

# Eight-hours adaptive deep brain stimulation in patients with Parkinson disease

Mattia Arlotti, PhD,\* Sara Marceglia, PhD,\* Guglielmo Foffani, PhD, Jens Volkmann, MD, PhD, Andres M. Lozano, MD, PhD, Elena Moro, MD, PhD, Filippo Cogiamanian, MD, Marco Prenassi, Ms, Tommaso Bocci, MD, Francesca Cortese, MD, Paolo Rampini, MD, Sergio Barbieri, MD, PhD, and Alberto Priori, MD, PhD

Neurology® 2018;90:e971-e976. doi:10.1212/WNL.00000000000005121

## Correspondence

Prof. Priori  
alberto.priori@unimi.it

## Abstract

### Objectives

To assess the feasibility and clinical efficacy of local field potentials (LFPs)-based adaptive deep brain stimulation (aDBS) in patients with advanced Parkinson disease (PD) during daily activities in an open-label, nonblinded study.

### Methods

We monitored neurophysiologic and clinical fluctuations during 2 perioperative experimental sessions lasting for up to 8 hours. On the first day, the patient took his/her daily medication, while on the second, he/she additionally underwent subthalamic nucleus aDBS driven by LFPs beta band power.

### Results

The beta band power correlated in both experimental sessions with the patient's clinical state (Pearson correlation coefficient  $r = 0.506$ ,  $p < 0.001$ , and  $r = 0.477$ ,  $p < 0.001$ ). aDBS after LFP changes was effective (30% improvement without medication [3-way analysis of variance, interaction day  $\times$  medication  $p = 0.036$ ;  $30.5 \pm 3.4$  vs  $22.2 \pm 3.3$ ,  $p = 0.003$ ]), safe, and well tolerated in patients performing regular daily activities and taking additional dopaminergic medication. aDBS was able to decrease DBS amplitude during motor "on" states compared to "off" states (paired  $t$  test  $p = 0.046$ ), and this automatic adjustment of STN-DBS prevented dyskinesias.

### Conclusions

The main findings of our study are that aDBS is technically feasible in everyday life and provides a safe, well-tolerated, and effective treatment method for the management of clinical fluctuations.

### Classification of evidence

This study provides Class IV evidence that for patients with advanced PD, aDBS is safe, well tolerated, and effective in controlling PD motor symptoms.

## MORE ONLINE

### → Class of Evidence

[NPub.org/coe](http://NPub.org/coe)

## RELATED ARTICLE

### Editorial

Approaching adaptive control in neurostimulation for Parkinson disease: Autopilot on  
Page 497

\*These authors equally contributed to this work.

From the Clinical Center for Neurotechnologies, Neuromodulation, and Movement Disorders (M.A., S.M., F.C., T.B., F.C., P.R., S.B.), Fondazione IRCCS Ca'Granda Ospedale Maggiore Policlinico, Milano; Dipartimento di Ingegneria e Architettura (S.M., M.P.), Università degli Studi di Trieste, Italy; CINAC (G.F.), Hospital Universitario HM Puerta del Sur, and Hospital Nacional de Paraplégicos, Toledo, Spain; Department of Neurology (J.V.), University of Würzburg, Germany; Division of Neurosurgery (A.M.L.), University of Toronto, ON, Canada; Division of Neurology (E.M.), Centre Hospitalier Universitaire de Grenoble, France; Department of Medico-Surgical Sciences and Biotechnologies (F.C.), Sapienza University Rome Polo Pontino, Rome; and "Aldo Ravelli" Research Center (A.P.), Department of Health Sciences, University of Milan & Ospedale San Paolo, Milan, Italy.

Go to [Neurology.org/N](http://Neurology.org/N) for full disclosures. Funding information and disclosures deemed relevant by the authors, if any, are provided at the end of the article.

The Article Processing Charge was funded by Newronika SRL.

This is an open access article distributed under the terms of the Creative Commons Attribution-NonCommercial-NoDerivatives License 4.0 (CC BY-NC-ND), which permits downloading and sharing the work provided it is properly cited. The work cannot be changed in any way or used commercially without permission from the journal.

## Glossary

**aDBS** = adaptive deep brain stimulation; **AE** = adverse event; **ANOVA** = analysis of variance; **DBS** = deep brain stimulation; **LFP** = local field potential; **PD** = Parkinson disease; **UDysRS** = Unified Dyskinesias Rating Scale; **UPDRS III** = Unified Parkinson's Disease Rating Scale, part III.

