SCIENTIFIC REPORTS

OPEN

Edge-subtraction X-ray ptychographic imaging with pink beam synchrotron radiation and a single photon-counting detector

Francesco Brun^{1,2*}, Vittorio Di Trapani^{3,4}, Darren Batey⁵, Silvia Cipiccia⁵ & Christoph Rau⁵

We present here a new method of performing X-ray edge-subtraction ptychographic imaging by combining multiple harmonics from an undulator synchtrotron source and an energy discriminating photon counting detector. Conventionally, monochromatic far-field X-ray ptychography is used to perform edge subtraction through the use of multiple monochromatic energy scans to obtain spectral information for a variety of applications. Here, we use directly the undulator spectrum from a synchrotron source, selecting two separate harmonics post sample using the Pixirad-1/Pixie-III detector. The result is two monochromatic images, above and below an absorption edge of interest. The proposed method is applied to obtain Au L-edge subtraction imaging of a Au-Ni grid test sample. The Au L-edge subtraction is particularly relevant for the identification of gold nanoparticles for biomedical applications. Switching the energy scan mechanism from a mechanical monochromator to an electronic detector threshold allows for faster spectral data collection with improved stability.

X-ray spectral imaging captures the energy-dependant response of a sample at every imaging element, mapping directly the elemental, chemical or magnetic information to the spatial structure^{1,2}. Edge-subtraction imaging is a type of spectral imaging where two images are acquired at two different energies across an absorption edge. Element identification is performed by digital subtraction of the two images, the resultant image is easily segmented and analysed. Although mainly exploited with monochromatic sources, spectral imaging with polychromatic sources is feasible by using energy resolving X-ray detectors³.

X-ray ptychography, a scanning coherent small angle scattering technique⁴, is now widely used at synchrotron sources to provide quantitative phase information at the highest resolutions across extended fields of view without the need for high quality optical elements⁵. The method relies on the phasing of diffraction intensities and so it requires a certain degree of spatial and temporal coherence^{6,7}. Conventional spectro-ptychography is achieved via an energy scan across an absorption edge and it has successfully been proved both in soft and hard X-ray regime for magnetic domain imaging^{8,9}.

Recently, single acquisition K-edge subtraction (KES) ptychography has been demonstrated within a single undulator harmonic using a hyperspectral detector¹⁰. However, the detector used suffers from a low flux tolerance resulting in relatively long acquisition times. Here we demonstrate a new modality for edge-subtraction ptychography that makes use of multiple undulator harmonics and a multiple threshold X-ray Photon Counting Detector (XPCD) — the Pixirad-1/Pixie-III¹¹ — as an harmonic selector. The nature of the Pixie-III is such that the acceptable count rate is significantly higher compared to a hyperspectral detector¹², resulting in faster acquisition times while still offering energy discriminating capabilities. The detector is capable of operating at more than 500 Hz, with 10⁵ counts s⁻¹ pixel⁻¹, giving the potential of spectroscopic ptychography at $2.6 \cdot 10^7$ photons mm⁻²s⁻¹.

We apply the proposed method to L-edge subtraction (LES) of a Au-Ni test grid as well as to a Siemens star. The experiment was carried out at the I13-1 coherence branchline¹³ of the Diamond Light Source. The undulator spectrum was filtered to isolate two harmonics, above and below the L-edge of Au, and the Pixirad-1/Pixie-III

¹Department of Engineering and Architecture, University of Trieste, Trieste, Italy. ²National Institute for Nuclear Physics (INFN) - Trieste division, Trieste, Italy. ³Department of Physical Sciences, Earth and Environment, University of Siena, Siena, Italy. ⁴National Institute for Nuclear Physics (INFN) - Pisa division, Pisa, Italy. ⁵Diamond Light Source, Harwell Science and Innovation Campus, Fermi Avenue, Didcot, OX11 0QX, UK. *email: fbrun@units.it



Figure 1. (a) Filtered incident pink beam at the sample position as measured with the PCO4000 detector while performing an energy scan (orange, solid) and differential X-ray spectrum as detected by Pixirad-1/Pixie-III (blue, stars) assessed via the threshold scan at a few selected values. (b) Detector's bandwidth when adopting the energy threshold settings to discriminate the 11.0 keV and the 13.8 keV peaks as measured at a few selected energy points.

detector was used to separate these harmonics thanks to its tunable energy thresholds. The results from the new method are compared with those obtained with conventional monochromatic LES imaging. We demonstrate firstly that this is possible with the bandwidth of a single undulator harmonic and secondly also that the harmonic selection can be achieved with an electronic threshold configuration, thus removing the need for a monochromator.

