also the shear modulus turns out to depend on deformation, contrarily to the original Gaussian (Flory) model, where shear modulus is insensitive to it. Furthermore, for small deformations and swelling ratios  $Q \ge 1$ , the assumption of non-Gaussian distributions at a constant crosslink density ( $\rho_{x0}$ , crosslink reference state) yields smaller values of Young's and shear moduli than the original Flory's predictions. Only when Q < 1 the Poisson distribution can imply larger moduli. At a fixed Young's or shear modulus, these findings bring to larger estimates of the crosslink density and smaller average values of the network mesh size. In case of large deformations with  $\rho_{x0}$  and f held constant, such quantities result again smaller than Flory's values at whatever deformation.

To define a strategy to thoroughly check the statistical mechanics results and identify the most realistic end-to-end length distribution in the hydrogel network, a theoretical–experimental inquiry based on LF-NMR was developed. For every hydrogel hereby studied (agar 1%; alginate 1%; scleroglucan 2%), statistics should be never regarded as Gaussian (Kolmogorov–Smirnov test). This is interesting as, while it could be generally expected from polymer theory, the Gaussian model still identifies the best distribution function in agar and scleroglucan gels. Quite surprisingly, Poisson's gives instead the best conformational statistics for the alginate hydrogel, especially in the low deformation regime. The possibility to deduce the most probable distribution in light of new statistical mechanics models guides the rheology interpretation by choosing the appropriate model for the mechanical moduli. Here, an onset of non-linear response develops at rather low deformation values, where network breaking remains unlikely (alginate 1%,  $\alpha_c \approx 1.01$ ; scleroglucan 2%,  $\alpha_c \approx 1.03$ ; agar 1%,  $\alpha_c \approx 1.001$ ). Let the number of crossinked strands to vary with the deformation, one should better understand to which extent such experimental deviations may be ascribed to conformational statistics corrections or network damaging. This is an interesting issue left for future work. Alongside, our approach is promising to get the most probable mesh size, that is, the starting point to build up a continuous mesh size distribution of a polymer network. As a final remark, considering the number of increasingly complex polymer systems in the most varied fields of natural and engineering sciences, we hope this study will suggest the rationale and stimulate the search for new hypothesis in the field.

#### Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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## Appendix A

We collect here the calculations of  $\ln \Omega_1$  for three end-to-end probability functions,  $W(\mathbf{r})$ , including their contributions to the mechanical quantities of interest (shear stress  $\tau$  and elastic modulus *G*). They are carried out in accordance with Eqs. (15)–(16) of the theoretical section (Configuration Term).

I. Laplace's density. It is characterized by an exponential distribution of the form:

$$W_{iL}(x_i) = \frac{1}{2}L_i e^{-L_i |x_i|}$$
(A.1)

where  $L_i$  are normalization coefficients, playing the role of materials parameters. As it turns out:

$$I_{iL} + c_{iL} = -\alpha_i + 1, \tag{A.2}$$

Eq. (15) returns the Jacobian trace variation induced by the geometric transform:

$$\int_{\Re^3} W_L(\mathbf{R}) \ln \frac{W_L(\mathbf{r})}{W_L(\mathbf{R})} d\mathbf{R} = 3 - \sum_i \alpha_i$$
(A.3)

implying:

$$\frac{1}{2}\ln\Omega_{yz} = -(\alpha_x + \alpha_y + \alpha_z) + \ln(\alpha_x\alpha_y\alpha_z) + 3 \tag{A.4}$$

II. Cauchy's density. For Cauchy's distributions like:

$$W_{iC}(x_i) = \frac{\chi_i}{\pi \left(x_i^2 + \chi_i^2\right)} \tag{A.5}$$

one gets instead:

$$I_{ic} + c_{ic} = -\ln(1 + \alpha_i)^2 + 2\ln 2$$
(A.6)

and:

$$\frac{1}{v}\ln\Omega_{1C} = -\ln(1+\alpha_x)^2 - \ln(1+\alpha_y)^2 - \ln(1+\alpha_z)^2 + \ln(\alpha_x\alpha_y\alpha_z) + 6\ln2$$
(A.7)

where, again, the intrinsic materials parameters ( $\chi_i$ ) do not play any role here. We remind, despite a resemblance to normal distributions, Cauchy's densities have no moment-generating function (i.e. due to their heavy tails, average value and variance are also undefined).

III. *Poisson's density (continuous)*. Following some technical literature on this subject (see Ilienko (2013) in the main text) consider the probability distribution:

$$F_i^{(+)}(x_i) \equiv \begin{cases} 0 & x_i < 0\\ f_i(x_i) & x_i \ge 0 \end{cases}$$
(A.8)

with:

$$f_i(x_i) \equiv \frac{\Gamma(x_i, \lambda_i)}{\Gamma(x_i)} , \qquad (A.9)$$

where:

$$\Gamma(x_i) = \int_0^\infty t^{x_i - 1} e^{-t} dt$$
(A.10)

$$\Gamma(x_i,\lambda_i) = \int_{\lambda_i}^{\infty} t^{x_i-1} e^{-t} dt$$
(A.11)

are, respectively, gamma and incomplete gamma functions, depending on a parameter  $\lambda_i > 0$ . Eq. (A.8) was introduced to define a continuous analogue of classical Poisson's law for non-negative values of the random variable,  $F_i^{(+)}(x_i) = P\{\mathbf{x}_i \le x_i\}$ . To extend it to the whole real axis, let us introduce:

$$F_i(x_i) = \frac{1}{2} \left[ 1 + F_i^{(+)}(x_i) + F_i^{(-)}(x_i) \right]$$
(A.12)

the odd counterpart being provided by:

$$F_i^{(-)}(x_i) \equiv -F_i^{(+)}(-x_i) .$$
(A.13)

Accordingly  $F_i(0) = \frac{1}{2}$ , and:

$$W_{i}(x_{i}) \equiv \frac{1}{2} \begin{cases} f_{i}'(-x_{i}) & x_{i} < 0\\ f_{i}'(x_{i}) & x_{i} \ge 0 \end{cases}$$
(A.14)

is the Poisson density function to be used in Flory's configuration calculus. To improve its suitability for calculation purposes, observe that:

$$\left\{\frac{\Gamma(x_i,\lambda_i)}{\Gamma(x_i)}\right\}' = -\left\{\frac{\gamma(x_i,\lambda_i)}{\Gamma(x_i)}\right\}'$$
(A.15)

prime denoting differentiation with respect to the independent variable  $(x_i)$ , while:

$$\gamma(x_i,\lambda_i) \equiv \int_0^{\lambda_i} t^{x_i-1} e^{-t} dt = \Gamma(x_i) - \Gamma(x_i,\lambda_i)$$
(A.16)

We now recall two theorems about Gamma-like functions:

$$\Gamma(x_i) = \frac{e^{-\ell x_i}}{x_i} \prod_{k=1}^{\infty} \frac{e^{\frac{x_i}{k}}}{1 + \frac{x_i}{k}}$$
(A.17)

$$\gamma(x_i,\lambda_i) = \frac{\lambda_i^{x_i}}{x_i} \boldsymbol{\Phi}(1, 1 + x_i;\lambda_i) , \qquad (A.18)$$

 $\ell \approx 0.577$  being Euler's constant and  $\Phi$  standing for a confluent hypergeometric function:

$$\boldsymbol{\Phi}(1, 1 + x_i; \lambda_i) = 1 + \frac{\lambda_i}{1 + x_i} + \frac{\lambda_i^2}{(1 + x_i)(2 + x_i)} + \dots$$
(A.19)

and rearrange Eqs. (A.14)-(A.15) so to get:

$$W_{iP}(x_i) = -\frac{1}{2} e^{-\lambda_i} A_1 A_2 A_3 \left[ \ell' + (\ln A_2)' + (\ln A_3)' \right]$$
(A.20)

with:

$$A_{1} = e^{\ell x_{i}}, \quad A_{2} = \prod_{k=1}^{\infty} e^{-\frac{x_{i}}{k}} \left(1 + \frac{x_{i}}{k}\right), \quad A_{3} = \lambda^{x_{i}} \Phi(1, 1 + x_{i}; \lambda_{i})$$
(A.21)

After some developments, the second term in the square parenthesis becomes:

$$(\ln A_2)' = -x_i \sum_{k=1}^{\infty} \frac{1}{k(k+x_i)}$$
(A.22)

being:

$$\sum_{k=1}^{\infty} \frac{1}{k(k+x_i)} = \frac{1}{x_i} \int_0^1 \frac{1-t^{x_i}}{1-t} dt = \frac{1}{x_i} \left[ \psi(x_i+1) - \psi(1) \right] ,$$
(A.23)

in which:

$$\psi(z) \equiv \left[\ln \Gamma(z)\right]' = \psi(1+z) - \frac{1}{z}$$
(A.24)

is the digamma function, and:

$$(\ln A_2)' = -\left[\psi(x_i) + \frac{1}{x_i} + \ell\right] \,. \tag{A.25}$$

 $A_{2}$  can be rewritten by a direct evaluation of the derivative  $\Phi'$ , getting:

$$(\ln A_3)' = \ln \lambda_i - \frac{\lambda_i e^{\lambda_i}}{(1+x_i)^2} \frac{\hat{\boldsymbol{\phi}}}{\boldsymbol{\phi}}$$
(A.26)

where, again,  $\Phi = \Phi(1, 1 + x_i; \lambda_i)$ , while the hypergeometric series at the numerator reads  $\hat{\Phi} = \hat{\Phi}(1 + x_i, 1 + x_i; 2 + x_i, 2 + x_i; -\lambda_i)$ , i.e.:

$$\hat{\Phi} = 1 + \frac{(1+x_i)^2}{(2+x_i)^2} \frac{(-\lambda_i)}{1!} + \frac{(1+x_i)^2}{(3+x_i)^2} \frac{(-\lambda_i)^2}{2!} + \dots$$
(A.27)

Finally, by gathering all calculations and taking into account that  $W_i$  is an even function, the configuration calculus can be carried out in terms of  $\widetilde{W}_{ip} = 2W_{ip}$  over the only positive axis:

$$\widetilde{W}_{iP}(x_i) = \frac{\gamma(x_i,\lambda_i)}{\Gamma(x_i)} \left\{ \psi(x_i+1) + \frac{\lambda_i e^{\lambda_i}}{(1+x_i)^2} \frac{\widehat{\boldsymbol{\phi}}}{\boldsymbol{\phi}} - \ln \lambda_i \right\}$$
(A.28)

### Appendix B

Since Eq. (A.28) is too complicated to get a closed-form result in Flory's calculus, we concentrate hereinafter on its exponential regime, pointed out by small parameter values,  $\lambda_i \ll 1$  (or, in the strongest sense,  $\lambda \to 0^+$ ). Whenever possible in the next calculations indices *i* will be omitted.