Optimizing deep brain stimulation (DBS) therapy for patients with Parkinson disease (PD) now seems feasible thanks to the successful results of preliminary studies on closed-loop, adaptive DBS (aDBS) strategies aimed at providing the best stimulation parameters according to the patient's clinical state.<sup>1–5</sup> aDBS is thought to overcome classic DBS therapy limitations, including stimulation-induced side effects in the long term such as gait and speech impairment and the presence of motor fluctuations not well controlled.<sup>6–8</sup>

To adapt stimulation parameters, aDBS uses the synchronous presynaptic and postsynaptic activity of local neuronal populations (local field potentials [LFPs]) recorded through the same implanted electrodes delivering stimulation. The power of the beta band oscillation (11–35 Hz), which is modulated by levodopa administration, movement execution and preparation, motor planning, and DBS,<sup>6–8</sup> is considered the most promising biomarker for aDBS.

Two main adaptation strategies have been tested in humans. The first one is based on an on-off approach that activates DBS only when the LFP beta power exceeds a personalized threshold,<sup>1,2</sup> and the second approach linearly modulates the stimulation voltage according to the changes in the LFP beta power, adapting moment-by-moment DBS parameters to the patient's state.<sup>3,4</sup> In both cases, aDBS proved to be more effective than conventional DBS in improving motor scores,<sup>1</sup> in controlling levodopa-induced dyskinesias,<sup>3,4</sup> and in reducing speech-related side effects.<sup>5</sup>

Despite the positive results, available data were obtained in short experimental sessions, up to 2 hours.<sup>3,4</sup>

As a preliminary step for developing an implantable device, in this work, we aimed to investigate in a long time window in an open-label, nonblinded study whether aDBS is able to follow and control clinical fluctuations using beta band power changes and is well tolerated by and safe for patients.

## Methods

We enrolled 13 rigid-akinetic patients with advanced PD who underwent surgery for subthalamic nucleus DBS electrode implantation in the Neurosurgery Unit at Fondazione IRCCS Ca'Granda Ospedale Maggiore Policlinico in Milan from March 2016 to January 2017 without experiencing any surgical complication. The study was approved by the institutional review board and conformed with the Declaration of Helsinki, and all patients provided written informed

consent to the experimental procedures. Patients were implanted bilaterally but studied unilaterally. The choice of the side is detailed in appendix e-1, <http://links.lww.com/WNL/A238>.

The experimental sessions took place after DBS surgery before the leads were connected to the subcutaneous pulse generator.

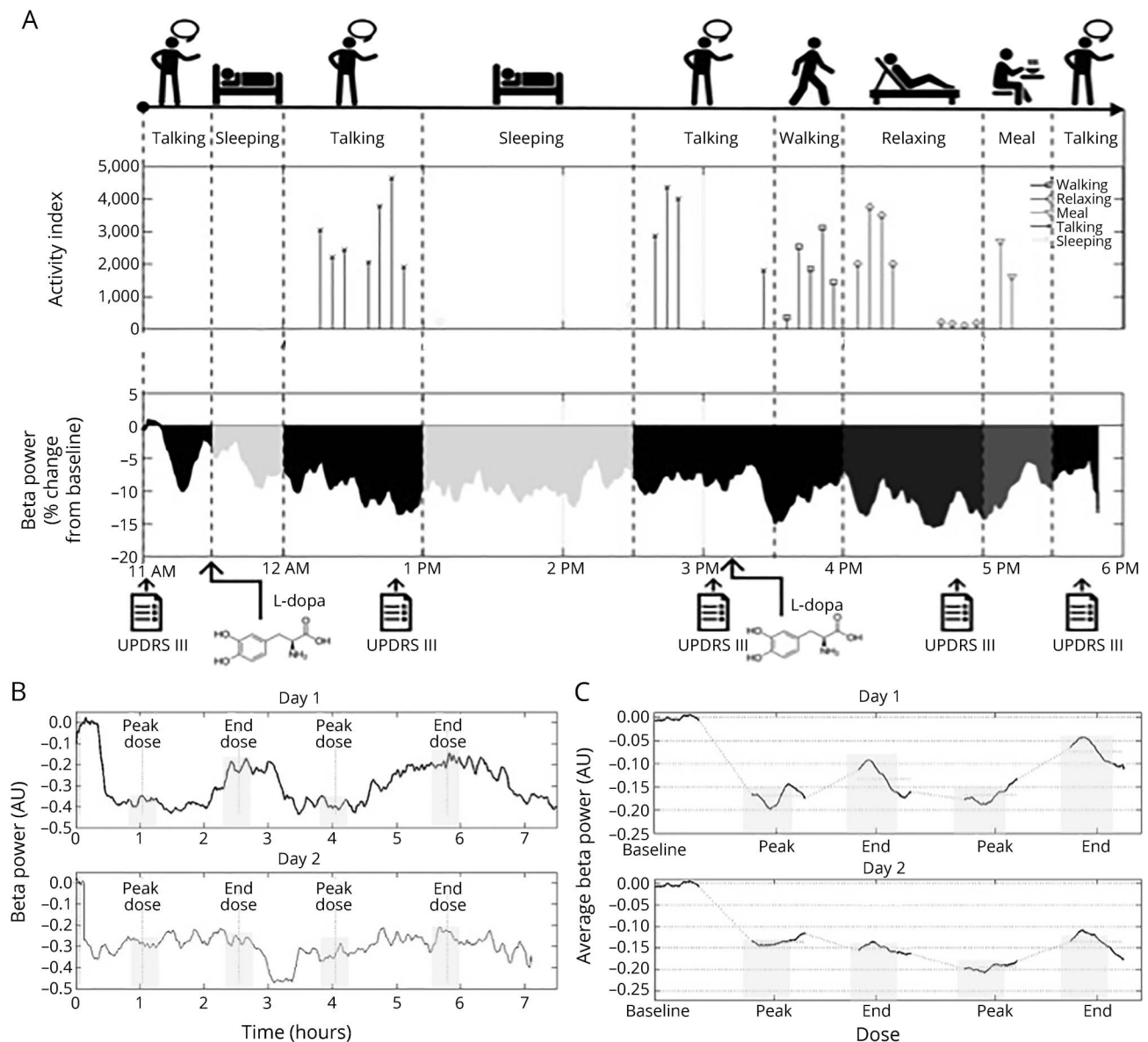
Before the experimental session started, a calibration session was performed to verify the presence of a significant beta peak in at least 1 side, to establish the best side for recording LFPs and testing aDBS, and to establish effective stimulation parameters (appendix e-1, <http://links.lww.com/WNL/A238>). Because, according to the literature,<sup>9</sup> we expected that the beta peak was not detectable in all patients and because the current aDBS algorithm is based on beta band modulations, those not showing a beta peak were excluded from the study.