Results

Threshold settings and detector bandwidth. The Pixirad-1/Pixie-III XPCD coupled to a CdTe sensor was used for the experiment. This detector has two programmable energy thresholds, T_{low} and T_{high} . The detector can operate in either integration or colour mode. In integration mode a single threshold is applied and a single image of the integration of all the counts above the threshold is produced. In colour mode Pixirad-1/Pixie-III outputs two images in a single acquisition: the first is the integration of the counts between T_{low} and T_{high} . The second is the integration of the counts above T_{high} . This modality has already been successfully explored to perform KES computed tomography¹⁴.

Discriminating between the two harmonics in the reported experiment requires an accurate setting of the energy thresholds. The undulator X-ray spectrum at the sample, as recorded with an imaging detector (PCO4000 camera) during an energy scan performed using the monochromator, is shown in Fig. 1a. The 4th harmonic at 11.0 keV is below the Au L-edge and the 5th harmonic at 13.8 keV is above. The bandwidth is 0.33 keV (Full Width Half Maximum - FWHM) for both the 4th and 5th harmonics, which enforces a spatial resolution limit of 113 nm⁶. Figure 1a also reports the differential X-ray spectrum detected by Pixirad-1/Pixie-III assessed via the so-called threshold scan at a few selected values. The counts above one single energy threshold were recorded for increasing values of this threshold in the range [6.0, 18.0] keV. Then, the difference between two adjacent measured values were used for the reported spectrum.

The optimal levels of T_{low} and T_{high} to isolate the harmonics is an optimisation between the finite energy resolution of the detector^{15,16} as reported in Fig. 1b) and the photon statistics. Narrower threshold separations produce images with a higher degree of monochromaticity but at the expense of photon statistics, thus increasing exposure times. Also, having the two thresholds too close can result in unresponsive pixels, because of single pixel miscalibration of the energy thresholds¹⁷. The following settings were found as optimal: for the "below" image, the detector energy thresholds were set at values of $T_{low} = 9.6 \text{ keV}$ and $T_{high} = 10.4 \text{ keV}$, whereas $T_{low} = 12.5 \text{ keV}$ and $T_{high} = 14.8 \text{ keV}$ were used for the "above" acquisition. It is worth noting that, in order to minimise the contamination between the adjacent harmonics, the energy windows were not centered onto the harmonic peaks but slightly shifted apart, to 10.8 keV and 14.3 keV, respectively.

Figure 1b shows the detector's bandwidth at the two chosen settings. These were measured by scanning the energy of the X-ray beam with the Si(111) monochromator available at the beamline and dividing the counts between the thresholds by the total number of counts recorded by the detector. The red circles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "below" and the blue triangles represent the bandwidth with the thresholds set for the harmonic "above". For both bandwidths an effective energy spread (FWHM) of 3 keV was measured, which is in agreement with previous similar independent measurements¹⁶.

Pink beam LES ptychography of a Au-Ni micro-grid. The LES imaging of a Au-Ni micro-grid test sample was performed in both monochromatic and pink beam mode. In both cases, two separate acquisitions were required, both above and below the Au L-edge. The illumination was defined by a 5 m diameter pinhole. The acquisitions consisted of a 40×40 regular snake scan, with a step size of 2 m (80% beam overlap) and 5 s exposure. For the monochromatic images the Si(111) monochromator was placed in the beam