A first point to make is that, as  $\gamma$ ,  $\phi$  and  $\hat{\phi}$  are all power series of  $\lambda$ , then when  $\lambda \ll 1$ :

$$\gamma(t,\lambda) = \sum_{n=0}^{\infty} (-1)^n \frac{\lambda^{n+t}}{n!(n+t)} \approx \frac{\lambda^t}{t} , \qquad (B.1)$$

$$\lambda \frac{\Phi}{\hat{\Phi}} \to 0 \tag{B.2}$$

and, neglecting  $\psi$  in comparison to  $|\ln \lambda|$ , one is left with:

$$\widetilde{W}_{p}(t) \approx -\frac{\lambda^{t} \ln \lambda}{t\Gamma(t)}$$
(B.3)

The contributions to Flory's integral, which only matter to the mechanical responses, become:

$$(\ln \lambda)^{-1} I(\alpha) \approx -(\ln \lambda) \alpha \,\Xi_{\lambda}[1] + (\ln \alpha) \,\Xi_{\lambda}[t^{-1}] + \Xi_{\lambda}[t^{-1}\ln \Gamma(\alpha t)] + \text{const.}$$
(B.4)

in which the functional notation in Eq. (23) was employed. Now:

$$\frac{1}{\Gamma(z+1)} = \sum_{k=0}^{\infty} \beta_k z^k \tag{B.5}$$

so that:

$$\beta_{n+1} = (n+1)^{-1} \sum_{j=0}^{n} (-1)^{j} s_{j+1} \beta_{n-j} , \qquad (B.6)$$

with  $\beta_0 = 1$ , while the coefficients:

$$s_j = \begin{cases} \ell & j = 1\\ \zeta(j) & j > 1 \end{cases}$$
(B.7)

depend on Riemann's zeta function  $\zeta(j)$ . Since:

$$\Gamma(z+1) = z\Gamma(z) \quad , \tag{B.8}$$

one obtains:

$$\Xi_{\lambda}[1] = \sum_{k=0}^{\infty} \beta_k \Lambda_{k+1} \tag{B.9}$$

in which, still for notational simplicity, we have set:

$$\Lambda_n \equiv \int_0^\infty \lambda^t t^n dt = (-1)^{1+n} \frac{\Gamma(1+n)}{(\ln \lambda)^{1+n}} > 0$$
(B.10)

Thus, as:

$$- \alpha (\ln \lambda)^2 \sum_{k=0}^{\infty} (-1)^k \beta_k \frac{\Gamma(k+2)}{(\ln \lambda)^{k+2}} = -\alpha \left\{ \beta_0 \Gamma(2) - \beta_1 \frac{\Gamma(3)}{\ln \lambda} + \dots \right\} \quad , \tag{B.11}$$

substituting  $\Gamma(n) = (n-1)!$  and the values of  $\beta_k$ , the first-order contribution in  $(\ln \lambda)^{-1}$  is:

$$-\alpha(\ln\lambda)^2 \Xi_{\lambda}[1] = -\alpha\left(1 - \frac{2\ell}{\ln\lambda}\right) + O(2)$$
(B.12)

To go ahead, note that:

$$\Xi_{\lambda}\left[t^{-1}\right] = \sum_{k=0}^{\infty} (-1)^k \beta_k \Lambda_k \tag{B.13}$$

from which:

$$(\ln \lambda)(\ln \alpha) \Xi_{\lambda} \left[ t^{-1} \right] = \left( -1 + \frac{\ell}{\ln \lambda} \right) \ln \alpha + O(2)$$
(B.14)

The last term in Eq. (B.4) rapidly converges in  $t \in [0, 1]$ . From the expansion  $\ln \Gamma(\alpha t) = -\ln(\beta_0 \alpha t + \beta_1 \alpha^2 t^2 \dots)$ :

$$\Xi_{\lambda}\left[t^{-1}\ln\Gamma(\alpha t)\right] \approx -\sum_{r=0}^{\infty}\beta_{r}\int_{0}^{\infty}\lambda^{t}t^{r}\ln(\beta_{0}\alpha t)dt$$
(B.15)

its dominant terms behave as  $\sim \ln \alpha$ :

$$\int_0^\infty \lambda^t t^r \ln(\beta_0 \alpha t) dt = \frac{(-1)^r}{(\ln \lambda)^{r+1}} \left\{ r! \left[ \ell' + \ln(-\ln \lambda) - \ln(\beta_0 \alpha) \right] + \text{const.} \right\}$$
(B.16)

thus we do not expect it is playing a significant role in experiments on isotropic media held at constant volume. However, as it represents the main signature of this end-to-end statistics, we leave it at the moment as it is. In conclusion, from the expression:

$$I_{i}(\alpha_{i}) \approx -(\alpha_{i} + \ln \alpha_{i}) + \frac{\ell}{\ln \lambda_{i}} \left( 2\alpha_{i} + \ln \alpha_{i} \right) + (\ln \lambda_{i}) \Xi_{\lambda_{i}} \left[ t^{-1} \ln \Gamma(\alpha_{i} t) \right] + \text{const.}$$
(B.17)

a 'ground state' approximation may be written as:

$$\frac{1}{\nu}\ln\Omega_{1P}^{(1)} \approx -\sum_{i} \alpha_{i} + \sum_{k} \Xi_{\lambda_{k}}^{(1)} \left[t^{-1}\ln\Gamma(\alpha_{k}t)\right] \ln\lambda_{k} + \text{const.}$$
(B.18)

while, at next order:

$$\frac{1}{\nu}\ln\Omega_{1P}^{(2)} \approx -\sum_{i}\alpha_{i} + \ell\sum_{p}\frac{2\alpha_{p} + \ln\alpha_{p}}{\ln\lambda_{p}} + \sum_{k}\Xi_{\lambda_{k}}^{(2)}\left[t^{-1}\ln\Gamma(\alpha_{k}t)\right]\ln\lambda_{k} + \text{const.}$$
(B.19)

Observe the Jacobian-logarithmic term in Flory's theory is replaced in Eqs. (B.18)–(B.19) by an integral of the logarithm of  $\Gamma$ , whereas the Jacobian trace is typical instead of exponential (e.g. Laplace's) statistics. Entropic constants are not available in these equation models.

As a last remark to be made, as  $\widetilde{W}_p$  was tackled upon  $\lambda_i \ll 1$ , its normalization condition should be rediscussed. Nevertheless, a numerical check performed with  $\lambda_i \sim 10^{-2}$  returned:

$$\int_{0}^{\infty} \widetilde{W}_{p}(t;\lambda_{i}\ll 1) dt = 1 + \varepsilon(\lambda_{i})$$
(B.20)

with  $\epsilon \leq 5 \cdot 10^{-2}$ , i.e. a reasonable agreement within a few percents.

# Appendix C

We regard here the perfect gas term as a functional perturbed by polymer statistics. It relies on the analysis presented in the second theoretical subsection and, in particular, on Eq. (28):

$$p = \prod_{i} \int_{-\frac{\delta x_i}{2}}^{\frac{\delta x_i}{2}} W_i(u) du$$
(C.1)

which has to be Taylor-expanded in  $\delta x_i$ . In the Gaussian case, we factorize for convenience  $\beta$ :

$$W_n(\mathbf{r};\beta) = \prod_i W_{in}(\mathbf{e}_i \cdot \mathbf{r};\beta_i), \quad \beta^3 \equiv \prod_i \beta_i$$
(C.2)

obtaining:

$$p = \left(\frac{\beta}{\sqrt{\pi}}\right)^3 \left[1 - \frac{1}{2}\sum_i (\beta_i \delta x_i)^2\right] \delta V + O(7)$$
(C.3)

so that  $(\beta/\sqrt{\pi})^3 \delta V$  identifies the probability  $P_{\mu}$  and the functional form to adopt is:

$$P_{n} \approx \frac{\delta v}{V} \left\{ 1 - \frac{\pi}{12} \left[ \left( \frac{\delta x}{x} \right)^{2} + \left( \frac{\delta y}{y} \right)^{2} + \left( \frac{\delta z}{z} \right)^{2} \right] \right\}^{-1}$$
(C.4)

As expected, the perturbation in square parenthesis formally resembles the dependence of  $\ln \Omega_{1n}(\alpha_i)$ , producing a correction factor in the new configuration partition function  $(\Omega_{2N})$ :

$$\Omega_{2N} \approx \omega_{2n} \Omega_{2n} \tag{C.5}$$

which reads:

$$\frac{1}{v}\ln\omega_{2n} = -\frac{1}{2}\ln\left\{1 - \frac{\pi}{12}\left[\alpha_x^{-2}\left(\frac{\delta x}{x_0}\right)^2 + \alpha_y^{-2}\left(\frac{\delta y}{y_0}\right)^2 + \alpha_z^{-2}\left(\frac{\delta z}{z_0}\right)^2\right]\right\}$$
(C.6)

and, finally:

$$\frac{1}{\nu} \ln \Omega_{2N} \approx \frac{1}{\nu} \ln \Omega_{2n} + \frac{\pi}{24} \xi_2 \sum_i \alpha_i^{-2}$$
(C.7)

where Flory's  $\ln \Omega_{2\pi}$  is still given by Eq. (27), while:

$$\xi_h \approx \frac{1}{3} \sum_i \left( \frac{\delta x_i}{x_{0i}} \right)^h \tag{C.8}$$

introduces an average length-scale parameter of order h, quantifying the coupling effect of network units to the mechanical response (at a scale ~  $x_{0}$ ). For simplicity, multiplicative factors in each perturbation term are grouped onward into single coefficients (e.g.  $\xi_n \equiv \frac{\pi}{24}\xi_2$ ).