The experimental protocol (figure 1A) included two 8-hour sessions (1 per day) conducted with a portable aDBS prototype device<sup>9</sup>: day 1, stimulation “off” and LFP recordings “on”; and day 2, stimulation “on” (aDBS) and LFP recordings “on.”

After 12 hours of medication withdrawal, each session started with a baseline assessment (medication “off,” stimulation “off”). The patient took his/her first morning medication afterward and was then assessed when his/her medication was effective (medication “on,” peak dose ≈45–60 minutes after medication intake) and then when the medication ended its effects (medication “off,” end dose 60–90 minutes after the peak dose). The same procedure was repeated throughout the 8 hours (figure 1A). According to the personal response timing, each patient took 2 or 3 medications. Hence, to allow comparisons, we considered the clinical assessments related to the first 2 administrations. On day 2, DBS was switched “on” at the beginning of the experimental session, immediately after the baseline assessment. The clinical assessments on day 2 followed the same schema as on day 1, according to levodopa response (peak dose, end dose).

For the clinical assessment, we collected the Unified Parkinson's Disease Rating Scale, part III, motor part (UPDRS III), the Unified Dyskinesias Rating Scale (UDysRS), parts 3 and 4, and the adverse events (AEs) experienced by the patient (appendix e-1, <http://links.lww.com/WNL/A238> for AE classification).

**Figure 1** Experimental protocol and aDBS functioning



(A) Top timeline shows the activities recorded during the 8 hours (10 AM–6 PM) for a representative patient. Middle plot represents the activity index (i.e., a custom index based on accelerometer data in the band of 0.5–4 Hz representing the amount of motor activity) corresponding to each activity, and the bottom trace is beta power percentage change from baseline throughout the 8 hours. Bottom arrows show the times in which the patient was assessed (baseline, peak dose 1, end dose 1, peak dose 2, end dose 2) and received levodopa. (B) Beta power changes from baseline in day 1 (top trace) and day 2 (bottom trace) of a representative patient (patient 4). The x-axis represents time (hours) and y-axis represents percent beta power change from baseline. Gray rectangles highlight beta power during clinical assessments (baseline, peak dose 1, end dose 1, peak dose 2, end dose 2). (C) Average beta power changes from baseline in day 1 (top trace) and day 2 (bottom trace). Only the time windows of  $\pm 10$  minutes around clinical assessments were represented to allow averaging among patients. The x-axis represents time (hours) and y-axis represents percent beta power change from baseline. Gray rectangles highlight beta power during clinical assessments (baseline, peak dose 1, end dose 1, peak dose 2, end dose 2). aDBS = adaptive deep brain stimulation; AU = arbitrary units; UPDRS = Unified Parkinson's Disease Rating Scale.