Figure 2. Top row: reference reconstructed images (modulus of the complex-valued ptychographs) acquired with the detector in energy integration mode and by using monochromatic beams at 11.0 keV (**a**) and 13.8 keV (**b**). The digital subtraction of (**a**,**b**) is reported in (**c**). Bottom row: reconstructed images acquired by using pink beam and the detector in colour mode when considering $[T_{low}, T_{high}] = [9.6, 10.4]$ keV (**d**) and $[T_{low}, T_{high}] = [12.5, 14.8]$ keV (**e**). The digital subtraction of (**d**,**e**) is reported in (**f**). [Scale bar = 25.0 m. Color bar for the above and below images representing the X-ray transmission].

path, the 4th (11.0 keV) and the 5th harmonics (13.8 keV) were selected in the two consecutive acquisitions. Pixirad-1/Pixie-III was configured in energy integration mode. The top row of Fig. 2 shows the reconstructed object modulus of the complex-valued ptychographs from below and above the absorption edge along with their digital subtraction. For the pink beam acquisition, the monochromator was removed from the beam path. The detector was set in colour mode and the two images were acquired consecutively with the optimised setting for T_{low} and T_{high} as described in the previous section. Figure 2d–f shows the reconstructed object modulus for the below, the above, and the corresponding digital subtraction images, respectively. In both monochromatic and pink beam mode the Au is successfully isolated via digital subtraction of the images across the edge.

Pink beam ptychography of a siemens star. A Siemens star test sample was imaged to evaluate the achievable resolution of the experiment when considering object phase reconstructed images. The acquisition consisted of scanning the sample with the same parameters as for the micro-grid sample, but with 38×38 points. Again, for the monochromatic references images the Si(111) monochromator was placed in the beam path and the 4th (11.0 keV) and the 5th harmonic (13.8 keV) were selected in the two consecutive acquisitions by using Pixirad-1/Pixie-III in energy integration mode. The top row of Fig. 3 shows the reconstructed object phase at the two considered monochromatic energies. For the pink beam acquisition, the monochromator was removed from the beam path and compound refractive lenses (CRLs) were added into the beam path. The detector was set in colour mode and the two images were acquired consecutively with the optimised setting for T_{low} and T_{high} as previously described. The reconstructed object phase of the complex-valued ptychographs is shown in Fig. 3. The spatial resolution obtained for the monochromatic and pink beam cases is similar. For each case, the Modulation Transfer Function was formed over a diagonal spoke. The best result of 141 nm was recorded for the reference monochromatic image at 13.8 keV and the worst case of 167 nm was recorded for the pink beam image with detector settings of $[T_{low}, T_{high}] = [9.6, 10.4]$ keV. The achieved resolution of approximately 150 nm is a factor of 67 greater than that resolved by the 5 m probe (beam) size alone. The Universal Quality Index (UQI) was used to estimate the similarity between the two sets of results. The UQI is in the [-1, +1] range and values towards +1 correspond to higher similarities between the images. We obtained for the monochromatic-pink beam comparison a UQI = 0.67 at 11.0 keV and a UQI = 0.70 at the 13.8 keV, which confirm the strong similarity of the results.



Figure 3. Reconstructed images (phase of the complex-valued ptychographs) of the Siemens star acquired by using monochromatic beams at 11.0 keV (**a**) and 13.8 keV (**b**). Reconstructed images by using pink beam and the detector in colour mode when considering $[T_{low}, T_{high}] = [9.6, 10.4]$ keV (**c**) and $[T_{low}, T_{high}] = [12.5, 14.8]$ keV (**d**). [Scale bar = 2.5 m].

Discussion

We have presented the first results of spectral edge subtraction ptychographic imaging using multiple undulator harmonics and a multi-energy threshold XPCD. LES imaging of a test sample was performed and compared with conventional monochromatic images. The harmonic separation required depends on the specific edge of interest. The considered experiment aims at LES imaging and L-edge is generally weaker than the K-edge so a narrow separation of the harmonics is required. This means that a fine tuning of the detector thresholds is needed. We have proved that, with optimized threshold settings, the quality of the pink beam reconstructed images is comparable to those acquired with monochromatic settings. The edge subtraction process is a precursor for further image segmentation and quantification. Although imperfections in the subtracted images are visible, simple segmentation by gray-level thresholding (slightly above the background noise) accurately isolates the target material.