I. Laplace's density. In this case:

$$\prod_{i} \left[ \int_{-\frac{\delta x_{i}}{2}}^{0} W_{iL}(u < 0) du + \int_{0}^{\frac{\delta x_{i}}{2}} W_{iL}(u > 0) du \right] = (1 - \frac{1}{4} \sum_{k} L_{k} \delta x_{k}) \prod_{i} \frac{1}{2} L_{i} \delta x_{i} + O(5)$$
(C.9)

and, letting  $P_i = \frac{1}{2} \prod_i L_i \delta x_i$ , one gets again a perturbation form conforming to Eq. (52):

$$P_{L} \approx \frac{\delta v}{V} \left[ 1 - \frac{1}{2} \left( \frac{\delta x}{x} + \frac{\delta y}{y} + \frac{\delta z}{z} \right) \right]^{-1}$$
(C.10)

With the same notations of Eq. (C.5):

$$\Omega_{2L} \approx \omega_{2L} \Omega_{2n} \tag{C.11}$$

the interlinking perturbation now writes:

$$\frac{1}{v}\ln\omega_{2L} \approx \frac{1}{4} \left[ \alpha_x^{-1} \left( \frac{\delta x}{x_0} \right) + \alpha_y^{-1} \left( \frac{\delta y}{y_0} \right) + \alpha_z^{-1} \left( \frac{\delta z}{z_0} \right) \right]$$
(C.12)

yielding, with  $\xi_{I} \equiv \frac{1}{4}\xi_{1}$ :

$$\frac{1}{\nu}\ln\Omega_{2L} \approx \frac{1}{\nu}\ln\Omega_{2n} + \xi_L \sum_i \alpha_i^{-1}$$
(C.13)

II. *Cauchy's density*. Taylor's series at leading orders of Gaussian and Cauchy's distributions coincide upon  $\chi_i \to \beta_i^{-1}$ :

$$\prod_{i} \int_{-\frac{\delta x_{i}}{2}}^{\frac{\delta x_{i}}{2}} W_{iC}(u) du = \left[ 1 - \frac{1}{12} \sum_{k} \left( \frac{\delta x_{k}}{\chi_{k}} \right)^{2} \right] \prod_{i} \left( \frac{\delta x_{i}}{\sqrt{\pi} \chi_{i}} \right) + O(5)$$
(C.14)

i.e.:

$$P_{c} = P_{\mu} + O(5)$$
 (C.15)

and, let  $\xi_C \equiv \frac{\pi}{24}\xi_2$ :

$$\frac{1}{v}\ln\Omega_{2C} \approx \frac{1}{v}\ln\Omega_{2n} + \xi_C \sum_i \alpha_i^{-2}$$
(C.16)

III. Poisson's density. Near the exponential limit, Taylor's expansion resembles Eq. (C.9):

$$p = -\left[1 + \frac{1}{4}\sum_{r} l_r(\ln\lambda_r) \,\delta x_r\right] \prod_i \frac{1}{2}(\ln\lambda_i) \delta x_i + O(5) \tag{C.17}$$

with the three semi-heuristic coefficients  $l_i = 1 - \frac{2\ell}{\ln \lambda_i} > 1$ . On identifying  $P_p = -\frac{1}{2} \prod_i (\ln \lambda_i) \delta x_i$ , one obtains:

$$P_{p} \approx \frac{\delta v}{V} \left[ 1 - \frac{1}{2} \left( l_{x} \frac{\delta x}{x} + l_{y} \frac{\delta y}{y} + l_{z} \frac{\delta z}{z} \right) \right]^{-1}$$
(C.18)

that, consistently with the exponential domain of Poisson's statistics, approaches  $P_L$  as  $l_i \rightarrow 1^-$ . Proceeding as usual with:

$$\Omega_{2P} \approx \omega_{2P} \Omega_{2n} \tag{C.19}$$

it turns out:

$$\frac{1}{v}\ln\omega_{2P} \approx \frac{1}{4} \left[ l_x \alpha_x^{-1} \left( \frac{\delta x}{x_0} \right) + l_y \alpha_y^{-1} \left( \frac{\delta y}{y_0} \right) + l_z \alpha_z^{-1} \left( \frac{\delta z}{z_0} \right) \right]$$
(C.20)

or:

$$\frac{1}{\nu}\ln\Omega_{2P} \approx \frac{1}{\nu}\ln\Omega_{2n} + \xi_P \sum_i \alpha_i^{-1}$$
(C.21)

where, let:

/

$$\xi_1^* = \frac{1}{3} \sum_i l_i \left( \frac{\delta x_i}{x_{0i}} \right) \ge \xi_1$$
(C.22)

the coupling coefficient in Eq. (C.21) reads  $\xi_{\rm p} \equiv \frac{1}{4}\xi_{\rm r}^*$ .

# Appendix D

We infer here the effect of the first configuration integral on the exponential limit of Poisson's statistics, where the experimental behavior deviates from Laplace's by the perturbation  $\Xi$  in Eq. (23). For simplicity, calculations are specialized to unswollen networks for  $\xi_i$ ,  $\xi_p \to 0^+$ , deducing the mechanical features of an isotropic system for  $Q \neq 1$ ,  $\lambda \ll 1$ .

In SH experiments, the lowest order displacement between the  $\ln \Omega_1$  contributions (subindices 1) to the shear stress in Poisson's and Laplace's statistics is given by:

$$\tau_{1,P} - \tau_{1,L} = -G_F \left(\frac{\partial \gamma}{\partial \alpha}\right)^{-1} \sum_{D_S(\alpha_i,1)} \ln \lambda_i \left(\frac{\partial \Xi_{\lambda_i}^{(1)} \left[t^{-1} \ln \Gamma(\alpha_i t)\right]}{\partial \alpha}\right)_{T,V}$$
(D.1)

still comprising a sum at constant volume, to be constrained to  $D_{c}(\alpha_{i}, 1)$  according to:

$$\left(\frac{\partial \Xi_{\lambda_i}\left[t^{-1}\ln\Gamma(\alpha_i t)\right]}{\partial\alpha}\right)_{T,V} \equiv \Xi_{\lambda_i}\left[\psi(\alpha_i t)\right]$$
(D.2)

We work it out by evaluating the expansion:

$$\psi(z+1) = -\ell + \sum_{\infty}^{k=2} (-1)^k \zeta(k) z^{k-1}$$
(D.3)

at  $z = \alpha_i t$ :

$$\Xi_{\lambda_i}\left[\psi(\alpha_i t)\right] = -\frac{1}{\alpha_i} \sum_{k=0}^{\infty} \beta_k \Lambda_k + \alpha_i \sum_{k=0}^{\infty} \beta_k \sum_{m=0}^{\infty} (-1)^m \zeta(m+2) \alpha_i^m \Lambda_{m+k+2}$$
(D.4)

and, since  $\Lambda_r \approx \lambda^{-1-r}$ , the leading term is:

 $\Xi_{\lambda_i} \left[ \psi(\alpha_i t) \right] \approx \left( \alpha_i \ln \lambda_i \right)^{-1} \tag{D.5}$ 

On the other hand, the derivative:

$$\left(\frac{\partial \Xi_{\lambda_i}\left[t^{-1}\ln\Gamma(\frac{t}{\alpha})\right]}{\partial\alpha}\right)_{T,V} = -\frac{1}{\alpha^2} \Xi_{\lambda_i}\left[\psi(\frac{t}{\alpha})\right]$$
(D.6)

cancels the perturbation in Eq. (D.1), i.e.:

$$\Xi_{\lambda_x}^{(1)}\left[\psi(\alpha t)\right]\ln\lambda_x = -\Xi_{\lambda_y}^{(1)}\left[\psi(\frac{t}{\alpha})\right]\ln\lambda_y \tag{D.7}$$

getting back to the lowest-order responses as predicted in Laplace's statistics:

$$\tau_{1,P} = \tau_{1,L}, \quad G_{1,P} = G_{1,L} \qquad (\lambda_i \to 0^+)$$
 (D.8)