To assess the aDBS device function throughout the whole 8-hour session, we collected the beta band power and, on day 2, the stimulation amplitude. We correlated the clinical assessment with the beta power corresponding to the time at which the UPDRS III was assessed ( $\pm 10$  minutes). We also collected the patient's physical activity using a wearable commercial bracelet equipped with a 3-axis accelerometer. A dedicated application was developed to acquire and store data

and to provide a clinical diary (sleep, rest, walk, talk, eat, other) to be filled in by the patient every 30 minutes.

We used data on day 1 to verify the ability of beta band power to act as a biomarker of patient's state, and more specifically, we tested whether the beta power was modulated by levodopa using nonsupraliminal levodopa doses (paired *t* test beta power "off" vs beta power "on,"  $p < 0.05$ ), the beta power

correlated to the patient's clinical state as measured by the UPDRS III (Pearson correlation coefficient,  $p < 0.05$ ), and the beta power correlated with the specific physical activities as measured by the wearable bracelet (Pearson correlation coefficient,  $p < 0.05$ ).

aDBS efficacy was assessed by a comparison of clinical data (UPDRS III and UDysRS) collected on day 1 vs 2 (3-way analysis of variance [ANOVA] with the factors day [2 levels, day 1 and day 2], condition [2 levels, medication "on" and medication "off"], and administration [2 levels, administration 1 and administration 2]). aDBS safety was verified by the occurrence and intensity of AEs related to stimulation. Data here are reported as mean  $\pm$  standard error.

## Results

We screened 13 patients (table 1). Of them, only 1 patient (patient 5) did not show a significant beta peak, and we lost the entire day 1 recording of patient 6 because of battery discharge. Hence, we analyzed 11 patients. Experimental details are reported in table e-1, <http://links.lww.com/WNL/A237>.

In day 1, we found that the beta power responded to levodopa administration, as expected, with an average decrease of  $18.0 \pm 0.03\%$  in peak dose compared to a  $8.3 \pm 0.03\%$  in end dose ( $p = 0.009$ ) with respect to baseline (medication "off,"

stimulation "off," after 12 hours of levodopa withdrawal). In addition, the beta power was confirmed to correlate with the patient's clinical state as measured by the UPDRS III (Pearson correlation coefficient = 0.477,  $p < 0.001$ ) and was specifically modulated during walking with respect to talking and relaxing (beta power change from baseline during: walking  $-14.0 \pm 4.212\%$ , talking  $-11.2 \pm 2.724\%$ , relaxing  $-8.8 \pm 2.418\%$ , 1-way ANOVA  $p < 0.0001$ ).

On day 2 (figure 2), we observed that aDBS was effective in reducing UPDRS III motor scores by almost 30% when the patients were "off" medication, whereas no improvement was observed in day 1 when the patients did not receive aDBS (baseline vs medication "off": day 1,  $32.6 \pm 2.8$  vs  $29.4 \pm 3.9$ ; day 2,  $30.5 \pm 3.4$  vs  $22.2 \pm 3.3$ ; 3-way ANOVA interaction day  $\times$  levodopa  $p = 0.036$ ; post hoc test  $p = 0.003$ ). When the patients were "on" levodopa, the cumulative effect of aDBS and levodopa provided a 45% improvement in the UPDRS III motor scores that was comparable to that elicited by levodopa alone on day 1 (baseline vs medication "on": day 1,  $32.6 \pm 2.8$  vs  $17.9 \pm 2.0$ ; day 2,  $30.5 \pm 3.4$  vs  $15.5 \pm 2.3$ ; post hoc test  $p = 0.4$ ). The cumulative effect of levodopa and aDBS did not elicit dyskinesias (medication "off" vs medication "on": day 1,  $3.4 \pm 1.0$  vs  $5.8 \pm 1.7$ ; day 2,  $3.5 \pm 0.9$  vs  $4.4 \pm 1.5$ ; 3-way ANOVA interaction day  $\times$  levodopa  $p = 0.51$ ). In fact, as expected, the amount of stimulation voltage delivered when the patient was on levodopa peak was significantly lower than that delivered when the patient was in the end peak