Pixirad-1/Pixie-III used during the experiment is coupled with a CdTe sensor, which is generally conceived for high-energy imaging¹⁸. We therefore also expect the methodology outlined here to be valid at higher energies. The use of high-energy X-rays in ptychography is very attractive for their larger penetration power, the depth of focus increases for a given resolution, the dose delivered to the sample is potentially lowered, and shorter wavelengths give access to higher resolution information. Moreover, for the specific case of edge subtraction (ES) ptychography, higher-energy X-rays are required to reach the absorption edges of high-Z elements.

The polychromatic source used in this experiment consists of a comb-like spectrum with energy peaks of different amplitudes. The photon statistics might be significantly different for different energy windows. Filtering of the beam and the detector exposure time can be tuned to mitigate amplitude and consequent signal-to-noise ratio variations. However, in the case of pronounced asymmetry in the energy peaks, attention should be paid to avoid a non-linear response or, even worse, the paralysis of the detector with a high photon flux.

The two images required for the ES were acquired without the need of a monochromator and any mechanical scan of it. This could be beneficial since the stabilization of high-heat-load double-crystal monochromators is one of the most critical challenges for their effective utilization in diffraction-limited storage rings¹⁹. In addition, having more than two energy thresholds²⁰ would allow for the edge subtraction to be performed in a single acquisition. Collecting the data in a single acquisition would be beneficial for the stability and quality of the final results. This is particularly relevant for ptychography, which typically requires longer acquisition times than direct



Figure 4. Sketch of the Au and Ni test grid. The values of K- and L-edge for Au and Ni are listed.

methods. The reduced scanning time of a single-acquisition approach would increase the experimental throughput. Increasing the number of energy thresholds beyond four would allow to target multiple elements at once.

The radiation damage is an important aspect for applications to biomedical imaging. In general ptychography is dose efficient, thanks to the diversity in measurements from the illumination structure and the splitting up of information across the scanning positions. The dose delivered to the sample during the 2D acquisition was estimated from the readout of an ionization chamber placed upstream of the pinhole. A dose of about 200 Gy was calculated for the ptychographic images presented in this article; a value far below the maximum tolerable dose limit described in^{21,22}. When considering a 3D acquisition of a hundred projections the delivered dose would be on the order of 2×10^5 Gy, thus still acceptable for the spatial resolution of approximately 150 nm. The methodology described in this work is therefore promising also for biomedical applications of spectro-nanotomography.

Materials and methods

Source. The experiment has been developed and conducted at the I13 beamline of Diamond Light Source (DLS). The beamline consists of two independent and complementary branchlines: the coherence branch (I13-1) and the imaging branch (I13-2). The coherence branch is a multimodal, multiscale instrument for reciprocal space imaging: including ptychography²³, bragg CDI²⁴, and bragg-ptychography. The imaging branch is focused on real space imaging. The I13-1 ×-ray source consists of a 2.8 m long undulator with 2.5 cm period. The beamline operates in the 7-24 keV energy range with a distance from the source of 215 m and with a sample-detector distance up to 14.5 m. The Au L-Edge imaging with the proposed technique, requires two isolated harmonics either side of the Au L2 (13.7 keV) and L3 (11.9 keV) edges. During the experiment the undulator was tuned to produce one harmonic above and one harmonic below the Au L-edge with a separation matching the detector energy resolution. The selected harmonics were the 4th and the 5th, respectively at 11.0 and 13.8 keV. This configuration was achieved from a 3 GeV electron storage ring, by opening the undulator gap up to 13.64 mm. In a higher energy storage ring, for a similar insertion device, a smaller undulator gap would have been required to obtain a similar X-ray spectrum. The beam was filtered in order to reduce the contribution from lower and higher harmonics by a combination of metal filters (1.3 mm of pyrolytic graphite plus 0.7 mm of Al) and a Si mirror whose reflectivity drops quickly above 13 keV. The spectrum of the adapted incident beam at the sample is shown in Fig. 1a where two main peaks at 11.0 keV and 13.8 keV, respectively are clearly visible. For the reference images, the X-ray beam was monochromated using a Si(111) double crystal monochromator with 10^{-4} bandwidth.