At the subsequent order, the behavior is generally anisotropic, as it is affected by each  $\lambda_i$ :

$$\frac{1}{\nu}\ln\Omega_{1P}^{(2)} \approx -\sum_{r} \alpha_{r} + \ell \sum_{i} \frac{2\alpha_{i} + \ln\alpha_{i}}{\ln\lambda_{i}} + \sum_{p} \Xi_{\lambda_{p}}^{(2)} \left[t^{-1}\ln\Gamma(\alpha_{p}t)\right] \ln\lambda_{p} + \text{const.}$$
(D.9)

i.e.:

$$\tau_{1,P} \approx \tau_{1,L} + \delta \tau_{P} + \delta \tau_{\psi} \tag{D.10}$$

The first perturbation comes from:

$$\sum_{\mathcal{D}_{S}(\alpha_{i},1)} \frac{1}{\ln \lambda_{i}} \left( \frac{\partial}{\partial \alpha} \left[ 2\alpha_{i} + \ln \alpha_{i} \right] \right)_{T,V} = \frac{2}{\ln \lambda_{x}} + \left( \frac{1}{\ln \lambda_{x}} - \frac{1}{\ln \lambda_{y}} \right) \alpha^{-1} - \frac{2}{\ln \lambda_{y}} \alpha^{-2}$$
(D.11)

and reads:

$$\delta \tau_{p} = -\frac{2\ell}{1+\alpha^{2}} G_{F} \left[ \frac{\alpha^{2}}{\ln \lambda_{x}} + \frac{\alpha}{2} \left( \frac{1}{\ln \lambda_{x}} - \frac{1}{\ln \lambda_{y}} \right) - \frac{1}{\ln \lambda_{y}} \right], \tag{D.12}$$

while the second follows from Eqs. (D.2)-(D.5):

$$\sum_{\mathsf{D}_{\mathcal{S}}(\alpha_{i},1)} \Xi_{\lambda_{i}}^{(2)} \left[ \psi(\alpha_{i}t) \right] \ln \lambda_{i} \approx \frac{1}{\alpha} \left( 1 - \frac{\ell}{\ln \lambda_{x}} \right) + \alpha \left( 1 - \frac{\ell}{\ln \lambda_{y}} \right) \left( -\frac{1}{\alpha^{2}} \right) \tag{D.13}$$

i.e.:

$$\delta \tau_{\psi} = \frac{\ell' \alpha}{1 + \alpha^2} G_F \left[ \left( \ln \lambda_x \right)^{-1} - \left( \ln \lambda_y \right)^{-1} \right]$$
(D.14)

To sum Eq. (D.12) to Eq. (D.14) cancels out  $\delta \tau_w$ , identifying the overall response:

$$\delta \tau_{A} \equiv \delta \tau_{P} + \delta \tau_{\Psi} = \frac{2\ell}{1+\alpha^{2}} G_{F} \left[ \left( \ln \lambda_{Y} \right)^{-1} - \alpha^{2} \left( \ln \lambda_{X} \right)^{-1} \right]$$
(D.15)

so that:

$$\tau_{1,P} = \frac{\alpha}{\alpha^4 - 1} \left\{ \alpha^2 - 1 + 2\ell \left[ \left( \ln \lambda_x \right)^{-1} - \alpha^2 \left( \ln \lambda_y \right)^{-1} \right] \right\} \gamma(\alpha) G_F$$
(D.16)

and, for an isotropic medium  $(\lambda_x = \lambda_y \equiv \lambda, l_p \equiv 1 - \frac{2\ell}{\ln \lambda})$  it turns out for  $\lambda \ll 1$ :

$$\tau_{1,P} \approx l_P \frac{\alpha^2 - 1}{\alpha^2 + 1} G_F > \tau_{1,L}$$
 (D.17)

$$G_{1,P} \approx l_P \frac{\alpha}{\alpha^2 + 1} G_F > G_{1,L}$$
 (D.18)

We have thus inferred that passing from Laplace's to Poisson's statistics in the unperturbed exponential limit ( $\xi_L$ ,  $\xi_p \rightarrow 0^+$ ,  $\lambda \ll 1$ ) requires to multiply the shear mechanical properties by the factor  $l_p$ . Perturbation effects then are additive in  $\xi_k$ , as it comes from Eqs. (52), (54).

Regarding the dependence on the swelling factor, consider the reduced configuration integral:

$$I_{HP} = v \sum_{D_{S}(\alpha_{i},1)} \int_{0}^{\infty} \widetilde{W}_{iP}(\lambda,t) \ln \widetilde{W}_{iP}(\lambda,\alpha_{i}t) dt$$
(D.19)

and the corresponding shear modulus expression, near  $\alpha \approx 1$ :

$$G_{1,P} \approx -\frac{k_B T}{V_0 \gamma} \left(\frac{\partial \ln I_{HP}}{\partial \gamma}\right)_{T,V}$$
(D.20)

i.e.:

$$G_{1,P} \propto \int_0^\infty \frac{\lambda^t}{\Gamma(t)} \left[ (t\psi(t) - 1)\psi(t) - \frac{t\Gamma''(t)}{\Gamma(t)} + \ln\lambda \right] dt = \left\{ \Xi \left[ t\psi^2(t) \right] - \Xi \left[ \psi(t) \right] - \Xi \left[ t\psi(t)(\ln\Gamma(t))' \right] + (\ln\lambda) \Xi [1] \right\}$$
(D.21)

the proportionality constant, function of  $G_F$  and  $\ln \lambda$ , being unimportant to the present aim. The algebraic sum of the first three terms on the rightest side turns out to be negligible, and one is left with the only  $\Xi[1]$  contribution. In fact:

$$\Xi[\psi(t)] \approx -\beta_0 \Lambda_0 - \beta_1 \Lambda_1 \tag{D.22}$$

$$\Xi \left[ t \psi^2(t) \right] \approx \beta_0 \Lambda_0 + \beta_1 \Lambda_1 + 2\ell \beta_0 \Lambda_1 \tag{D.23}$$

$$\Xi \left[ t \psi(t) (\ln \Gamma(t))' \right] \approx 2(\beta_0 \Lambda_0 + \beta_1 \Lambda_1) + 2\ell \beta_0 \Lambda_1$$
(D.24)

and:

$$\Xi \left[ t \psi^2(t) \right] - \Xi \left[ \psi(t) \right] - \Xi \left[ t \psi(t) (\ln \Gamma(t))' \right] = O(3)$$
(D.25)

When  $D_s = D_s(\alpha_i, Q \neq 1)$ ,  $\Xi[1]$  is linearly multiplied by  $Q^{\frac{1}{3}}Q^{-1}$  (see Eq. (B.4)), rescaling Eq. (D.21) by means of  $Q^{-\frac{2}{3}}$ , still in accordance with Eq. (73). The same factor will also rescale any value of  $\xi_L$  and  $\xi_p$ , in the presence of finite perturbations. By adopting an akin procedure, it can be equally shown that Laplace's and Poisson's uniaxial stresses and elastic moduli of unperturbed deformation experiments,  $D_U = D_U(\alpha_i, Q \neq 1)$ , stand in the same proportionality relations, bringing to Eqs. (68)–(69) and Eqs. (72)–(73) of the main text.

# Appendix E

Based on Fig. 2 and Table 1 of the main text, one can conclude that the number of cubical meshes  $(N_{TM_i})$  and sides  $(N_{TS_i})$  in the polymeric network at generation  $n_i$  are given, respectively, by:

$$N_{TMi} = 1 + 26 \sum_{k=1}^{M} 3^{3(k-1)}$$
(E.1)

$$N_{TSi} = 12 + 132 \sum_{k=1}^{n_i} 3^{(k-1)}$$
(E.2)

Considering that a real system is not composed by meshes of identical side  $\zeta_i$  but, more realistically, comprises different meshes with sides spanning from  $\zeta_1$  to  $\zeta_N$ , ( $\zeta_1 < \zeta_2 < ... < \zeta_N$ ), we assume that the polymeric network is the result of summing up meshes of all dimensions. Thus, the fraction of meshes ( $F_{Mi}$ ) and sides ( $F_{Si}$ ) of length  $\zeta_i$  is given by:

$$F_{Mi} = \frac{1 + 26\sum_{k=1}^{n_i} 3^{3(k-1)}}{\sum_{i=1}^{N} \left(1 + 26\sum_{k=1}^{k=n_i} 3^{3(k-1)}\right)}$$
(E.3)

$$F_{Si} = \frac{12 + 132 \sum_{k=1}^{n_1} 3^{(k-1)}}{\sum_{i=1}^{N} \left(1 + 132 \sum_{k=1}^{k=n_i} 3^{(k-1)}\right)}$$
(E.4)

In order to make the model more flexible, it is convenient moving from the discrete mesh (Eq. (E.3) and side (Eq. (E.4) distribution to a continuous one. Thus, differentiation of Eqs. (E.1) and (E.2) leads to:

$$\frac{dN_{TMi}}{dk} = 26 \cdot 3^{3(k-1)} \ln_e(3) \cdot 3$$
(E.5)

$$\frac{dN_{TSi}}{dk} = 132 \cdot 3^{(k-1)} \ln_e(3)$$
(E.6)

while integrating Eq. (E.5) and (E.6) yields:

$$N_{TMi} = \int dN_{TMi} = 26 \cdot \ln_e(3) \cdot 3 \int 3^{3(k-1)} dk = \frac{26}{27} 3^{3(n_i-1)} + C_M$$
(E.7)

$$N_{TSi} = \int dN_{TSi} = 132 \cdot \ln_e(3) \int 3^{(k-1)} dk = \frac{132}{3} 3^{3n_i} + C_S$$
(E.8)

where  $C_M$  and  $C_S$  are two integration constants that follow from imposing that Eqs. (E.7) and (E.8) give the same estimation of  $N_{TM_i}$  and  $N_{TS_i}$ , as provided by Eqs. (E.1) and (E.2), respectively. Accordingly, we have:

$$\frac{26}{27}3^{3(n_i-1)} + C_M = 1 + 26\sum_{k=1}^{n_i} 3^{3(k-1)}$$
(E.9)

$$C_{M} = 1 + \frac{26}{27} \left( 3^{3n_{i}} - 3^{3n_{i}} \right) + \frac{26}{27} \sum_{k=1}^{n_{i}-1} 3^{3k} = 1 + \frac{26}{27} \sum_{k=1}^{n_{i}-1} 3^{3k}$$
(E.10)

$$\frac{132}{3}3^{3n_i} + C_S = 12 + 132 \sum_{k=1}^{n_i} 3^{(k-1)}$$
(E.11)

$$C_{S} = 12 + \frac{132}{3} \left(3^{n_{i}} - 3^{n_{i}}\right) + \frac{132}{3} \sum_{k=1}^{n_{i}-1} 3^{k} = 12 + \frac{132}{3} \sum_{k=1}^{n_{i}-1} 3^{k}$$
(E.12)