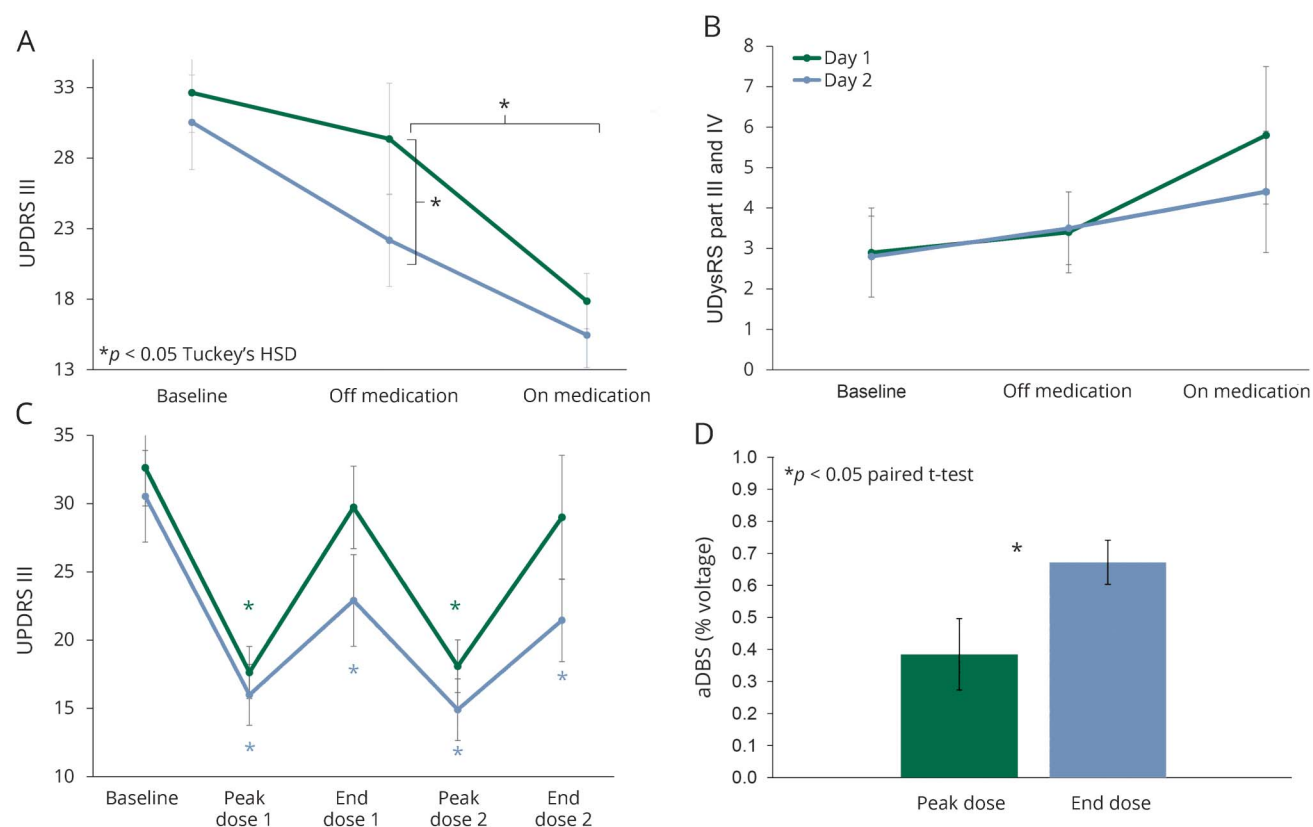
**Table 1** Patients' preoperative clinical details

Case	Sex	Age, y	Disease duration, y	Fluctuation onset, y	Onset side	Preoperative LEDD	Preoperative response to levodopa <sup>a</sup>		
							UPDRS III score, medication "off"	UPDRS III score, medication "on"	
1	1	M	59	10	6	R	208	25	13
2	2	M	62	9	6	R	685.55	41	18
3	3	M	67	12	5	R	1,494	25	10
4	4	M	50	8	5	R	1,055	32	16
5	5	M	47	11	2.5	R	1,080	19	10
6	6	M	58	7	2	R	1,856.66	37	11
7	7	F	65	14	4	L	652	22	8
8	8	M	70	12	2	L	872	13	3
9	9	F	47	7	2	L	1,436.1	24	8
10	10	M	54	13	4.5	L	785	24	8
11	11	M	59	14	12	L	665	30	10
12	12	F	58	11	5	L	1,250	39	16
13	13	F	70	13	7	L	208	25	12

Abbreviations: LEDD = levodopa equivalent daily dose; UPDRS = Unified Parkinson's Disease Rating Scale.

<sup>a</sup> Preoperative response to levodopa refers to UPDRS III score assessed by a neurologist at the time of indication for DBS surgery ( $\approx$ 6 months before surgery).