Detector. Pixirad-1/Pixie-III is a direct detection XPCD built with a hybrid architecture, where a semiconductor sensor is coupled with flip-chip bonding technique to the ASIC. The sensor is a Schottky type diode array with electron collection on the pixels composed of a thick CdTe crystal (650 m) substrate. A common problem in XPCDs is the limited energy resolution due to charge sharing effects. In Pixie-III this problem is mitigated by summing up the signals of neighbouring pixels, to correctly evaluate the total energy of any event involving up to 4 pixels. This hardware solution improves the energy resolution¹¹, and this is beneficial for spectral imaging applications. Pixie-III is a 0.16 mm CMOS ASIC organized as a 512 × 402 matrix of square pixels with 62 m pitch resulting in an active area of 31.7×24.9 mm². The readout implements, at single pixel level, two 15-bit counters fed by two independent discriminators with programmable thresholds. During operation the detector is cooled at -30 °C and the CdTe crystal is biased with a working voltage of 400 V. Compared with other XPCDs based on the Medipix ASIC, the Pixie-III is a large area detector (one module of Pixie-III corresponds roughly to a 2×2 configuration of Medipix). This avoids the well-known problem of dead gaps in multi-module detectors, due to the fact that up until now it has been possible to make pixel detector read-out chips that can be abutted on three sides only and the fourth side is used for on-chip peripheral logic and wire-bond pads that permit electronic read-out. Dead gaps complicate X-ray imaging because several pixels need to be excluded or inpainted during the reconstruction process²⁵. Moreover, miscalibration of the different modules composing a large area detector sometimes occurs and this might affect the quality of the final recorded signal, thus requiring *ad hoc* pre-processing²⁶.

Samples and acquisitions. A suitable test object composed of a regular microscale grid of Au and Ni component (see schematic in Fig. 4) was scanned to demonstrate the feasibility of Au isolation via L-Edge subtraction. Ni was chosen because the X-ray absorption edges of Ni (K=8.3 keV and L1=1.0 keV) are far away from those of Au. Then a Siemens star was scanned to assess the spatial resolution achievable when considering object phase

reconstructed images. The Siemens star is made of Au and has an inner spike width of 50 nm. The detector distance is set by taking into account the resolution required for the lowest energy and the beam size required for the highest energy^{7,23}. The optimized experimental configuration resulted in a sample to detector distance of 10 m and a 5 m pencil beam illumination defined by a pinhole.

Reconstruction and analysis. The ptychographic reconstruction of the acquired patterns was performed using the PtyREX²⁷ reconstruction and analysis package available at Diamond Light Source. The software allows for several optimizations²³ (e.g. correction of motor position misalignment) which compensate for any potential artifacts. Each dataset was processed through 1000 iterations of ePIE²⁸ and multi-modal reconstruction with 4 modes was performed^{29,30}. For the case of the Siemens star reconstructions, the phase components of the complex-valued ptychographs are shown. The resulting pixel size was 72×72 nm for the 11.0 keV case (as well as for the pink beam + Pixirad-1/Pixie-III) and 57×57 nm for the 13.8 keV case (as well as for the pink beam + Pixirad-1/Pixie-III) ndex (UQI) was used to quantitatively compare the reference monochromatic image with the proposed pink beam image. For the case of the Au-Ni grid sample, after reconstruction the edge subtraction is performed on the modulus components of the complex-valued ptychographs. Since the pixel size of the reconstructed images is energy-dependent, image registration and calibration were necessary before performing the pixel-by-pixel LES. The resultant image is the difference in absorption across the selected edge.