On the basis of Eqs. (E.10) and (E.12), Eqs.(E.7) and (E.8) become:

$$N_{TMi} = 1 + \frac{26}{27} 3^{3n_i} + \frac{26}{27} \sum_{k=1}^{n_i - 1} 3^{3k}$$
(E.13)

$$N_{TSi} = 12 + \frac{132}{3}3^{n_i} + \frac{132}{3}\sum_{k=1}^{n_i-1}3^k$$
(E.14)

Assuming  $n_i \ge 1$ , it is easy to verify that the sum of the first and third term (summation) of Eq. (E.13) is negligible in comparison to the second one, so that:

$$N_{TMi} \approx \frac{26}{27} 3^{3n_i}$$
(E.15)

In Eq. (E.14), instead, prevailing terms are the second and first of the summation, thence:

$$N_{\text{TSi}}\% \approx \frac{132}{3}3^{n_i} + \frac{132}{3}3^{(n_i-1)} = 132 \cdot 3^{(n_i-1)}\left(1 + \frac{1}{3}\right)$$
(E.16)

and, in light of Eqs. (E.15) and (E.16), Eqs. (E.3) and (E.4) can be written as:

$$F_{Mi}\% \approx \frac{3^{3n_i}}{\sum_{i=1}^N 3^{n_i}}$$
 (E.17)

$$F_{Si}\% \approx \frac{3^{n_i}}{\sum_{i=1}^{N} 3^{n_i}}$$
 (E.18)

where now  $n_i$  are real numbers  $\geq 1$ , whose determination comes from the experimental values of  $F_{M_i}$ , i.e. the probability  $P_i$  of finding a cubical mesh of size  $\zeta_i$  (see Eq. (91)):

$$\frac{P_2}{P_1} = \frac{F_{M2}}{F_{M1}} = 3^{3(n_2 - n_1)}, \quad \frac{P_i}{P_{i-1}} = \frac{F_{Mi}}{F_{Mi-1}} = 3^{3(n_i - n_{i-1})}$$
(E.19)

Eq. (E.19) allows to determine  $n_i$  in terms of  $n_1$ :

$$n_{i} = n_{i-1} + \frac{1}{3} \ln_{3} \left( \frac{P_{i}}{P_{i-1}} \right) = n_{1} + \frac{1}{3} \ln_{3} \left( \frac{P_{i}}{P_{1}} \right)$$
(E.20)

and, finally, Eq. (E.20), Eq. (E.17) and Eq. (E.18) become:

$$F_{Mi}\% \approx \frac{3^{3n_i}}{\sum_{i=1}^N 3^{3n_i}} = \frac{3^{3\binom{n_i+\frac{1}{3}\ln_3\binom{P_i}{P_1}}{}}}{\sum_{i=1}^N 3^{3\binom{n_i+\frac{1}{3}\ln_3\binom{P_i}{P_1}}{}}} = \frac{3^{\binom{\ln_3\binom{P_i}{P_1}}{P_1}}}{\sum_{i=1}^N 3^{\binom{\ln_3\binom{P_i}{P_1}}{P_1}}} = \frac{P_i}{\sum_{i=1}^N P_i}$$
(E.21)

$$F_{Si}\% \approx \frac{3^{n_i}}{\sum_{i=1}^N 3^{n_i}} = \frac{3^{\left(n_1 + \frac{1}{3}\ln_3\left(\frac{P_1}{P_1}\right)\right)}}{\sum_{i=1}^N 3^{\left(n_1 + \frac{1}{3}\ln_3\left(\frac{P_1}{P_1}\right)\right)}} = \frac{3^{\left(\frac{1}{3}\ln_3\left(\frac{P_1}{P_1}\right)\right)}}{\sum_{i=1}^N 3^{\left(\frac{1}{3}\ln_3\left(\frac{P_1}{P_1}\right)\right)}} = \frac{\sqrt[3]{P_i}}{\sum_{i=1}^N \sqrt[3]{P_i}}$$
(E.22)

### References

1007/3-540-11471-8 2.

- Abrami, M., Chiarappa, G., Farra, R., Grassi, G., Marizza, P., & Grassi, M. (2018). Use of low field NMR for the characterization of gels and biological tissues. *ADMET DMPK*, 6(1), 34–46. http://dx.doi.org/10.5599/admet.6.1.430.
- Aldous, D. (1989). Exponential combinatorial extrema. In Probability approximations via the poisson clumping heuristic (pp. 131–148). New York, NY: Springer New York, http://dx.doi.org/10.1007/978-1-4757-6283-9\_7.
- Amabili, M. (2018). Nonlinear mechanics of shells and plates in composite, soft and biological materials. Cambridge University Press, URL: https://books.google.it/books?id=h5VuDwAAQBAJ.
- Amsden, B. (1998). Solute diffusion within hydrogels. Mechanisms and models. Macromolecules, 31(23), 8382-8395. http://dx.doi.org/10.1021/ma980765f.
- Anssari-Benam, A., Bucchi, A., & Saccomandi, G. (2021). On the central role of the invariant I<sub>2</sub> in nonlinear elasticity. *International Journal of Engineering Science*, 163, Article 103486. http://dx.doi.org/10.1016/j.ijengsci.2021.103486, URL: https://www.sciencedirect.com/science/article/pii/S0020722521000331.
- Arnott, S., Fulmer, A., Scott, W., Dea, I., Moorhouse, R., & Rees, D. (1974). The agarose double helix and its function in agarose gel structure. Journal of Molecular Biology, 90(2), 269–284. http://dx.doi.org/10.1016/0022-2836(74)90372-6, URL: http://www.sciencedirect.com/science/article/pii/0022283674903726.
- Arruda, E. M., & Boyce, M. C. (1993). A three-dimensional constitutive model for the large stretch behavior of rubber elastic materials. Journal of the Mechanics and Physics of Solids, 41(2), 389–412. http://dx.doi.org/10.1016/0022-5096(93)90013-6, URL: https://www.sciencedirect.com/science/article/pii/ 0022509693900136.
- Baek, S., & Srinivasa, A. (2004). Diffusion of a fluid through an elastic solid undergoing large deformation. International Journal of Non-Linear Mechanics, 39(2), 201–218. http://dx.doi.org/10.1016/S0020-7462(02)00153-1.
- Baker, M., & Ericksen, J. (1954). Inequalities restricting the form of the stress-deformation relations for isotropic elastic solids and Reiner-Rivlin fluids. Journal of the Washington Academy of Sciences, 44, 33–35, URL: https://www.jstor.org/stable/24533303.
- Ball, R., Doi, M., Edwards, S., & Warner, M. (1981). Rubber-like elasticity. Polymer, 22, 1010.
- Ball, R. C., & Edwards, S. F. (1980). Elasticity and stability of a dense gel. Macromolecules, 13(3), 748-761. http://dx.doi.org/10.1021/ma60075a049.
- Basu, A., Wen, Q., Mao, X., Lubensky, T. C., Janmey, P. A., & Yodh, A. G. (2011). Nonaffine displacements in flexible polymer networks. *Macromolecules*, 44(6), 1671–1679. http://dx.doi.org/10.1021/ma1026803.
- Beatty, M. F. (1987). Topics in finite elasticity: Hyperelasticity of rubber, elastomers, and biological tissues—With examples. Applied Mechanics Reviews, 40(12), 1699–1734. http://dx.doi.org/10.1115/1.3149545.
- Beatty, M. (2003). An average-stretch full-network model for rubber elasticity. 70, (pp. 65-86). http://dx.doi.org/10.1007/1-4020-2308-1\_7,
- Bechir, H., Chevalier, L., & Idjeri, M. (2010). A three-dimensional network model for rubber elasticity: The effect of local entanglements constraints. *International Journal of Engineering Science*, 48(3), 265–274. http://dx.doi.org/10.1016/j.ijengsci.2009.10.004, URL: https://www.sciencedirect.com/science/article/pii/S0020722509001566.
- Bird, R. B., Armstrong, R., & Hassager, O. (1990). Dynamics of polymeric liquids, volume 1: fluid mechanics (2nd ed.). (pp. 72-75). Wiley, New York.
- Blatz, P. J., & Ko, W. L. (1962). Application of finite elastic theory to the deformation of rubbery materials. *Transactions of the Society of Rheology*, 6(1), 223–252. http://dx.doi.org/10.1122/1.548937.
- Bluhm, T. L., Deslandes, Y., Marchessault, R. H., Pérez, S., & Rinaudo, M. (1982). Solid-state and solution conformation of scleroglucan. Carbohydrate Research, 100(1), 117–130. http://dx.doi.org/10.1016/S0008-6215(00)81030-7, URL: http://www.sciencedirect.com/science/article/pii/S0008621500810307.
- Burak Erman, M. J. E. (1989). Rubber-like elasticity. Annual Review of Physical Chemistry, 40, 351–374. http://dx.doi.org/10.1146/annurev.pc.40.100189.002031. Burnham, K. P., & Anderson, D. R. (2004). Multimodel inference: Understanding AIC and BIC in model selection. Sociological Methods & Research, 33(2), 261–304.
- http://dx.doi.org/10.1177/0049124104268644. Candau, S., Bastide, J., & Delsanti, M. (1982). Structural, elastic, and dynamic properties of swollen polymer networks. 44, (pp. 27–71). http://dx.doi.org/10.
- Carroll, M. (2011). A strain energy function for vulcanized rubbers. Journal of Elasticity, 103, 173-187. http://dx.doi.org/10.1007/s10659-010-9279-0.
- Chan, A. W., & Neufeld, R. J. (2009). Modeling the controllable pH-responsive swelling and pore size of networked alginate based biomaterials. *Biomaterials*, 30(30), 6119–6129. http://dx.doi.org/10.1016/j.biomaterials.2009.07.034, URL: http://www.sciencedirect.com/science/article/pii/S0142961209007467.