**Figure 2** aDBS efficacy on day 2



(A) Graph represents average UPDRS III values on day 1 (green line) and day 2 (light gray line) at baseline, at end dose/medication “off,” and at peak dose/medication “on.” Error bars are SEMs. UPDRS III values at end dose/medication “off” on day 1 were significantly different from those on day 2 and from those on peak dose/medication “on” on the same day 1. (B) Graph represents average UDysRS, part III and IV values on day 1 (green line) and on day 2 (light gray line) at baseline, at end dose/medication “off,” and at peak dose/medication “on.” Error bars are SEMs. No significant differences were detected among conditions. (C) Details of the UPDRS III values on day 1 (green line) and on day 2 (light gray line) at baseline, at end dose/medication “off,” and at peak dose/medication “on” in the 2 sessions throughout the whole 8-hour experiment. On day 1, only values at peak dose/medication “on” were different from baseline values, whereas on day 2, the difference was significant at all time points after aDBS was turned on. (D) Histogram represents the average voltage change in the peak dose/medication “on” condition (green) and in the end dose/medication “off” (light gray) during day 2. Error bars are SEMs. aDBS = adaptive deep brain stimulation; HSD = highest significant difference; UPDRS = Unified Parkinson’s Disease Rating Scale; UDysRS = Unified Dyskinesias Rating Scale.

(normalized stimulation voltage as a percent of the maximum voltage in table e-1, <http://links.lww.com/WNL/A237>, medication “off” vs medication “on”:  $0.67 \pm 0.23$  vs  $0.38 \pm 0.37$ , paired *t* test  $p = 0.046$ ). As a further verification of the aDBS functioning, we found that the beta power was confirmed to correlate with the patient’s clinical state as measured by the UPDRS III (Pearson correlation coefficient = 0.506,  $p < 0.001$ ) even in day 2. Finally, no AEs specifically related to aDBS or complaints regarding either the experimental procedure or the device/stimulation were reported.

## Discussion

In our 8-hour experiment, our aDBS device provided a stimulation output that was always calibrated to the beta rhythm and to the patient’s state.

To the best of our knowledge, this is the longest experiment with aDBS. Previous experiments with aDBS from our group and other laboratories showed aDBS effectiveness in shorter time

windows.<sup>1-5</sup> Our observations showed that changing DBS voltage linearly with beta rhythm provides constant benefit for hours of unrestricted patient activity and in conjunction with normal levodopa assumption. Conversely, in previous experiments, to understand whether aDBS was able to control stimulation side effects better than conventional DBS, patients were administered a supraliminal dose of levodopa, able to induce dyskinesias, especially if summed to DBS.<sup>3,4</sup>

Despite these new insights provided by the current experiment, this study has some limitations. First, aDBS was delivered with an external prototype immediately after the surgery for DBS electrode placement, in the so-called acute experimental setting. In this time window, several adaptation processes at the level of the tissue-electrode interface occur, and the presence of edema and the lesional effect due to electrode insertion limit the possibility to mimic the more stable chronic phase. In addition, unilateral aDBS was applied, and the study was conducted in an open-label, unblinded fashion. Finally, the analysis of daily of life activities (e.g., talking, relaxing, sleeping) was based on a self-reporting diary

and on the data from a single accelerometer placed on the patient's wrist in 30-minute time windows. This provided an indication of the predominance of a certain activity during this time frame, and it cannot track the probable co-occurrence of different activities. To account for this intrinsic inaccuracy, the beta power was studied in average during the time frame. This approach, however, provided evidence of an average correlation between the beta power and the patient's activity that should be better studied with more quantitative approaches based on multiple sensors.

Although still obtained in an acute experimental setting a few days after DBS surgery, our results show that beta band-based aDBS can induce stable control of PD-related motor disturbances by adapting stimulation parameters according to the patient's state. Overall, this finding is a step forward in the development of the new generation of implantable aDBS devices for treating PD.

### Author contributions

Mattia Arlotti: study design and concept, data acquisition, analysis and interpretation, manuscript drafting. Sara Marceglia: study concept, data analysis and interpretation, statistical analysis, manuscript drafting. Guglielmo Foffani: data interpretation, critical revision of manuscript for intellectual content. Jens Volkmann, Andres M. Lozano, and Elena Moro: critical revision of manuscript for intellectual content. Filippo Cogiamanian: data acquisition. Marco Prenassi: data analysis. Tommaso Bocci, Francesca Cortese, and Paolo Rampini, data acquisition. Sergio Barbieri: critical revision of manuscript for intellectual content. Alberto Priori: study concept and design, critical revision of manuscript for intellectual content.

### Study funding

The study was partly supported by donation in memory of Aldo Ravelli and by grant GR-2011-02352807 from the Italian Ministry of Health.