Received: 7 January 2020; Accepted: 16 March 2020; Published online: 16 April 2020

References

- Fredenberg, E. Spectral and dual-energy X-ray imaging for medical applications. Nucl. Instruments Methods Phys. Res. Sect. A: Accel. Spectrometers, Detect. Assoc. Equip. 878, 74–87, https://doi.org/10.1016/j.nima.2017.07.044 (2018).
- 2. Suzuki, M. *et al.* Three-dimensional visualization of magnetic domain structure with strong uniaxial anisotropy via scanning hard X-ray microtomography. *Appl. Phys. Express* **11**, 036601, https://doi.org/10.7567/APEX.11.036601 (2018).
- Egan, C. K. et al. 3D chemical imaging in the laboratory by hyperspectral X-ray computed tomography. Sci. Reports 5, 15979, https:// doi.org/10.1038/srep15979 (2015).
- Rodenburg, J. M. et al. Hard-X-Ray Lensless Imaging of Extended Objects. Phys. Rev. Lett. 98, 034801, https://doi.org/10.1103/ PhysRevLett.98.034801 (2007).
- Holler, M. et al. Three-dimensional imaging of integrated circuits with macro- to nanoscale zoom. Nat. Electron. 2, 464–470, https:// doi.org/10.1038/s41928-019-0309-z (2019).
- Spence, J., Weierstall, U. & Howells, M. Coherence and sampling requirements for diffractive imaging. Ultramicroscopy 101, 149–152, https://doi.org/10.1016/j.ultramic.2004.05.005 (2004).
- 7. Edo, T. B. et al. Sampling in x-ray ptychography. Phys. Rev. A 87, 053850, https://doi.org/10.1103/PhysRevA.87.053850 (2013).
- Maiden, A., Morrison, G., Kaulich, B., Gianoncelli, A. & Rodenburg, J. Soft X-ray spectromicroscopy using ptychography with randomly phased illumination. *Nat. Commun.* 4, 1669, https://doi.org/10.1038/ncomms2640 (2013).
- 9. Donnelly, C. et al. Three-dimensional magnetization structures revealed with X-ray vector nanotomography. *Nature* 547, 328–331, https://doi.org/10.1038/nature23006 (2017).
- Batey, D. J. *et al.* Spectroscopic imaging with single acquisition ptychography and a hyperspectral detector. *Sci. Reports* 9, 12278, https://doi.org/10.1038/s41598-019-48642-y (2019).
- Bellazzini, R. et al. PIXIE III: A very large area photon-counting CMOS pixel ASIC for sharp X-ray spectral imaging. J. Instrumentation 10, C01032, https://doi.org/10.1088/1748-0221/10/01/C01032 (2015).
- Veale, M., Seller, P., Wilson, M. & Liotti, E. HEXITEC: A High-Energy X-ray Spectroscopic Imaging Detector for Synchrotron Applications. Synchrotron Radiat. News 31, 28–32, https://doi.org/10.1080/08940886.2018.1528431 (2018).
- Cipiccia, S. et al. Multi-scale multi-dimensional imaging at I13-coherence branchline in diamond light source. AIP Conf. Proc. 2054, 050005, https://doi.org/10.1063/1.5084623 (2019).
- Brun, F. et al. Single-shot K-edge subtraction x-ray discrete computed tomography with a polychromatic source and the Pixie-III detector. Phys. Medicine & Biol. 65, 055016, https://doi.org/10.1088/1361-6560/ab7105 (2020).
- Di Trapani, V. et al. Characterization of noise and efficiency of the Pixirad-1/Pixie-III CdTe X-ray imaging detector. J. Instrumentation 13, C12008, https://doi.org/10.1088/1748-0221/13/12/C12008 (2018).
- Di Trapani, V. et al. Characterization of the acquisition modes implemented in Pixirad-1/Pixie-III X-ray Detector: Effects of charge sharing correction on spectral resolution and image quality. Nucl. Instruments Methods Phys. Res. Sect. A: Accel. Spectrometers, Detect. Assoc. Equip. 955, 163220, https://doi.org/10.1016/j.nima.2019.163220 (2020).
- Vincenzi, A. et al. Energy characterization of Pixirad-1 photon counting detector system. J. Instrumentation 10, C04010, https://doi. org/10.1088/1748-0221/10/04/C04010 (2015).
- Da Silva, J. et al. Overcoming the challenges of high-energy X-ray ptychography. J. Synchrotron Radiat. 26, 1751–1762, https://doi. org/10.1107/S1600577519006301 (2019).
- 19. Yabashi, M. et al. Optics for coherent x-ray applications. J. Synchrotron Radiat. 21, 976–985, https://doi.org/10.1107/ \$1600577514016415 (2014).
- Williams, S. *et al.* The ExcaliburRX-3M X-Ray Photon Counting Area Detector for Coherent Diffraction Imaging at the I13 Beamline at Diamond Light Source. 2017 IEEE Nucl. Sci. Symp. Med. Imaging Conf. NSS/MIC 2017 - Conf. Proc. 8532988, https:// doi.org/10.1109/NSSMIC.2017.8532988 (2018).
- Howells, M. R. et al. An assessment of the resolution limitation due to radiation-damage in x-ray diffraction microscopy. J. electron spectroscopy related phenomena 170, 4–12, https://doi.org/10.1016/j.elspec.2008.10.008 (2009).
- Gianoncelli, A. et al. Soft x-ray microscopy radiation damage on fixed cells investigated with synchrotron radiation ftir microscopy. Sci. Reports 5, 10250, https://doi.org/10.1038/srep10250 (2015).
- Batey, D. et al. Reciprocal-space up-sampling from real-space oversampling in x-ray ptychography. Phys. Rev. A At. Mol. Opt. Phys. 89, 043812, https://doi.org/10.1103/PhysRevA.89.043812 (2014).
- Newton, M., Parsons, A., Wagner, U. & Rau, C. Coherent x-ray diffraction imaging of photo-induced structural changes in BiFeO3 nanocrystals. *New J. Phys.* 18, 093003, https://doi.org/10.1088/1367-2630/18/9/093003 (2016).
- Brun, F., Delogu, P., Longo, R., Dreossi, D. & Rigon, L. Inpainting approaches to fill in detector gaps in phase contrast computed tomography. *Meas. Sci. Technol.* 29, 014001, https://doi.org/10.1088/1361-6501/aa91ad (2018).
- Brombal, L. et al. Large-area single-photon-counting CdTe detector for synchrotron radiation computed tomography: A dedicated pre-processing procedure. J. Synchrotron Radiat. 25, 1068–1077, https://doi.org/10.1107/S1600577518006197 (2018).
- 27. Batey, D. J. Ptychographic Imaging of Mixed States (PhD thesis, University of Sheffield, 2014).