- Chui, M. M., Phillips, R. J., & McCarthy, M. J. (1995). Measurement of the porous microstructure of hydrogels by nuclear magnetic resonance. *Journal of Colloid and Interface Science*, 174(2), 336–344. http://dx.doi.org/10.1006/jcis.1995.1399. URL: http://www.sciencedirect.com/science/article/pii/S0021979785713999.
- Coviello, T., Grassi, M., Lapasin, R., Marino, A., & Alhaique, F. (2003). Scleroglucan/borax: characterization of a novel hydrogel system suitable for drug delivery. *Biomaterials*, 24(16), 2789–2798. http://dx.doi.org/10.1016/S0142-9612(03)00087-5, URL: http://www.sciencedirect.com/science/article/pii/ S0142961203000875.
- Coviello, T., Grassi, M., Rambone, G., & Alhaique, F. (2001). A crosslinked system from Scleroglucan derivative: preparation and characterization. *Biomaterials*, 22(13), 1899–1909. http://dx.doi.org/10.1016/S0142-9612(00)00374-4. URL: https://www.sciencedirect.com/science/article/pii/S0142961200003744.
- Coviello, T., Matricardi, P., Alhaique, F., Farra, R., Tesei, G., Fiorentino, S., et al. (2013). Guar gum/borax hydrogel: Rheological, low field NMR and release characterizations. Express Polymer Letters, 7, 733–746. http://dx.doi.org/10.3144/expresspolymlett.2013.71.
- Curro, J. G., & Mark, J. E. (1984). A non-Gaussian theory of rubberlike elasticity based on rotational isomeric state simulations of network chain configurations. II. Bimodal poly(dimethylsiloxane) networks. *Journal of Chemical Physics*, 80(9), 4521–4525. http://dx.doi.org/10.1063/1.447237.
- D. Stein, A., A. Hoffman, D., Frank, C., & D. Fayer, M. (1992). Reorientational motion of a cross-link junction in a poly(dimethylsiloxane) network measured by time-resolved fluorescence depolarization. *Journal of Chemical Physics*, 96, http://dx.doi.org/10.1063/1.461972.
- de Gennes, P. (1979). Scaling concepts in polymer physics (p. 324 S.). Ithaca, New York, USA: Cornell University Press.
- de Vos, P., Bučko, M., Gemeiner, P., Navrátil, M., Švitel, J., Faas, M., et al. (2009). Multiscale requirements for bioencapsulation in medicine and biotechnology. *Biomaterials*, 30(13), 2559–2570. http://dx.doi.org/10.1016/j.biomaterials.2009.01.014, URL: http://www.sciencedirect.com/science/article/ pii/S0142961209000210.
- De'Nobili, M., Rojas, A., Abrami, M., Lapasin, R., & Grassi, M. (2015). Structure characterisation by means of rheological and NMR experiments as a first necessary approach to study the L-(+)-ascorbic acid diffusion from pectin and pectin/alginate films to agar hydrogels that mimic food materials. *The Journal* of Food Process Engineering, 165, http://dx.doi.org/10.1016/j.jfoodeng.2015.05.014.
- Destrade, M., Saccomandi, G., & Sgura, I. (2017). Methodical fitting for mathematical models of rubber-like materials. *Proceedings of the Royal Society A*, 473(2198), Article 20160811. http://dx.doi.org/10.1098/rspa.2016.0811, URL: https://royalsocietypublishing.org/doi/abs/10.1098/rspa.2016.0811.

Dietmar, G., & Thomas, S. (2011). Fracture mechanics - with an introduction to micromechanics. http://dx.doi.org/10.1007/978-3-642-19240-1.

- Djabourov, M., Clark, A. H., Rowlands, D. W., & Ross-Murphy, S. B. (1989). Small-angle x-ray scattering characterization of agarose sols and gels. *Macromolecules*, 22(1), 180–188. http://dx.doi.org/10.1021/ma00191a035.
- Donati, I., & Paoletti, S. (2009). Material properties of alginates. In B. H. A. Rehm (Ed.), Alginates: biology and applications (pp. 1–53). Berlin, Heidelberg: Springer Berlin Heidelberg, http://dx.doi.org/10.1007/978-3-540-92679-5 1.
- Draget, K. I., Smidsrød, O., & Skjåk-Bræk, G. (2005). Alginates from algae. In *Biopolymers online*. American Cancer Society, http://dx.doi.org/10.1002/3527600035. bpol6008, URL: https://onlinelibrary.wiley.com/doi/abs/10.1002/3527600035.bpol6008.
- Edwards, S. F., & Vilgis, T. A. (1988). The tube model theory of rubber elasticity. Reports on Progress in Physics, 51(2), 243-297. http://dx.doi.org/10.1088/0034-4885/51/2/003.
- Eichinger, B. E. (2015). Rubber elasticity: Solution of the James-guth model. *Physical Review E*, 91, Article 052601. http://dx.doi.org/10.1103/PhysRevE.91.052601, URL: https://link.aps.org/doi/10.1103/PhysRevE.91.052601.

Elías-Zúñiga, A. (2006). A non-Gaussian network model for rubber elasticity. Polymer, 47(3), 907-914. http://dx.doi.org/10.1016/j.polymer.2005.11.078.

Elías-Zúñiga, A., & Beatty, M. F. (2002). Constitutive equations for amended non-Gaussian network models of rubber elasticity. International Journal of Engineering Science, 40(20), 2265–2294. http://dx.doi.org/10.1016/S0020-7225(02)00140-4.

- Erman, B. (2010). Advances in constraint theories of rubber-like elasticity of polymers. Current Opinion in Solid State & Materials Science, 14(2), 35-37. http://dx.doi.org/10.1016/j.cossms.2009.08.003.
- Erman, B., & Flory, P. J. (1982a). Relationships between stress, strain, and molecular constitution of polymer networks. Comparison of theory with experiments. *Macromolecules*, 15(3), 806–811. http://dx.doi.org/10.1021/ma00231a023.
- Fariña, J., Sineriz, F., Molina, O., & Perotti, N. (2001). Isolation and physicochemical characterization of soluble scleroglucan from sclerotium rolfsii. Rheological properties, molecular weight and conformational characteristics. *Carbohydrate Polymers*, 44, 41–50. http://dx.doi.org/10.1016/S0144-8617(00)00189-2.
  Feller, W. (1991). An introduction to probability theory and its applications (p. xi + 704). John Wiley, New York.
- Fixman, M., & Alben, R. (1973). Polymer conformational statistics. I. Probability distribution. Journal of Chemical Physics, 58(4), 1553–1558. http://dx.doi.org/ 10.1063/1.1679334.
- Flory, P. (1953). Baker lectures 1948, Principles of polymer chemistry. Ithaca, New York, USA: Cornell University Press, URL: https://books.google.it/books?id= COOEbEkt75R0C.
- Flory, P. J., & Erman, B. (1982). Theory of elasticity of polymer networks. 3. Macromolecules, 15(3), 800-806. http://dx.doi.org/10.1021/ma00231a022.
- Flory, P. J., & Rehner, J. (1943). Statistical mechanics of cross-linked polymer networks II. Swelling. Journal of Chemical Physics, 11(11), 521–526. http: //dx.doi.org/10.1063/1.1723792.
- Fox, M. (2001). Optical properties of solids (pp. 145-150). Oxford: Oxford University Press.
- Gedde, U. W. (1995). Polymer physics (p. xi + 298). Chapman & Hall, London.
- Gent, A. N. (1996). A new constitutive relation for rubber. Rubber Chemistry and Technology, 69(1), 59-61. http://dx.doi.org/10.5254/1.3538357.
- Gong, J., Katsuyama, Y., Kurokawa, T., & Osada, Y. (2003). Double-network hydrogels with extremely high mechanical strength. Advanced Materials, 15(14), 1155–1158. http://dx.doi.org/10.1002/adma.200304907.
- Gottlieb, M. (1982). The relationship between the modified Flory rubber elasticity theory and the Dossin–Graessley small strain model. *Journal of Chemical Physics*, 77(9), 4783–4785. http://dx.doi.org/10.1063/1.444386.
- Grassi, M., Lapasin, R., Coviello, T., Matricardi, P., Di Meo, C., & Alhaique, F. (2009). Scleroglucan/borax/drug hydrogels: Structure characterisation by means of rheological and diffusion experiments. *Carbohydrate Polymers*, 78, 377–383. http://dx.doi.org/10.1016/j.carbpol.2009.04.025.
- Grassi, M., Lapasin, R., & Pricl, S. (1996). A study of the rheological behavior of scleroglucan weak gel systems. Carbohydrate Polymers, 29(2), 169–181. http://dx.doi.org/10.1016/0144-8617(95)00120-4, URL: http://www.sciencedirect.com/science/article/pii/0144861795001204.
- Gundogan, N., Okay, O., & Oppermann, W. D.-I. (2004). Swelling, elasticity and spatial inhomogeneity of Poly(N,N-dimethylacrylamide) hydrogels formed at various polymer concentrations. *Macromolecular Chemistry and Physics*, 205, 814–823. http://dx.doi.org/10.1063/1.461972.
- Hadizadeh, S., Linhananta, A., & Plotkin, S. S. (2011). Improved measures for the shape of a disordered polymer to test a mean-field theory of collapse. *Macromolecules*, 44(15), 6182–6197. http://dx.doi.org/10.1021/ma200454e.
- Hermans, J. J. (1962). Statistical thermodynamics of swollen polymer networks. Journal of Polymer Science, 59(167), 191–208. http://dx.doi.org/10.1002/pol. 1962.1205916715, URL: https://onlinelibrary.wiley.com/doi/abs/10.1002/pol.1962.1205916715.
- Hild, G. (1998). Model networks based on 'endlinking' processes: synthesis, structure and properties. Progress in Polymer Science, 23(6), 1019–1149. http://dx.doi.org/10.1016/S0079-6700(97)00055-5.
- Hill, J. M., & Arrigo, D. J. (1995). New families of exact solutions for finitely deformed incompressible elastic materials. *IMA Journal of Applied Mathematics*, 54(2), 109–123. http://dx.doi.org/10.1093/imamat/54.2.109.
- Holz, M., Heil, S. R., & Sacco, A. (2000). Temperature-dependent self-diffusion coefficients of water and six selected molecular liquids for calibration in accurate 1H NMR PFG measurements. *Physical Chemistry Chemical Physics*, 2, 4740–4742. http://dx.doi.org/10.1039/B005319H, URL: http://dx.doi.org/10.1039/ B005319H.