### Disclosure

M. Arlotti reports no disclosures relevant to the manuscript. S. Marceglia and G. Foffani: shareholder of Newronika Srl, a spinoff company of the Fondazione IRCCS Ca'Granda Ospedale Maggiore Policlinico and of the University of Milan. J. Volkmann, A. Lozano, and E. Moro: member of the scientific advisory board of Newronika Srl, a spinoff company of the Fondazione IRCCS Ca'Granda Ospedale Maggiore Policlinico and of the University of Milan. F. Cogiamanian: shareholder of Newronika Srl, a spinoff company of the Fondazione IRCCS Ca'Granda Ospedale Maggiore Policlinico and of the University of Milan. M. Prenassi, T. Bocci, and F. Cortese report no disclosures relevant to the manuscript. P. Rampini, S. Barbieri, and A. Priori: shareholder of Newronika Srl, a spinoff company of the Fondazione IRCCS Ca'Granda Ospedale Maggiore Policlinico and of the University of Milan. Go to [Neurology.org/N](#) for full disclosures.

Received August 4, 2017. Accepted in final form December 20, 2017.

### References

1. Little S, Pogossyan A, Neal S, et al. Adaptive deep brain stimulation in advanced Parkinson disease. *Ann Neurol* 2013;74:449–457.
2. Little S, Beudel M, Zrinzo L, et al. Bilateral adaptive deep brain stimulation is effective in Parkinson's disease. *J Neurol Neurosurg Psychiatry* 2016;87:717–721.
3. Rosa M, Arlotti M, Ardolino G, et al. Adaptive deep brain stimulation in a freely moving Parkinsonian patient. *Mov Disord* 2015;30:1003–1005.
4. Rosa M, Arlotti M, Marceglia S, et al. Adaptive deep brain stimulation controls levodopa-induced side effects in Parkinsonian patients. *Mov Disord Epub* 2017 Feb 17.
5. Little S, Tripoliti E, Beudel M, et al. Adaptive deep brain stimulation for Parkinson's disease demonstrates reduced speech side effects compared to conventional stimulation in the acute setting. *J Neurol Neurosurg Psychiatry Epub* 2016 Aug 16.
6. Fasano A, Aquino CC, Krauss JK, Honey CR, Bloem BR. Axial disability and deep brain stimulation in patients with Parkinson disease. *Nat Rev Neurol* 2015;11:98–110.
7. Rodriguez-Oroz MC, Moro E, Krack P. Long-term outcomes of surgical therapies for Parkinson's disease. *Mov Disord* 2012;27:1718–1728.
8. Krack P, Martinez-Fernandez R, del Alamo M, Obeso JA. Current applications and limitations of surgical treatments for movement disorders: surgical treatments for movement disorders. *Mov Disord* 2017;32:36–52.
9. Giannicola G, Marceglia S, Rossi L, et al. The effects of levodopa and ongoing deep brain stimulation on subthalamic beta oscillations in Parkinson's disease. *Exp Neurol* 2010;226:120–127.

# Eight-hours adaptive deep brain stimulation in patients with Parkinson disease

Mattia Arlotti, PhD, Sara Marceglia, PhD, Guglielmo Foffani, PhD, Jens Volkmann, MD, PhD, Andres M. Lozano, MD, PhD, Elena Moro, MD, PhD, Filippo Cogiamanian, MD, Marco Prenassi, Tommaso Bocci, MD, Francesca Cortese, MD, Paolo Rampini, MD, Sergio Barbieri, MD, PhD, and Alberto Priori, MD, PhD

## Correspondence

Dr. Priori  
alberto.priori@unimi.it

Cite as: *Neurology*® 2018;90:e971-e976. doi:10.1212/WNL.0000000000005121

## Study question

Is local field potential (LFP)-based adaptive deep brain stimulation (aDBS) administered during daily activities feasible and effective for patients with advanced Parkinson disease (PD)?

## Summary answer

LFP-based aDBS is a feasible, safe, well-tolerated, and effective way to manage these patients' clinical fluctuations.

## What is known and what this paper adds

LFP-based aDBS may provide improvements over classic DBS techniques, but available evidence comes from experimental sessions that only lasted up to 2 hours. This study provides Class IV evidence for the feasibility and efficacy of LFP-based aDBS over longer sessions, up to 8 hours.

## Participants and setting

This study examined 13 patients with rigid-akinetic advanced PD at a Department of Clinical Neurology and Neurosurgery in Milan, Italy between March 2016 and January 2017.

## Design, size, and duration

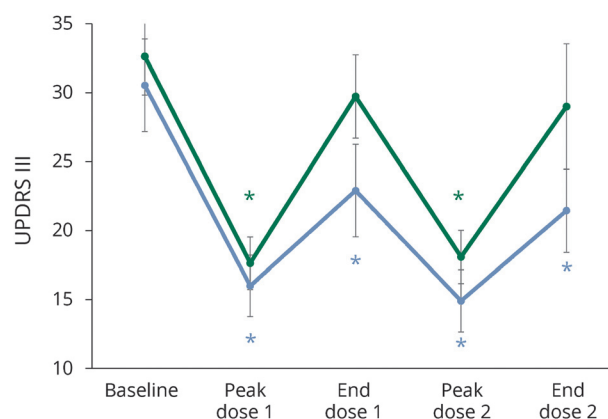
The participants underwent surgical insertion of DBS electrodes into the subthalamic nucleus and then underwent two 8-hour experimental sessions over consecutive days. LFP recordings were conducted during both sessions, but aDBS was activated only in the second session. The patients took their prescribed medications on both days. Clinical assessments were made based on the Unified PD Rating Scale (UPDRS), the Unified Dyskinesias Rating Scale, and adverse events.