- Maiden, A. M. & Rodenburg, J. M. An improved ptychographical phase retrieval algorithm for diffractive imaging. Ultramicroscopy 109, 1256–62, https://doi.org/10.1016/j.ultramic.2009.05.012 (2009).
- Thibault, P. & Menzel, A. Reconstructing state mixtures from diffraction measurements. Nature 494, 68–71, https://doi.org/10.1038/ nature11806 (2013).
- Batey, D., Claus, D. & Rodenburg, J. Information multiplexing in ptychography. Ultramicroscopy 138, 13–21, https://doi. org/10.1016/j.ultramic.2013.12.003 (2014).

Acknowledgements

The KEST project, funded by INFN - Istituto Nazionale di Fisica Nucleare (National Scientific Committee 5 for Technological and Interdisciplinary research) is acknowledged. The research leading to this result has been supported by the project CALIPSOplus under Grant Agreement 730872 from the EU Framework Programme for Research and Innovation HORIZON 2020. Diamond Light Source is acknowledged for the funding and beamtime provided under proposal no. MG21555-1.

Author contributions

S.C. and D.B. conceived the experiment(s), F.B., V.D.T., D.B., S.C. conducted the experiment(s), F.B., D.B., S.C. wrote the article. F.B., V.D.T., D.B., S.C., C.R. reviewed the manuscript.

Competing interests

The authors declare no competing interests.

Additional information

Correspondence and requests for materials should be addressed to F.B.

Reprints and permissions information is available at www.nature.com/reprints.

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons license, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons license and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this license, visit http://creativecommons.org/licenses/by/4.0/.

© The Author(s) 2020