- Hossain, M., & Steinmann, P. (2013). More hyperelastic models for rubber-like materials: consistent tangent operators and comparative study. The Journal of the Mechanical Behavior of Materials, 22(1-2), 27-50. http://dx.doi.org/10.1515/jmbm-2012-0007.
- Huang, Z.-P. (2014). A novel constitutive formulation for rubberlike materials in thermoelasticity. Journal of Applied Mechanics, 81(4), http://dx.doi.org/10.1115/ 1.4025272, 041013.
- Huang, Y., Szleifer, I., & Peppas, N. A. (2002). A molecular theory of polymer gels. Macromolecules, 35(4), 1373–1380. http://dx.doi.org/10.1021/ma011294r. Ilienko, A. (2013). Continuous counterparts of Poisson and binomial distributions and their properties. Annales Universitatis Scientiarium Budapestinensis. Sectio Mathematica, 39, 1
- James, H. M., & Guth, E. (1943). Theory of the elastic properties of rubber. Journal of Chemical Physics, 11(10), 455-481. http://dx.doi.org/10.1063/1.1723785.
- Johner, A., Vilgis, T. A., & Joanny, J. F. Polyelectrolyte gel elasticity in poor solvent. Macromolecular Symposia, 146(1), 223-226. http://dx.doi.org/10.1002/ masy.19991460130.
- Koetting, M. C., Peters, J. T., Steichen, S. D., & Peppas, N. A. (2015). Stimulus-responsive hydrogels: Theory, modern advances, and applications. *Materials Science and Engineering Reports*, 93, 1–49. http://dx.doi.org/10.1016/j.mser.2015.04.001, URL: http://www.sciencedirect.com/science/article/pii/ S0927796X15000339.
- Kolmogorov, A. L. (1933). Sulla determinazione empirica di una legge di distribuzione. G Ist Ital Attuari, 4, 83-91, URL: https://ci.nii.ac.jp/naid/10030673552/en/.
- Kotz, S., Kozubowski, T., & Podgorski, K. (2001). The laplace distribution and generalizations. a revisit with applications to communications, economics, engineering, and finance. Birkhäuser Boston, Inc., Boston, MA, http://dx.doi.org/10.1007/978-1-4612-0173-1\_5.
- Kouwijzer, M., & Pérez, S. (1998). Molecular modeling of agarose helices, leading to the prediction of crystalline allomorphs. *Biopolymers*, 46(1), 11–29. http://dx.doi.org/10.1002/(SICI)1097-0282(199807)46:1<11::AID-BIP2>3.0.CO;2-0.
- Labropoulos, K., Niesz, D., Danforth, S., & Kevrekidis, P. (2002). Dynamic rheology of agar gels: Theory and experiments. Part I. development of a rheological model. Carbohydrate Polymers, 50, 393–406. http://dx.doi.org/10.1016/S0144-8617(02)00084-X.
- Lapasin, R., & Pricl, S. (1995). Rheology of industrial polysaccharides: theory and applications; blackie academic & professional. http://dx.doi.org/10.1007/978-1-4615-2185-3.
- Mark, J. E. (1992). Molecular aspects of rubberlike elasticity. Angewandte Makromolekulare Chemie, 202(1), 1–30. http://dx.doi.org/10.1002/apmc.1992. 052020101.
- Mark, J. E., & Curro, J. G. (1983). A non-Gaussian theory of rubberlike elasticity based on rotational isomeric state simulations of network chain configurations. I.
- Polyethylene and polydimethylsiloxane short-chain unimodal networks. Journal of Chemical Physics, 79(11), 5705–5709. http://dx.doi.org/10.1063/1.445656. Matricardi, P., Alhaique, F., & Coviello, E. (2016). Polysaccahride hydrogels: characterization and biomedical applications (p. 540). Taylor & Francis Group, Boca Baton USA: CBC Press
- Matricardi, P., Meo, C. D., Coviello, T., Hennink, W. E., & Alhaique, F. (2013). Interpenetrating polymer networks polysaccharide hydrogels for drug delivery and tissue engineering. Advanced Drug Delivery Reviews, 65(9), 1172–1187. http://dx.doi.org/10.1016/j.addr.2013.04.002, URL: http://www.sciencedirect.com/ science/article/pii/S0169409X13000628.
- Matricardi, P., Onorati, I., Coviello, T., & Alhaique, F. (2006). Drug delivery matrices based on scleroglucan/alginate/borax gels. International Journal of Pharmaceutics, 316, 21–28. http://dx.doi.org/10.1016/j.ijpharm.2006.02.024.
- Meiboom, S., & Gill, D. (1958). Modified spin-echo method for measuring nuclear relaxation times. Review of Scientific Instruments, 29(8), 688-691. http://dx.doi.org/10.1063/1.1716296.
- Menduina, C., Freire, J. J., Llorente, M. A., & Vilgis, T. (1986). Correctly averaged non-Gaussian theory of rubberlike elasticity. application to the description of the behavior of poly(dimethylsiloxane) bimodal networks. *Macromolecules*, 19(4), 1212–1217. http://dx.doi.org/10.1021/ma00158a045.
- Mergell, B., & Everaers, R. (2001). Tube models for rubber-elastic systems. Macromolecules, 34(16), 5675–5686. http://dx.doi.org/10.1021/ma002228c.
- Mezzasalma, S. A. (2001). Polymer chain size from geodesic path and geometrical bolyai–lobachevskij partition function. Application to swelling of macromolecules in solution and micellar growth. Journal of Statistical Physics, 102, 1331–1341. http://dx.doi.org/10.1023/A:1004848630492.
- Mezzasalma, S. A. (2008). Macromolecules in solution and Brownian relativity. London: Academic Press-Elsevier, http://dx.doi.org/10.1016/S1573-4285(07)00009-9.
- Mihai, L. A., & Goriely, A. (2017). How to characterize a nonlinear elastic material? A review on nonlinear constitutive parameters in isotropic finite elasticity. Proceedings of the Royal Society of London, Series A (Mathematical and Physical Sciences), 473(2207), Article 20170607. http://dx.doi.org/10.1098/rspa.2017. 0607, URL: https://royalsocietypublishing.org/doi/abs/10.1098/rspa.2017.0607.
- Mihai, L. A., Woolley, T. E., & Goriely, A. (2019). Likely equilibria of the stochastic rivlin cube. Philosophical Transactions of the Royal Society, Series A, 377(2144), Article 20180068. http://dx.doi.org/10.1098/rsta.2018.0068, URL: https://royalsocietypublishing.org/doi/abs/10.1098/rsta.2018.0068.
- Mooney, M. (1940). A theory of large elastic deformation. Journal of Applied Physics, 11(9), 582-592. http://dx.doi.org/10.1063/1.1712836.
- Ngai, K. L., & Roland, C. M. (1994). Junction dynamics and the elasticity of networks. *Macromolecules*, 27(9), 2454–2459. http://dx.doi.org/10.1021/ma00087a014.
- Ogden, R. W., & Hill, R. (1972). Large deformation isotropic elasticity on the correlation of theory and experiment for incompressible rubberlike solids. Proceedings of the Royal Society of London. Series A, 326(1567), 565–584. http://dx.doi.org/10.1098/rspa.1972.0026, URL: https://royalsocietypublishing.org/ doi/abs/10.1098/rspa.1972.0026.
- Okumura, D., Kondo, A., & Ohno, N. (2016). Using two scaling exponents to describe the mechanical properties of swollen elastomers. *Journal of the Mechanics and Physics of Solids*, *90*, 61–76. http://dx.doi.org/10.1016/j.jmps.2016.02.017, URL: https://www.sciencedirect.com/science/article/pii/S0022509615301290.
- Ornstein, L. S., & Zernike, F. (1914). Accidental deviations of density and opalescence at the critical point of a single substance. Proceedings of the Royal Netherlands Academy of Arts and Sciences, 17(II), 793-806.
- Palleschi, A., Bocchinfuso, G., Coviello, T., & Alhaique, F. (2005). Molecular dynamics investigations of the polysaccharide scleroglucan: first study on the triple helix structure. Carbohydrate Research, 340(13), 2154–2162. http://dx.doi.org/10.1016/j.carres.2005.06.026, URL: http://www.sciencedirect.com/science/ article/pii/S0008621505003137.
- Panyukov, S. (1989). Topology fluctuations in polymer networks. Journal of Experimental and Theoretical Physics, 69, 342-353.
- Panyukov, S. (1990). Scaling theory of high elasticity. Journal of Experimental and Theoretical Physics, 98, 668-680.
- Panyukov, S., & Rabin, Y. (1996). Statistical physics of polymer gels. Physics Reports, 269(1), 1–131. http://dx.doi.org/10.1016/0370-1573(95)00068-2.
- Pasut, E., Toffanin, R., Voinovich, D., Pedersini, C., Murano, E., & Grassi, M. (2008). Mechanical and diffusive properties of homogeneous alginate gels in form of particles and cylinders. *Journal of Biomedical Materials Research*, 87A(3), 808–818. http://dx.doi.org/10.1002/jbm.a.31680, URL: https://onlinelibrary.wiley. com/doi/abs/10.1002/jbm.a.31680.
- Peköz, E. A., & Röllin, A. (2011). New rates for exponential approximation and the theorems of Rényi and Yaglom. The Annals of Probability, 39(2), 587–608. http://dx.doi.org/10.1214/10-AOP559.
- Pence, T. J., & Tsai, H. (2006). Swelling-induced cavitation of elastic spheres. Mathematics and Mechanics of Solids, 11(5), 527–551. http://dx.doi.org/10.1177/1081286504046481.
- Priss, L. (1981). Molecular origin of constants in the theory of rubber-like elasticity considering network chains steric interaction. Pure and Applied Chemistry, 53, 1581–1596.
- Provencher, S. W. (1982). A constrained regularization method for inverting data represented by linear algebraic or integral equations. Computer Physics Communications, 27(3), 213–227. http://dx.doi.org/10.1016/0010-4655(82)90173-4, URL: http://www.sciencedirect.com/science/article/pii/ 0010465582901734.