## Primary outcomes

The primary outcomes were correlations during long lasting recordings (up to 8 hours) between beta band power and UPDRS scores and comparisons between UPDRS scores on days 1 and 2.

## Main results and the role of chance

Beta band power correlated with UPDRS scores on days 1 (Pearson's  $r = 0.477$ ;  $p < 0.001$ ) and 2 (Pearson's  $r = 0.506$ ;  $p < 0.001$ ). Activating aDBS achieved a nearly 30% reduction in



day 2 UPDRS motor scores when patients were “off” levodopa that was not observed when comparing analogous timepoints on day 1 ( $p = 0.003$ ). When patients were “on” levodopa, the combined effect of aDBS and levodopa on day 2 was a ~45% reduction in UPDRS motor scores comparable to that observed for levodopa alone on day 1 ( $p = 0.4$ ). No aDBS-related adverse events, including dyskinesia, were reported.

## Bias, confounding, and other reasons for caution

This was an unblinded open-label study. The experiments were conducted immediately after implantation surgeries, so adaptation processes had not yet occurred.

## Generalizability to other populations

The aDBS algorithm here validated is specific for PD-STN target, but the feasibility and safety of the aDBS approach is potentially generalizable to other DBS indications.

## Study funding/potential competing interests

This study was funded by private donations and the Italian government. Some authors report having financial interests in Newronika Srl. Go to [Neurology.org/N](http://Neurology.org/N) for full disclosures.

A draft of the short-form article was written by M. Dalefield, a writer with Editage, a division of Cactus Communications. The authors of the full-length article and the journal editors edited and approved the final version.

# Neurology®

## **Eight-hours adaptive deep brain stimulation in patients with Parkinson disease**

Mattia Arlotti, Sara Marceglia, Guglielmo Foffani, et al.

*Neurology* 2018;90:e971-e976 Published Online before print February 14, 2018

DOI 10.1212/WNL.0000000000005121

### **This information is current as of February 14, 2018**

<b>Updated Information &amp; Services</b>	including high resolution figures, can be found at: <a href="http://n.neurology.org/content/90/11/e971.full.html">http://n.neurology.org/content/90/11/e971.full.html</a>
<b>Supplementary Material</b>	Supplementary material can be found at: <a href="http://n.neurology.org/content/suppl/2018/02/14/WNL.0000000000005121.DC1">http://n.neurology.org/content/suppl/2018/02/14/WNL.0000000000005121.DC1</a>
<b>References</b>	This article cites 7 articles, 1 of which you can access for free at: <a href="http://n.neurology.org/content/90/11/e971.full.html##ref-list-1">http://n.neurology.org/content/90/11/e971.full.html##ref-list-1</a>
<b>Subspecialty Collections</b>	This article, along with others on similar topics, appears in the following collection(s): <b>Basal ganglia</b> <a href="http://n.neurology.org/cgi/collection/basal_ganglia">http://n.neurology.org/cgi/collection/basal_ganglia</a> <b>Motor Control</b> <a href="http://n.neurology.org/cgi/collection/motor_control">http://n.neurology.org/cgi/collection/motor_control</a> <b>Parkinson's disease/Parkinsonism</b> <a href="http://n.neurology.org/cgi/collection/parkinsons_disease_parkinsonism">http://n.neurology.org/cgi/collection/parkinsons_disease_parkinsonism</a>
<b>Permissions &amp; Licensing</b>	Information about reproducing this article in parts (figures, tables) or in its entirety can be found online at: <a href="http://n.neurology.org/misc/about.xhtml#permissions">http://n.neurology.org/misc/about.xhtml#permissions</a>
<b>Reprints</b>	Information about ordering reprints can be found online: <a href="http://n.neurology.org/misc/addir.xhtml#reprintsus">http://n.neurology.org/misc/addir.xhtml#reprintsus</a>

*Neurology*® is the official journal of the American Academy of Neurology. Published continuously since 1951, it is now a weekly with 48 issues per year. Copyright © 2018 The Author(s). Published by Wolters Kluwer Health, Inc. on behalf of the American Academy of Neurology. All rights reserved. Print ISSN: 0028-3878. Online ISSN: 1526-632X.