- Puglisi, G., & Saccomandi, G. (2016). Multi-scale modelling of rubber-like materials and soft tissues: an appraisal. Proceedings of the Royal Society of London, Series A (Mathematical and Physical Sciences), 472(2187), Article 20160060. http://dx.doi.org/10.1098/rspa.2016.0060, URL: https://royalsocietypublishing. org/doi/abs/10.1098/rspa.2016.0060.
- Richbourg, N. R., & Peppas, N. A. (2020). The swollen polymer network hypothesis: Quantitative models of hydrogel swelling, stiffness, and solute transport. *Progress in Polymer Science*, 105, Article 101243. http://dx.doi.org/10.1016/j.progpolymsci.2020.101243, URL: https://www.sciencedirect.com/science/article/ pii/S0079670020300368.
- Rinaudo, M., & Vincendon, M. (1982). 13C NMR structural investigation of scleroglucan. Carbohydrate Polymers, 2(2), 135–144. http://dx.doi.org/10.1016/0144-8617(82)90059-5, URL: http://www.sciencedirect.com/science/article/pii/0144861782900595.
- Ronca, G., & Allegra, G. (1975). An approach to rubber elasticity with internal constraints. Journal of Chemical Physics, 63(11), 4990–4997. http://dx.doi.org/ 10.1063/1.431245.
- Rubinstein, M., & Colby, R. (2003). Polymer physics. Oxford University Press, URL: https://books.google.it/books?id=EJrYoAEACAAJ.
- Rubinstein, M., & Panyukov, S. (2002). Elasticity of polymer networks. Macromolecules, 35(17), 6670–6686. http://dx.doi.org/10.1021/ma0203849.
- Saalwächter, K., & Sommer, J.-U. (2007). NMR reveals non-distributed and uniform character of network chain dynamics. Macromolecular Rapid Communications, 28(14), 1455–1465. http://dx.doi.org/10.1002/marc.200700169, URL: https://onlinelibrary.wiley.com/doi/abs/10.1002/marc.200700169.
- Scherer, G. W. (1994). Hydraulic radius and mesh size of gels. Journal of Sol-Cel Science and Technology, 1(3), 285–291. http://dx.doi.org/10.1007/BF00486171.
  Schurz, J. (1991). Rheology of polymer solutions of the network type. Progress in Polymer Science, 16(1), 1–53. http://dx.doi.org/10.1016/0079-6700(91)90006-7, URL: http://www.sciencedirect.com/science/article/pii/0079670091900067.
- Smirnov, N. (1948). Table for estimating the goodness of fit of empirical distributions. The Annals of Mathematical Statistics, 19(2), 279-281. http://dx.doi.org/ 10.1214/aoms/1177730256.
- Sommer, J. U., & Saalwächter, K. (2005). Segmental order in end-linked polymer networks: A Monte Carlo study. European Physical Journal E, 18(2), 167–182. http://dx.doi.org/10.1140/epie/i2005-10037-3.
- Sommer, J.-U., Vilgis, T. A., & Heinrich, G. (1994). Fractal properties and swelling behavior of polymer networks. Journal of Chemical Physics, 100(12), 9181–9191. http://dx.doi.org/10.1063/1.466673.
- Spencer, A. (1971). Theory of invariants. In A. C. Eringen (Ed.), Continuum physics (pp. 239–353). New York: Academic Press, URL: https://www.sciencedirect. com/science/article/pii/B978012240801450008X.
- Thorne, A. (1988). Spectroscophysics (p. xvi + 390). London: Chapman and Hall Ltd.
- Toda, A. (2011). Weak limit of the geometric sum of independent but not identically distributed random variables. (pp. 1–13). arXiv:1111.1786.
- Treloar, L. (1973). The elasticity and related properties of rubbers. *Reports on Progress in Physics*, 36(7), 755–826. http://dx.doi.org/10.1088/0034-4885/36/7/001. Treloar, L. R. G. (1975). *The physics of rubber elasticity* (3rd ed.). (p. 310). Clarendon Oxford.
- Usatenko, Z., & Sommer, J.-U. (2008). Calculation of the segmental order parameter for a polymer chain in good solvent. *Macromolecular Theory and Simulations*, 17(1), 39-44. http://dx.doi.org/10.1002/mats.200700053.
- Valentín, J. L., Carretero-González, J., Mora-Barrantes, I., Chassé, W., & Saalwächter, K. (2008). Uncertainties in the determination of cross-link density by equilibrium swelling experiments in natural rubber. *Macromolecules*, 41(13), 4717–4729. http://dx.doi.org/10.1021/ma8005087.
- Varga, O. (1966). Polymer reviews, Stress-strain behavior of elastic materials: selected problems of large deformations. Interscience Publishers, URL: https://books.google.it/books?id=w7l-zQEACAAJ.
- Viñarta, S. C., François, N. J., Daraio, M. E., Figueroa, L. I., & Fariña, J. I. (2007). Sclerotium rolfsii scleroglucan: The promising behavior of a natural polysaccharide as a drug delivery vehicle, suspension stabilizer and emulsifier. *International Journal of Biological Macromolecules*, 41(3), 314–323. http: //dx.doi.org/10.1016/j.ijbiomac.2007.04.001, URL: http://www.sciencedirect.com/science/article/pii/S0141813007001043.
- Vilgis, T., & Wilder, J. (1998). Polyelectrolyte networks: elasticity, swelling, and the violation of the Flory-Rehner hypothesis. Computational and Theoretical Polymer Science, 8(1), 61-73. http://dx.doi.org/10.1016/S1089-3156(98)00015-4.
- Wang, X., & Ni, Q. (2003). Determination of cortical bone porosity and pore size distribution using a low field pulsed NMR approach. Journal of Orthopaedic Research, 21(2), 312–319. http://dx.doi.org/10.1016/S0736-0266(02)00157-2.
- Webber, R. E., Creton, C., Brown, H. R., & Gong, J. P. (2007). Large strain hysteresis and mullins effect of tough double-network hydrogels. *Macromolecules*, 40(8), 2919–2927. http://dx.doi.org/10.1021/ma062924y.
- Whittall, K. P., & MacKay, A. L. (1989). Quantitative interpretation of NMR relaxation data. Journal of Magnetic Resonance, 84(1), 134–152. http://dx.doi.org/ 10.1016/0022-2364(89)90011-5, URL: http://www.sciencedirect.com/science/article/pii/0022236489900115.
- Wilber, J. P., & Criscione, J. C. (2005). The Baker-Ericksen inequalities for hyperelastic models using a novel set of invariants of hencky strain. International Journal of Solids and Structures, 42(5), 1547–1559. http://dx.doi.org/10.1016/j.ijsolstr.2004.08.001, URL: https://www.sciencedirect.com/science/article/pii/ S0020768304004482.
- Wu, P., & van der Giessen, E. (1992). On improved 3-D non-Gaussian network models for rubber elasticity. Mechanics Research Communications, 19(5), 427–433. http://dx.doi.org/10.1016/0093-6413(92)90021-2, URL: https://www.sciencedirect.com/science/article/pii/0093641392900212.